

EXHIBIT 2N

**IN THE UNITED STATES DISTRICT COURT
FOR THE SOUTHERN DISTRICT OF WEST VIRGINIA
CHARLESTON DIVISION**

IN RE: ETHICON, INC., PELVIC REPAIR SYSTEM PRODUCTS LIABILITY LITIGATION	Master File No. 2:12-MD-02327 MDL 2327
THIS DOCUMENT RELATES TO: ALL CASES LISTED BELOW	JOSEPH R. GOODWIN U.S. DISTRICT JUDGE

<i>Mullins, et al. v. Ethicon, Inc., et al.</i>	2:12-cv-02952
<i>Sprout, et al. v. Ethicon, Inc., et al.</i>	2:12-cv-07924
<i>Iquinto v. Ethicon, Inc., et al.</i>	2:12-cv-09765
<i>Daniel, et al. v. Ethicon, Inc., et al.</i>	2:13-cv-02565
<i>Dillon, et al. v. Ethicon, Inc., et al.</i>	2:13-cv-02919
<i>Webb, et al. v. Ethicon, Inc., et al.</i>	2:13-cv-04517
<i>Martinez v. Ethicon, Inc., et al.</i>	2:13-cv-04730
<i>McIntyre, et al. v. Ethicon, Inc., et al.</i>	2:13-cv-07283
<i>Oxley v. Ethicon, Inc., et al.</i>	2:13-cv-10150
<i>Atkins, et al. v. Ethicon, Inc., et al.</i>	2:13-cv-11022
<i>Garcia v. Ethicon, Inc., et al.</i>	2:13-cv-14355
<i>Lowe v. Ethicon, Inc., et al.</i>	2:13-cv-14718
<i>Dameron, et al. v. Ethicon, Inc., et al.</i>	2:13-cv-14799
<i>Vanbuskir, et al. v. Ethicon, Inc., et al.</i>	2:13-cv-16183
<i>Mullens, et al. v. Ethicon, Inc., et al.</i>	2:13-cv-16564
<i>Shears, et al. v. Ethicon, Inc., et al.</i>	2:13-cv-17012
<i>Javins, et al. v. Ethicon, Inc., et al.</i>	2:13-cv-18479
<i>Barr, et al. v. Ethicon, Inc., et al.</i>	2:13-cv-22606
<i>Lambert v. Ethicon, Inc., et al.</i>	2:13-cv-24393
<i>Cook v. Ethicon, Inc., et al.</i>	2:13-cv-29260
<i>Stevens v. Ethicon, Inc., et al.</i>	2:13-cv-29918
<i>Harmon v. Ethicon, Inc., et al.</i>	2:13-cv-31818
<i>Snodgrass v. Ethicon, Inc., et al.</i>	2:13-cv-31881
<i>Miller v. Ethicon, Inc., et al.</i>	2:13-cv-32627
<i>Matney, et al. v. Ethicon, Inc., et al.</i>	2:14-cv-09195
<i>Jones, et al. v. Ethicon, Inc., et al.</i>	2:14-cv-09517
<i>Humbert v. Ethicon, Inc., et al.</i>	2:14-cv-10640
<i>Gillum, et al. v. Ethicon, Inc., et al.</i>	2:14-cv-12756
<i>Whisner, et al. v. Ethicon, Inc., et al.</i>	2:14-cv-13023

<i>Tomblin v. Ethicon, Inc., et al.</i>	2:14-cv-14664
<i>Schepleng v. Ethicon, Inc., et al.</i>	2:14-cv-16061
<i>Tyler, et al. v. Ethicon, Inc., et al.</i>	2:14-cv-19110
<i>Kelly, et al. v. Ethicon, Inc., et al.</i>	2:14-cv-22079
<i>Lundell v. Ethicon, Inc., et al.</i>	2:14-cv-24911
<i>Cheshire, et al. v. Ethicon, Inc., et al.</i>	2:14-cv-24999
<i>Burgoyne, et al. v. Ethicon, Inc., et al.</i>	2:14-cv-28620
<i>Bennett, et al. v. Ethicon, Inc., et al.</i>	2:14-cv-29624

RULE 26 EXPERT REPORT OF PROF. DR. MED. UWE KLINGE

I. SUMMARY OF OPINIONS

Based on my background training and experience as a general and abdominal surgeon who used Prolene mesh for hernia repair in patients and treated Prolene-mesh-related complications in patients, and based on over 20 years of studying Prolene and other surgical meshes as a biomaterials scientist, 10 years of which were as a consultant to Ethicon regarding safe mesh design in their preclinical studies of Prolene and other surgical meshes, performing histopathological analysis on hundreds of explanted hernia, sling and prolapse meshes, being an invited lecturer at conferences around the world on the topic of surgical meshes, authoring or co-authoring over 100 peer-reviewed publications regarding surgical meshes, including numerous ones regarding Prolene mesh, reviewing thousands of pages of scientific literature, thousands of pages of internal Ethicon documents and thousands of pages of deposition testimony, the following is a summary of my opinions in this case, all of which I hold to a reasonable degree of medical and scientific certainty.¹

2

The Prolene mesh in TVT undergoes a Chronic FBR.

After implantation of the TVT mesh, there is a chronic (permanent) foreign body reaction in a woman's pelvic tissue whereby the woman's body will react to the polypropylene indefinitely, creating a chronic inflammatory response that leads to scarring around the mesh fibers. Claims by Ethicon in its TVT Instructions for Use (IFU) that "a transient foreign body response may occur" and in its TVT marketing brochures that there is "[n]o foreign body reaction after PROLENE mesh implantation" are inconsistent, false and misleading, and Ethicon knew or should have been known them to be untrue at the time the company employees wrote these documents and certainly prior to the launch of TVT in 1998.

The weight (surface area) of the Prolene mesh in TVT unnecessarily increases the risk of patient injury versus lighter weight mesh design.

The greater the surface area of a medical implant, the greater the foreign body reaction and the inflammatory response. Ethicon had critical mesh design information regarding the negative consequences in the human tissue of heavy weight, small pore meshes beginning as early as

¹ Because the material used in Ethicon's incontinence repair meshes is of identical construction, i.e., so-called "Old Construction" 6 mil Prolene, with certain exceptions as noted herein, the acronym "TVT" will be used throughout this report to represent the entire TVT incontinence sling product line by Ethicon.

1998. The heavy weight Prolene mesh (105-110 g/m²) in Ethicon's TVT products is many times stronger than it needs to be for its intended purpose of treating stress urinary incontinence and thus, it is "overengineered" and leaves much more polymer material in a woman's delicate and sensitive pelvic tissues than is necessary. Any pelvic mesh designed with this much excess surface area and weight unreasonably and unnecessarily increases the risk of injury to the patient and is a less safe design than lighter weight mesh as it causes an unnecessarily increased FBR and inflammatory response

The distance between the fibers of the Prolene mesh in TVT unnecessarily increases the risk of patient injury versus mesh design with a larger distance between the fibers.

The smaller the distance between the fibers of a mesh implant, the greater the risk of scar tissue forming in the pores ("bridging fibrosis" or "fibrotic bridging"). As early as 1998, and certainly by the early 2000's, Ethicon had critical design information that the risk of bridging fibrosis is increased by polypropylene surgical mesh with a distance between the fibers of less than 1mm in all directions, which in turn increases the risk of a rigid scar plate forming throughout the mesh, leading to integration of the entire mesh in scar tissue. Any pelvic mesh designed with pores this small unreasonably and unnecessarily increases the risk of injury to the patient and is a less safe design than mesh with a greater distance between the fibers. The pore size of the Prolene mesh in Ethicon's TVT products is, according to Ethicon, less than 1mm.

Ethicon's failure to implement new, critical mesh design changes (lighter weight, greater distance between the fibers) in TVT before the launch of TVT-R in 1998 was unreasonable; it unnecessarily compromised patient safety; and it has led to patient complications like chronic inflammatory reaction, excessive scarring through and around the mesh, nerve entrapment, chronic pain, dyspareunia, erosions, recurrence and the necessity of reoperation in an attempt to correct these problems. The Prolene mesh in Ethicon's TVT products is unsuitable for use as a permanent implant for treatment of a woman's stress urinary incontinence. Ethicon did not act as a reasonable manufacturer in choosing to use the "Old Construction 6 mil" Prolene mesh in its TVT products.

3

The Prolene mesh in TVT undergoes pore deformation under minimal stress.

A knitted surgical mesh device like the TVT that is permanently implanted in human tissue must be designed in such a manner that the pores of the mesh do not collapse and deform upon the expected forces of implantation as well as the expected in vivo forces. Under minimal strain, the TVT mesh pores deform and collapse thereby increasing the risk of injury to patients in which it is implanted and is a less safe design than products that better withstand these conditions and do not display these poor outcomes. Permanent deformation and pore collapse of the TVT mesh leads to fibrotic bridging, scar plate formation, excessive scarring through and around the mesh and a host of tissue complications that can lead to chronic pain, recurrence, erosions, dyspareunia and need for reoperation, to name a few, making it unnecessarily unsafe for its intended purpose of being permanently implanted in a woman's pelvic tissue.

The Prolene mesh in TVT contracts/shrinks.

The Prolene mesh in Ethicon's TVT products contracts or shrinks 30-50% after implantation. This shrinkage was known in the medical device community prior to the launch of TVT in 1998. TVT mesh shrinkage, caused by fibrosis leads to nerve entrapment, chronic pelvic pain, erosions, organ dysfunction, recurrence and the need for reoperation to remove some or all of the contracted mesh and excessive scar tissue, thereby making TVT unsuitable for its intended use as a permanent pelvic implant to treat stress urinary incontinence in women.

The Mechanical Cut Prolene Mesh in the TVT products deforms, frays, loses particles, curls and ropes increasing the risk of complications to the patients.

The TVT mesh is a knitted textile design without a border and therefore, as tension is placed on the mesh, its frayed, unbordered edges shed particles of polypropylene before, during and after the surgery. As tension is placed on the mesh, it also curls and ropes causing increased scarring between the fibers. The release of particles into the surrounding tissue with its increase of surface area and the curled roped mesh all lead to an increased inflammatory response, chronic foreign body reaction, erosions, chronic pelvic pain, failure of the implant, chronic sexual dysfunction and dyspareunia, organ damage, urinary dysfunction, inability to remove the device and the need for surgical intervention.

There are safer alternative pelvic mesh design characteristics than those of TVT.

There are alternative design characteristics of pelvic floor meshes that would be safer in a woman's pelvic tissues as a treatment for incontinence than some of the design characteristics of the Prolene mesh in TVT. The Old Construction TVT MCM Prolene mesh was created in the 1970's, years before Ethicon developed meshes for both hernia repair and pelvic floor repair using safer mesh design. For example, by the late 1990's and early 2000's, the technology of surgical meshes had evolved to produce meshes that were lighter weight, had greater distance between the fibers, had better stability under stress, had laser cut edges and had a different polymer material. Ethicon began marketing lighter weight meshes with larger distance between the fibers as early as 1998 and continued to advance this technology in its hernia and certain pelvic floor repair mesh products through 2002. It had designed meshes with a different polymer (PVDF) by at least 2002 and meshes that were laser cut by 1998, including TVT laser cut samples.² Ethicon knew in 1999 that the TVT with the laser cut mesh had a marked reduction in the amount of loose ends falling off compared to mechanically cut mesh, and is less difficult to deform, facilitating correct placement of the mesh.³ However, Ethicon has continued to market its 1970's technology Old Construction Prolene mesh in its original TVT-R up to the present date.

Based upon the opinions above, I am able to conclude, to a reasonable degree of medical and scientific certainty, that the Prolene mesh used in Ethicon's TVT products is designed in such a way that it does in fact unnecessarily cause a greater inflammatory response and greater foreign body reaction in women's pelvic tissues leading to harmful complications in some patients. I am also able to conclude that these materials were inadequately tested and studied before being sold to treat incontinence and that as a result of all of these factors, set forth more fully in this report,

² ETH.MESH.12009078-12009081

³ ETH.MESH.10182456-10182461

the TVT device is not adequately designed to be safely implanted in a woman's pelvis for the rest of her life.

II. BACKGROUND AND QUALIFICATIONS

With regard to my medical training, I attended medical school in Aachen, Germany from 1977 to 1983. I began my medical profession at the surgical department of the University Hospital of the RWTH, Aachen, Germany (Department heads/Mentors: Prof. Reifferscheid - 1985, Schumpelick 1985-2010, Neumann 2010-). From 1995 to 2006, my practice was focused primarily on abdominal surgery, and specifically, hernia repair. As a hernia surgeon, I used textile implants (flat meshes) for the repair of abdominal wall hernia or defects in more than 300 patients; mainly groin hernia, umbilical hernia, incisional hernia and parastomal hernia. Although I never performed surgery for repair of SUI or POP, I implanted and studied the Prolene mesh used in TVT extensively over many years.

In 1993, in addition to my surgical practice, I began focusing on surgical research in the area of biomaterial science including tissue engineering and material characteristics, and I designed preclinical models for safe surgical mesh design, including histopathological analysis. I am the author/co-author of approximately 200 peer-reviewed publications listed in PubMed, over 100 of which involve hernia and/or surgical mesh. I have authored and/or contributed to more than 50 book chapters and have been an invited lecturer to more than 160 speaking engagements/conferences. I have received numerous research grants from various institutions and corporations including several grants from the German Ministry for Education and Research, the Ministry for Economics, the German research foundation DFG, the NRW Ministry for Education and Research, the Interdisciplinary Center for Clinical Research of the University of Aachen (RWTH), as well as from industry (Ethicon, Covidien). (Attached hereto as Appendix "A" is a current copy of my Curriculum Vitae with a list of my publications).

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III. BRIEF HISTORY OF TEXTILE MESHES FOR TISSUE REPAIR 1958-1993 – THE ABDOMINAL WALL

The current use of textile meshes is based on Usher who, in 1958, started to publish the successful reinforcement of the abdominal wall in six dogs. Initially, meshes were regarded as an alternative procedure, particularly in big hernias. In 1986, Lichtenstein presented his procedure of mesh implantation as the new standard for groin hernia repair. With this technique, the mesh reinforces the tissue in a so-called "tension free" manner. In the early years, Usher used a knitted structure of polypropylene, later widely known as Marlex®. However, Marlex® had increased stiffness after implantation along with considerable complications. Alternatives to Marlex were the polyester mesh Mersilene® from Ethicon or the ePTFE mesh from Gore.

In the late 1980's and early 1990's, when polypropylene surgical mesh was increasingly used in hernia surgeries, there was a general lack of knowledge about the materials and about the clinical outcomes associated with these materials. Side effects often manifested with a considerable delay of up to several years. Correspondingly, reports dealing with pain as a major postoperative complication (less than 10% of all hernia publications in PubMed) were published with a delay of years [Fig.1]. We began to look at the scar formation pathologically and developed the theory that incisional hernias could be due to a defective wound healing process

with an impaired collagen formation, favoring the necessity to support tissues in these patients by prosthetics.

Delayed complications after mesh publications in PubMed 1960-2008

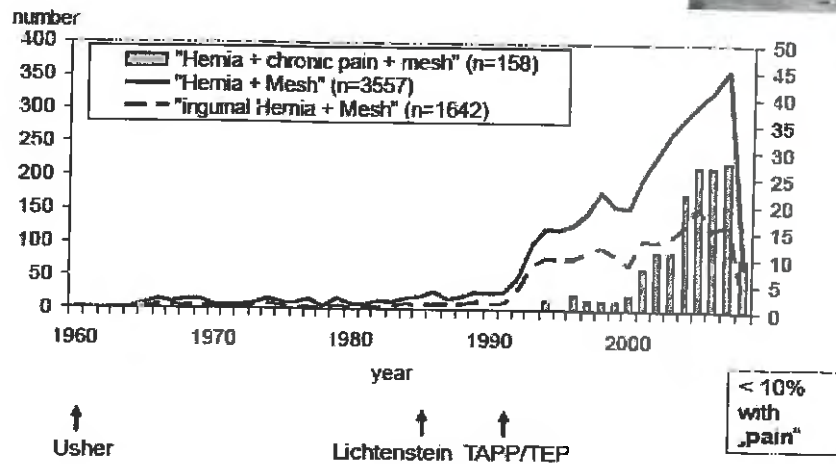


Figure 1

IV. DEVELOPMENT OF THE FIRST LARGE PORE MESH CONSTRUCTION THAT WAS ADAPTED TO PHYSIOLOGICAL REQUIREMENTS

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In the early 1990's, we speculated that an adaptation of the strength of surgical meshes to the physiological requirements of the tissues in which they would be implanted may allow a considerable material reduction which could improve biocompatibility. We felt that the textile characterization of meshes at that time did not sufficiently reflect the physicochemical properties of the textile, so we began our work by first identifying the relevant parameters.

In conjunction with various grants, RWTH University initiated a research program to study safe mesh design. Through cooperative efforts with Ethicon and the support by these research grants, the project went on for about 10 years. In this period, we gained significant knowledge about the textiles; we defined standard biomechanical characterization for better comparison of different mesh designs; we established models for testing the tissue response in animals; we looked for parameters that reflected the inflammatory and fibrotic activity of the foreign body reaction; and we developed a technique to quantify the biomechanical impact on, and the biomechanical properties of, tissues.

As our research progressed, we calculated that hernia meshes needed a tensile strength of 16 N/cm and an elasticity of about 20-30% at this strain. Ethicon provided our research team with thin (about 40 μ m) polypropylene threads. Because we were provided only with these 40- μ m fibers, we had to combine 5 strands of them at interval distances of 2-3 mm to withstand a strain of 16 N/cm. As this polypropylene net was very floppy, we added an absorbable fiber of Vicryl® (Ethicon) to temporarily make it stiffer. After absorption of the Vicryl®, there remained an open structure with about 30% of the material of the Prolene. This new structure with pores larger than

2 mm, later marketed as Vypro® by Ethicon (1998) and patented in 2000 in the US (6,192,962), was then studied extensively in several experimental studies. The results were presented at several conferences and most of it has been published in PubMed-listed journals. Vypro® was the first truly lightweight, large pore surgical mesh and became the first of the second-generation surgical meshes. This development would become what is known as the “Lightweight Large Pore Concept” which has been adopted by surgical mesh manufacturers worldwide in developing newer generation meshes and was set forth in various publications by my colleagues and me, as well as other surgical mesh scientists, starting in 1998.⁴ Ethicon’s own employees have testified that they agree with our work, including that lighter weight meshes with larger distance between the mesh fibers will reduce the foreign body response and inflammatory reaction compared to heavier weight meshes with smaller pores. Dr. Axel Arnaud, Ethicon’s Medical Affairs Group Director, testified that our lightweight large pore concept is “agreed upon by most of the people involved in the science of meshes...this is the basic science about meshes [and] I certainly will not challenge this.”⁵

V. BIOCOMPATIBILITY

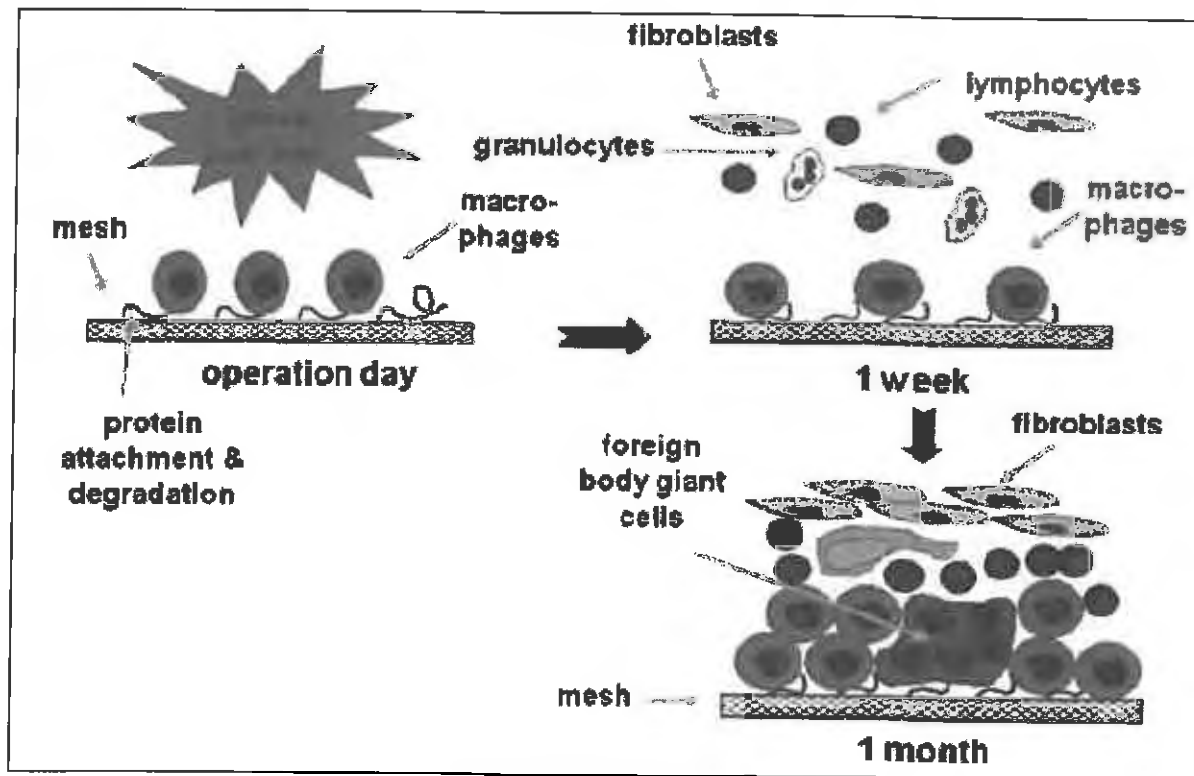
A. Foreign Body Reaction

All experimental and clinical studies indicate that surgical mesh products cause an initial and chronic inflammatory tissue response in the patient after implantation. The quality of the inflammatory reaction to foreign bodies of different natures is surprisingly constant, characterized by a rapid accumulation of huge numbers of phagocytic cells, in particular, blood monocytes and tissue-derived macrophages. This type of inflammatory process is known as a foreign body reaction (FBR). It is characterized by an initial inflammatory burst caused by a release of a huge combination of potent inflammatory mediators which then attract other cell types including T-cells, polymorphonuclear granulocytes (PMNs), plasma cells and fibroblasts. Within a few days, this cellular activity forms an early granuloma layer around the mesh fibers recognized by the very typical foreign body giant cells and an outer layer of fibrosis with deposition of collagen. This late stage granuloma is not a static type of chronic inflammation but rather, it represents a chronic wound with an increased cell turnover even years after implantation. The various inflammatory cells, e.g., macrophages, at the interface and in contact with the polymer, undergo apoptotic cell death and are replaced. [Fig. 2]

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⁴ Klosterhalfen, B., Junge, K., Klinge, U. *The lightweight and large porous mesh concept for hernia repair*. Expert Rev. Med. Devices. 2005; 2(1); Klinge U, Klosterhalfen B, Muller M, Ottinger A, Schumpelick V. Shrinking of Polypropylene Mesh in vivo: An Experimental Study in Dogs. Eur J Surg. 1998; 164: 965-969; Klinge, U., Klosterhalfen, B., Birkenhauser, V., Junge, K., Conze, J., Schumpelick, V. Impact of Polymer Pore Size on the Interface Scar Formation in a Rat Model. Journal of Surgical Research. 103, 208-214 (2002); Cobb W, Kercher K, Heniford T. The Argument for Lightweight Polypropylene Mesh in Hernia Repair. Surgical Innovation. 2005; 12(1):T1-T7; Cobb WS, Burns JM, Peindl RD, Carbonell AM, Matthews BD, Kercher KW, Heniford BT Textile analysis of heavyweight, mid-weight, and lightweight polypropylene mesh in a porcine ventral hernia model. J Surg Res. 2006 Nov; 136(1):1-7. Epub 2006 Sep 22.

⁵ Arnaud deposition 9/25/13 772:25 to 777:16; 779:4-11

Figure 2⁶

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We published our results in 1998 and 1999 of the histological analyses from explanted mesh from both animals and humans. The tissue response in humans was almost identical to the morphological observations in the animal models. In our 1999 study, we reviewed approximately 350 human explant samples of various mesh modifications gathered from centers all over Europe. Even 15 years after explantation, the longest observation in our study, a persistent chronic FBR could still be detected, indicating that mesh is likely never completely inert with respect to local inflammatory processes. The persistence of this FBR is important, especially in younger patients in whom the mesh will remain for several decades. The delay before explantation of mesh for infection of up to 56 months, for chronic pain of up to 48 months and for recurrence of up to 180 months established that in many clinical studies with shorter surveys of less than 1-2 years, the morbidity rates are underestimated.^{7,8} It is well known in the medical community that the vagina is considered a “clean-contaminated” field. The implantation of mesh may result in a biofilm which will make it difficult for the host cells to kill the mesh infection; in fact, the development of these biofilms will protect the harmful bacteria that the host cells set out to kill.⁹

⁶ Semin Immunopathol (2011) 33:235-243 – Formation of a foreign body granuloma at the mesh to host tissue interface

⁷ Klinge U, Klosterhalfen B, Muller M, Ottinger A, Schumpelick V. Shrinking of Polypropylene Mesh in vivo: An Experimental Study in Dogs. Eur J Surg. 1998; 164: 965-969

⁸ Klinge U, Klosterhalfen B, Muller M, Schumpelick V. Foreign Body reaction to Meshes Used for the Repair of Abdominal Wall Hernias; Eur J Surg 1998; 164: 951-960

⁹ Osterberg B. ActaChirScand1979;145:431, Merritt K. J BiomatAppl 1991;5:185, An Y. J Biomed Mater Res (Appl Biomat) 1998;43:338

Furthermore, my colleague and Ethicon's top pathology consultant for 20 years, Bernd Klosterhalfen, informed Ethicon at an expert meeting at Ethicon's Norderstedt facilities in 2006 that based on our studies, the tissues in the body can react to the mesh for up to 20 years.¹⁰

At another Ethicon expert meeting at Norderstedt the following year, in a PowerPoint presentation to the experts in attendance, Ethicon stated that there can be "excessive FBR > massive scar plate > more shrinkage" depending on the type of mesh.¹¹ Ethicon stated in that presentation that "small porous meshes (<1mm) lead to 'fibrotic bridging' > increased shrinkage."

Ethicon employees have testified that Ethicon knew before the launch of its pelvic meshes, for both incontinence and prolapse repair, that in some women, there would be a severe FBR and chronic life-altering inflammatory reaction causing debilitating and chronic pain, erosions, recurrence, need for revision surgery and dyspareunia.^{12, 13, 14, 15}

It is my opinion to a reasonable degree of medical and scientific certainty that after implantation of the TVT mesh, there is a chronic (permanent) foreign body reaction in a woman's pelvic tissue whereby the woman's body will react to the polypropylene indefinitely, creating a chronic inflammatory response that leads to scarring around the mesh fibers. Claims by Ethicon in its TVT Instructions for Use (IFU) that "a transient foreign body response may occur" and in its TVT marketing brochures that there is "[n]o foreign body reaction after PROLENE mesh implantation" are inconsistent, false and misleading.^{16, 17} In addition to abundant scientific literature to the contrary, deposition testimony of numerous Ethicon employees in this litigation also demonstrates the falsity of this statement.^{18, 19, 20}

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B. Weight

As is evidenced in countless pages of deposition testimony of Ethicon employees and internal Ethicon documents, Ethicon was aware that lighter weight meshes with greater distance between the mesh fibers lessened the risk of these harmful tissue reactions and thus, lessened the risk of injury to patients.

Ethicon's Medical Affairs Director, Piet Hinoul, recounts the history of Ethicon's attempts to develop lighter weight, larger pore meshes and the multiple reasons for doing so in a 2012 Clinical Expert Report for their light weight, large pore mesh, Ultrapro/Prolift + M:²¹

Knitted, polypropylene mesh as a reinforcement for Hernia Repair has been used for 40+ years and is an accepted method for reducing recurrence of abdominal wall defects seen in both incisional and inguinal hernias. However,

¹⁰ ETH.MESH.00870466 2006 Expert Meeting Norderstedt

¹¹ ETH.MESH.01782867 "Factors Related to Mesh Shrinkage" Powerpoint presentation by Kestin Sychaj

¹² Hinoul deposition 4/5/12 99:09-99:25, 4/6/12 518:14-520:20, 6/26/13 175:1-176:17, 184:18-22 328:10-24;

¹³ Owens deposition 9/12/2012 98:11 to 99:07;

¹⁴ Batke deposition 08/01/13 257:23 to 259:13

¹⁵ Arnaud deposition 9/25/13 769:23 to 770:4

¹⁶ ETH.MESH.00339437-442 "5 Years of Proven Performance" Feb 2002

¹⁷ ETH.MESH.02340504 TVT IFU

¹⁸ Barbolt deposition 10/9/13 137:01 to 137:17;

¹⁹ Holste deposition 07/29/13, 51:3 to 53:6

²⁰ Hellhammer deposition 9/11/2013, 60:24-61:1; 210:15-211:16

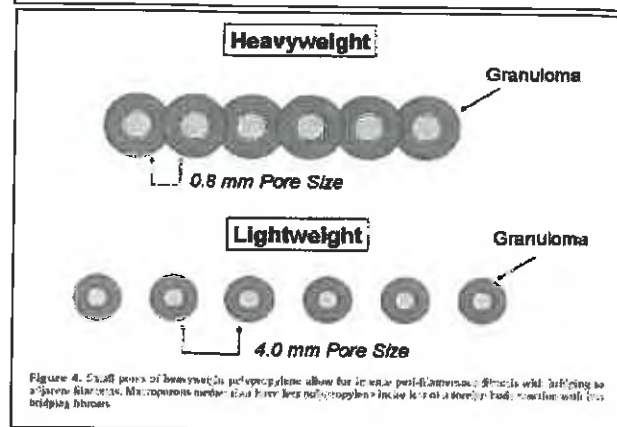
²¹ ETH.MESH.08315779 "Clinical Expert Report" dtd 9-25-2012 at 782.

implantation of polypropylene mesh is associated with an increase in problems associated with the foreign material implant. Complications associated with these materials have led to changes in implant materials and construction with a goal to 1) reduce implant mass and 2) increase the mesh pore size. The impact of such reductions in material mass on the durability of the repair must be considered. Assessing the breaking strength of healthy tissue, in vivo measurements of maximum pressure during the stresses of coughing, jumping and Valsalva maneuver, and mathematical modeling of abdominal wall forces, have led to the conclusion that synthetic mesh implants, even the lower mass mesh implants, are significantly stronger than required (Deprest et 2006, Cobb et al. 2005).²²

The Cobb 2005 article states that heavy weight meshes with less than 1 mm between the mesh fibers lead to scarring across the mesh fibers ("fibrotic bridging"). He lists several meshes of varying weights in the article of which Prolene is one of the heaviest weight meshes. [See Figures 3 and 4]²³

Table 1. Polypropylene meshes of differing densities

Surgipro ^a	110 g/m ²
Prolene ^b	105 g/m ²
Marlex ^c	95 g/m ²
Prolite ^d	90 g/m ²
Prolene Soft Mesh ^b	45 g/m ²
Vypro II ^b	35 g/m ²
Ultrapro ^b	28 g/m ²



Figures 3 and 4

²² ETH.MESH.08315779 "Clinical Expert Report" dtd 9-25-2012 at 782.

²³ Cobb W, Kercher K, Heniford T. The Argument for Lightweight Polypropylene Mesh in Hernia Repair. Surgical Innovation. 2005; 12(1):T1-T7

It is my opinion, to a reasonable degree of medical and scientific certainty, that the greater the surface area of a medical implant, the greater the foreign body reaction and the inflammatory response will be. Ethicon had critical mesh design information regarding the negative consequences in the human tissue of heavy weight, small pore meshes beginning as early as 1998. The heavy weight Prolene mesh (105-110 g/m²) in Ethicon's TVT products is many times stronger than it needs to be for its intended purpose of treating stress urinary incontinence and thus, it is "overengineered" and leaves much more polymer material in a woman's delicate and sensitive pelvic tissues than is necessary. Any pelvic mesh designed with this much excess surface area and weight unreasonably and unnecessarily increases the risk of injury to the patient and is a less safe design than lighter weight mesh as it causes an unnecessarily increased FBR and inflammatory response.

C. Pore Size

Polypropylene filaments cause an intense inflammatory response in the abdominal wall as well as in the tissues of the pelvic floor. There is an increased fibrotic reaction hindering the physiological remodeling at the tissue/implant interface. This intense scar formation contributes to the wound contraction.²⁴

In our studies from the late 1990's, in which we evaluated the inflammatory response and fibrotic reaction in the tissues at the interface with the mesh implant, we saw that that large pore mesh (Vypro) was integrated into a loose network of perifilamentous fibrosis with fat tissue present in between the fibers. In contrast, the small pore mesh was incorporated entirely in perifilamentary granulomas and scar tissue, which bridged the whole pore diameter <1 mm. This phenomenon, known as "fibrotic bridging", exists when granulomas, side by side, form a common outer fibrotic capsule joining each mesh fiber and forming a rigid "scar plate" covering the whole mesh. This scar plate leaves no space for further tissue ingrowth and leads to a number of complications including loss of elasticity and pain associated with the rigidity, shrinkage or contraction of the mesh, mesh erosion, nerve entrapment, chronic pain and dyspareunia.

The concept of fibrotic bridging and harmful scar plate formation is evident in numerous internal Ethicon documents.^{25, 26, 27, 28, 29, 30, 31, 32, 33, 34, 35, 36, 37} [Figure 5]

²⁴ Junge K., Binnebosel, M., Rosch R., Jansen, M., Kammer, D., Otto, J., Schumpelick, V., Klinge, U., *Adhesion formation of a polyvinylidenefluoride/polypropylene mesh for intra-abdominal placement in a rodent animal model.* (2009) Surg Endosc; 23(2):327-33

²⁵ ETH.MESH.04037600 Innovations in mesh development

²⁶ ETH.MESH.05920616 7/20/07; Chomiak, Martin to Batke, Boris; Jamieson, Gillian; Koehler, Petra; Hellhammer, Dr. Brigitte SUBJECT: Defining light weight mesh

²⁷ ETH.MESH.05585033

²⁸ ETH.MESH.05446127 3/13/2006 Holste, Dr. Joerg to Engel, Dr. Dieter; Manley, Quentin; Storch, Mark L. SUBJECT: AW: Mesh and Tissue Contraction in Animal

²⁹ ETH.MESH.05475773

³⁰ ETH.MESH.04015102 3/01/12 Batke, Boris to Mayes, Casey SUBJECT: AW: AGES Pelvic Floor Conference-Gala Dinner Invitation

³¹ ETH.MESH.04037600 Mesh Innovations PowerPoint

³² ETH.MESH.09651393 Invention Disclosure

³³ ETH.MESH.05585066 "Ultrapro" Powerpoint presentation by Boris Batke

³⁴ ETH.MESH.05916450 "Chronic Pain Prevention/future - Bioengineer's point of view"

³⁵ ETH.MESH.04037600 "Innovations in Mesh Development" PowerPoint presentation by Boris Batke

³⁶ ETH.MESH.00237968 "R&D Perspective - The Journey from Prolift to Prolift +M" PowerPoint presentation by Cliff Volpe

³⁷ ETH.MESH.01782867 "Factors Related to Mesh Shrinkage" by Kerstin Spychaj

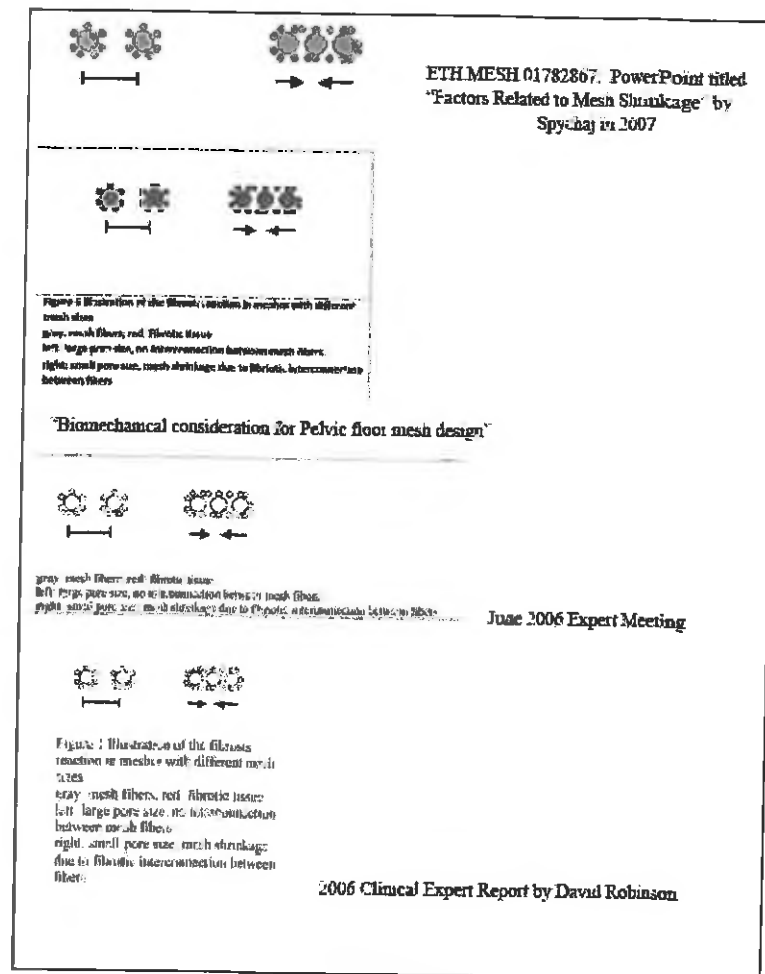


Figure 5

With the development of Vypro, we were able to increase the distance between the mesh fibers by up to 500-600% (Vypro 3-5 mm vs. Prolene <1mm) and decreased the weight from 105-110 g/m² (Prolene) to 25g/m² (Vypro). Given that the risk of bridging fibrosis is increased by less distance between the fibers, any mesh designed with smaller pores unnecessarily increases the risk of injury to the patient and is a less safe design than mesh a larger distance between the fibers. Simply put: the greater the pore size or open space in between fibers, the less the risk of fibrotic bridging and formation of a rigid and potentially dangerous scar plate encapsulating the mesh. Again, Ethicon had this critical mesh design information regarding the consequences in the human tissue of heavy weight, small pore meshes as a result of our university's cooperative safe mesh design research with them in the 1990's. This is evident in numerous depositions of Ethicon scientists.^{38, 39, 40, 41, 42}[Figure 6]

³⁸ Batke deposition 08/01/02 113:3 to 114:3, 172:6 to 174:15, 118:10 to 120:25

³⁹ Hellhammer deposition 09/12/13 403:18 to 404:9; 407:13-23

⁴⁰ Holste depositions 07/29/13 51:3 to 53:6; Holste Deposition 12/14/12 89:20 to 90:21

⁴¹ Semin Immunopathol (2011) 33:235-243 - a Scar net formation following large pore (~3 mm) and b scar plate formation following small-pore (~0.3 mm) mesh implantation

⁴² Arnaud deposition 9/25/13 756:9 to 757:8

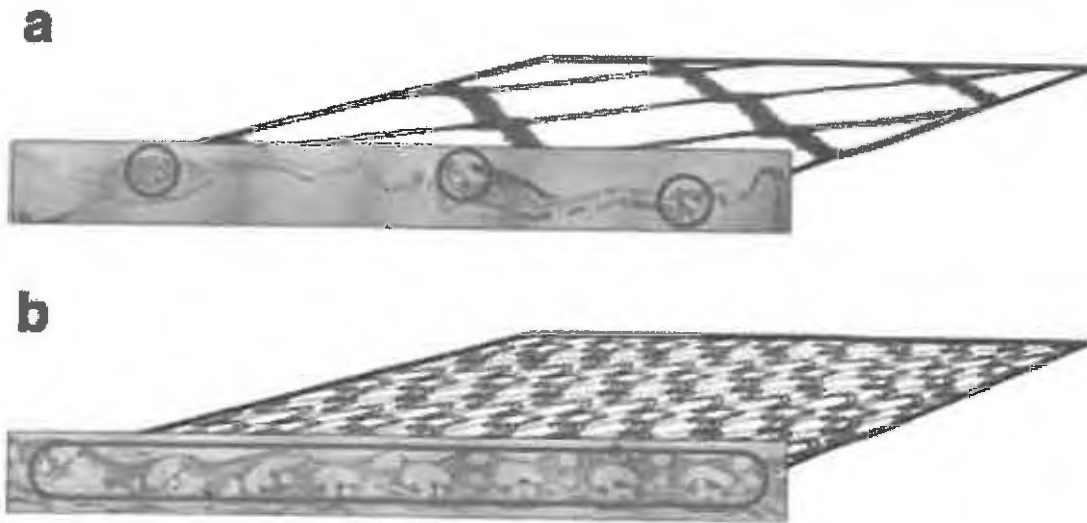


Figure 6

A rather infamous DVD produced by Ethicon and featuring an Ethicon consultant and fellow hernia surgeon, Dr. Todd Heniford, was shown at conferences and seminars in the late 2000's. Ethicon was involved in the production of that DVD as evidenced by the cover of the DVD and their name at the end of it.⁴³ That DVD touts the benefits of lightweight, large pore meshes and, importantly, describes the dangers of heavy weight, small pore meshes.⁴⁴ Dr. Heniford uses slides in the DVD that are from his published literature with his colleague, Dr. William Cobb that has been referenced in numerous Ethicon documents, PowerPoint presentations, professional education materials, expert meetings and Clinical Expert Reports.^{45, 46, 47, 48}

At one point in the DVD, published with an Ethicon/JNJ logo from 2007, Dr. Heniford states that with the advent of lightweight, large pore meshes "there really is not a reason to use heavyweight polypropylene in the human body...to say well this is the mesh I've always used is not an excuse to continue to use it." ". Ethicon internal documents by Joerg Holste and Boris Batke indicate Ethicon's awareness of this DVD and its concern that Prolene is very similar to the Marlex shown in the DVD.^{49, 50}

In the work of Dr. Cobb, the weight of TVT Prolene is listed as one of the heaviest weighted mesh. Ethicon cites to this work repeatedly. The Prolene mesh in TVT is Ethicon's oldest, heaviest weight, smallest pore polypropylene mesh; yet to this day, Ethicon continues to sell it in all of their currently-marketed TVT products. Although Ethicon now claims that the Prolene

⁴³ B. Todd Heniford 2007 "The benefits of lightweight meshes in Ventral Hernia Repair in Ventral Hernia Repair" Cover

⁴⁴ B. Todd Heniford 2007 "The benefits of lightweight meshes in Ventral Hernia Repair in Ventral Hernia Repair" Video

⁴⁵ ETH-47802 Cobb WS, Burns JM, Peindl RD, Carbonell AM, Matthews BD, Kercher KW, Heniford BT *Textile analysis of heavyweight, mid-weight, and lightweight polypropylene mesh in a porcine ventral hernia model*. J Surg Res. 2006 Nov;136(1):1-7. Epub 2006 Sep 22.;

⁴⁶ ETH.MESH.01424029 Cobb W, Kercher K, Heniford T. *The Argument for Lightweight Polypropylene Mesh in Hernia Repair*. Surgical Innovation. 2005; 12(1):T1-T7;

⁴⁷ ETH.MESH.08315779 Piet Hinoul Clinical Expert Report Gynecare Prolift +M Pelvic Floor Repair;

⁴⁸ ETH MESH.00237968 "R&D Perspective - The Journey from Prolift to Prolift +M" PowerPoint by Cliff Volpe

⁴⁹ ETH.MESH.05479411 Heavyweight to Lightweight Meshes PowerPoint

⁵⁰ ETH.MESH.05918776 2004 email re Marlex Experience

mesh in the TVT is “lightweight”, it is clear from the testimony from one of their lead scientists that the mesh is heavyweight.⁵¹ In their depositions, Ethicon employees have acknowledged that they knew that the heavy weight, small pore mesh in TVT Prolene mesh can lead to an increased risk of a greater FBR, more intense and chronic inflammatory response, shrinkage or contraction of the mesh, nerve entrapment in the pelvic tissues, erosions and chronic pelvic pain.^{52, 53, 54}

Ethicon has used its “Old Construction” 6 mil Prolene hernia mesh (first marketed in 1974) in all of its TVT meshes since the original TVT was launched in 1998.⁵⁵ Axel Arnaud, the Medical Director of Ethicon France acknowledged that the Prolene mesh used in TVT products has never changed.⁵⁶ It is my opinion, to a reasonable degree of medical and scientific certainty, that the weight and the distance between the mesh fibers of the “Old Construction” 6 mil Prolene hernia mesh causes a greater FBR and more intense inflammatory response in human tissues than lighter weight meshes with greater distance between the fibers, making it more susceptible to fibrotic bridging, scar plate formation and encapsulation of the mesh in scar tissue leading to a cascade of harmful reactions in human tissue, including pelvic tissues, thus unnecessarily increasing the risk of injury to women.

A number of Ethicon employees have testified that they became aware of the lightweight large pore concept by 1998 through Ethicon’s collaboration with both Dr. Bernd Klosterhalfen and me during the development of Vypro.⁵⁷ Numerous Ethicon internal documents demonstrate the Ethicon was acutely aware of the heavyweight, small pore

problem.^{58, 59, 60, 61, 62, 63, 64, 65, 66, 67, 68, 69, 70} Ethicon employees have also admitted that the Prolene mesh used in TVT products was heavyweight and small pore mesh.^{71, 72}

A decision was apparently made in 1998 to change the TVT Prolene mesh construction. In 1998, Ethicon indicated that its “long-term desire [was] to support the PHS [Prolene Hernia System] and TVT devices with the new construction material.”⁷³ [Emphasis added] Ethicon seemingly planned from the time of the launch of TVT to replace the “Old Construction 6 mil”

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⁵¹ Hellhammer deposition 09/11/13 156:15-23

⁵² Batke deposition 08/01/13 87:12 to 88:10, 113:3 to 114:3, 257:23 to 259:13

⁵³ Holste deposition 07/29/13 51:3 to 53:6, 55:22 to 57:4

⁵⁴ Vailhe deposition 6/20/13 182:2 to 185:5

⁵⁵ Holste deposition 7/29/2013 38:21 to 40:15; Batke deposition 08/01/2013 103:11 to 104:21

⁵⁶ Arnaud deposition 07/19/2013 37:7 to 40:10

⁵⁷ Batke deposition 08/01/12, 113:3 to 114:3, 172:6 to 174:15, 118:10 to 120:25; Hellhammer deposition 09/11/13 57:16 to 59:16; Hellhammer deposition 09/12/13 550:1 to 550:14; Holste depositions 07/29/13, 51:3 to 53:6; Holste Deposition 12/14/12, 89:20-90:21; Arnaud deposition 09/25/13 756:9 to 756:19

⁵⁸ ETH.MESH.04037600 Innovations in mesh development ETH.MESH.01782867 “Factors Related to Mesh Shrinkage” by Kerstin Spychaj

⁵⁹ ETH.MESH.05920616 7/20/07; Chomiak, Martin to Batke, Boris; Jamieson, Gillian; Koehler, Petra; Hellhammer, Dr. Brigitte SUBJECT: Defining light weight mesh

⁶⁰ ETH.MESH.05585033

⁶¹ ETH.MESH.05446127 3/13/2006 Holste, Dr. Joerg to Engel, Dr. Dieter; Manley, Quentin; Storch, Mark L. SUBJECT: AW: Mesh and Tissue Contraction in Animal

⁶² ETH.MESH.05475773

⁶³ ETH.MESH.04015102 3/01/12 Batke, Boris to Mayes, Casey SUBJECT: AW: AGES Pelvic Floor Conference-Gala Dinner Invitation

⁶⁴ ETH.MESH.04037600 Mesh Innovations PowerPoint

⁶⁵ ETH.MESH.09651393 Invention Disclosure;

⁶⁶ ETH.MESH.05585066 “Ultrapro” Powerpoint presentation by Boris Batke;

⁶⁷ ETH.MESH.05916450 “Chronic Pain Prevention future – Bioengineer’s point of view”

⁶⁸ ETH.MESH.04037600 “Innovations in Mesh Development” PowerPoint presentation by Boris Batke;

⁶⁹ ETH.MESH.00237968 “R&D Perspective – The Journey from Prolift to Prolift +M” PowerPoint presentation by Cliff Volpe;

⁷⁰ ETH.MESH.01203957 The Future of surgical meshes: the industry’s perspective PowerPoint by Piet Hinoul

⁷¹ Hellhammer deposition 09/12/13 550:1-14

⁷² ETH.MESH.05479535

⁷³ ETH.MESH.09264884

mesh with a new mesh construction; however, they delayed making these improvements as stated below:

Product's improvements

In order to meet our objective and launch TVT on October 30th, 1997, we decided to simplify our activity both at manufacturing and development level.

As we have moved ahead in our European activity, we have in fact realised that product improvement is not a major issue in Europe.

Anyhow, we recognise that some amendments are desirable and therefore are going to work on a second generation product to be released 1 Q99.

Following changes will be made:

- **new construction Prolene* mesh to be used (after clinical test by Prof. Ulmsten and Prof. Nilsson - 40 patients with 6 months follow-up)**

- 5 mm needles instead of 6 mm (width)

- shiny surface of needles (instead of opaque) to provide "slim" effect

- new shrinking tube (transparent) for needle-tape swaging

- blister pack

Manufacturing and operations will be followed up during 1998, so as to ensure release of second generation product 1 Q99.⁷⁴ [Emphasis added]

Unfortunately for patients, Ethicon chose not to replace its "Old Construction 6 mil" Prolene mesh in its TVT products but rather, chose to use the same mesh they had been marketing since 1974, without regard to critical design developments and considerations that they had studied, developed and were ready to launch.

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It is my opinion, to a reasonable degree of medical and scientific certainty that the smaller the distance between the fibers of a mesh implant, the greater the risk of scar tissue forming in the pores ("bridging fibrosis" or "fibrotic bridging"). As early as 1998, and certainly by the early 2000's, Ethicon had critical design information that the risk of bridging fibrosis is increased by surgical mesh with pore size less than 1mm in all directions, which in turn increases the risk of a rigid scar plate forming throughout the mesh, leading to integration of the entire mesh in scar tissue. Any pelvic mesh designed with pores this small unreasonably and unnecessarily increases the risk of injury to the patient and is a less safe design than mesh with greater distance between the fibers.

It is also my opinion, to a reasonable degree of medical and scientific certainty, that Ethicon's failure to implement new, critical mesh design changes (lighter weight, larger distance between the fibers) in its TVT products before its launch in 1998 was unreasonable, compromised patient safety and has led to patient complications like chronic inflammatory reaction, excessive scarring through and around the mesh, nerve entrapment, chronic pain, dyspareunia, erosions, recurrence and the necessity of reoperation in an attempt to correct these problems. The Prolene mesh in Ethicon's TVT products is unsuitable for use as a permanent implant for treatment of a woman's stress urinary incontinence.

⁷⁴ ETH.MESH.10183005

D. Pore Deformation

In approximately 2005, I applied for and received a grant to study the porosity of textile meshes in an attempt to objectify porosity in a reproducible manner. Working with an engineer at the FH Aachen University of Applied Sciences, Prof Thomas Muehl, we published the results of this granted project in 2008 in the Journal of Biomedical Materials Research Part B: Applied Biomaterials.⁷⁵

Our research was based on my research since the late 1990's that pore sizes that prevent fibrotic bridging and will permit ingrowth of physiological tissues should exceed 1 mm between two polypropylene filaments. As stated in our publication, "To exclude large pore areas that may be provided by long and thin pores with narrow parts of pores, the pore geometry has to be evaluated as well. Therefore, only those pores and those parts of the pores are extracted, which have dimensions greater than 1mm or 1000 μ m in all directions. The remaining porosity is defined as 'effective porosity'".

We published two additional studies of the pore size/porosity of surgical meshes in 2013 and 2014 based on our 2008 work which studied and analyzed Ethicon's Prolift and Prolift +M pelvic organ prolapse meshes.^{76 77}

An Ethicon R&D Scientist, Vincenza Zaddem, Team Leader of Prolift +M and Technical Lead of Prolift, was shown the Muehl study from 2007 and she testified that it sounded like a valid test and that she believed that it would be a good test for Ethicon to look into in order to determine the effective porosity and effective porosity under strain of their pelvic meshes.⁷⁸ This was again confirmed in testimony by another Ethicon employee, Joerg Holste and circulated numerous times within Ethicon as a "more sophisticated set up" than Ethicon's method of porosity testing.^{79, 80, 81} Ethicon was also aware of the concept of "effective porosity" and the necessity of maintaining pore sizes of >1mm after stretch.^{82, 83, 84, 85, 86, 87} [Figure 7]

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⁷⁵ Muehl T, Binnebosel M, Klinge U, Goedderz T. New Objective Measurement to Characterize the Porosity of Textile Implants. J Biomed Mater Res Part B: Appl Biomater. 2007; 84B:176-183

⁷⁶ J. Otto, et al., Elongation of textile pelvic floor implants under load is related to complete loss of effective porosity, thereby favoring incorporation of scar plates; J Biomed Mater Res A. 2013 Apr 29

⁷⁷ Klinge, U., Otto, J., Muehl, T. (2014) High Structural Stability of Textile Implants Prevents Pore Collapse and Preserves Effective Porosity at Strain

⁷⁸ Zaddem deposition 03/28/12, 387:14 to 387:20

⁷⁹ Holste deposition 10/9/2013, 417:9 to 418:22

⁸⁰ ETH.MESH.02184130 2008 email circulating New Objective to Characterize the Porosity of Textile Implants

⁸¹ ETH.MESH.04945136 2010 email circulating New Objective to Characterize the Porosity of Textile Implants

⁸² ETH.MESH.03021946 T-Pro Stage Gate Meeting on August 25, 2008

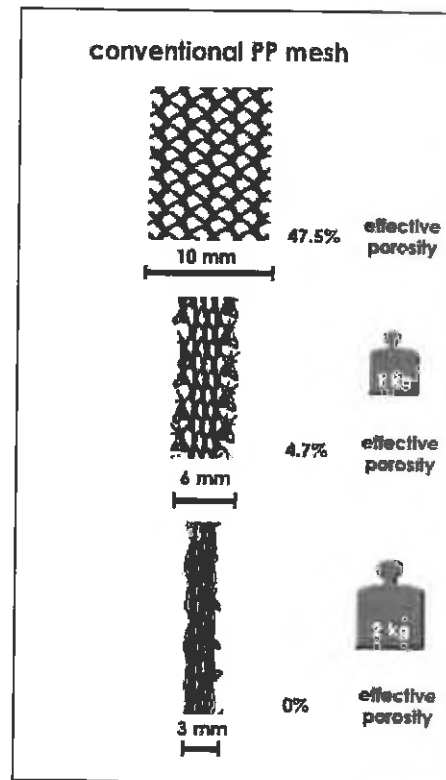
⁸³ ETH.MESH.02587926 When the Implant Worries the Body

⁸⁴ ETH.MESH.01752532: Mesh Design Argumentation Issues

⁸⁵ ETH.MESH.01785259 January 17, 2010 Email re; +M relaxation

⁸⁶ ETH.MESH.02587925 "When the implant worries the body" PowerPoint presentation

⁸⁷ ETH.MESH.02185582 "Biomechanical Considerations for Pelvic Floor Mesh"

Figure 7⁸⁸

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Ethicon estimates that its TVT slings will encounter elongation or stretch once placed in a woman's body up to 50%.⁸⁹ In other Ethicon internal documents, Ethicon estimates the in vivo forces placed on its TVT slings will be approximately 1N.⁹⁰ In other Ethicon documents, Ethicon scientists quote the intra-abdominal pressures as follows:⁹¹

- Standing: 23cm H₂O
- Lifting 5kg: 22 cm H₂O
- Valsalva: 79 cm H₂O
- Coughing: 96 cm H₂O
- Bearing down: 102 cm H₂O

Moalli et al. cited our published work in 1999 that "forces applied to mid-urethral slings in vivo is estimated to be in the range of approximately 5 to 15 N or 1.1 to 3.4 lbs."⁹²

When developing the protocol for testing the TVT meshes, I determined the uniaxial forces that would be placed on the mesh using the following assumptions:

⁸⁸ ETH.MESH.03021946 T-Pro Stage Gate Meeting 8/25/08

⁸⁹ ETH.MESH.00541379 Memo to File from Martin Weisberg re: Mesh Fraying to TVT Devices; ETH.MESH.00584811

⁹⁰ ETH.MESH.00584491 2006 email re AFNOR standards; ETH.MESH.01219414: Elongation Characteristic of Laser Cut PROLENE Mesh for TVT; Smith deposition 08/21/2013, 587:22 to 588:23

⁹¹ ETH.MESH.05237872 "Mesh Properties – How important are they?" by Peter Meier

⁹² Moalli P., Papas, N., Menefee S., Albo, M., Meyn, L., Abramowitch, D., Tensile properties of five commonly used mid-urethral slings relative to TVT *Int Urogynecol J* (2008) 19:665-633

• In contrast to flat meshes without tensile stress, narrow slings may be considered to work as ligaments having to withstand uniaxial strain.⁹³ This is undisputable for the process of implantation and the early postoperative time. To mimic the mechanical strain in this phase, we applied strain to the mesh in an uniaxial setting;

• The strain applied should cover the forces and the elongation that can be assumed to be relevant;

• Forces were related to the width of the sling, and thus N/cm was used for comparison with estimated membrane tensions;

• Membrane tension of 16 N/cm was calculated as requirement for the abdominal wall. As the diameter of the pelvis is less than a half of the abdominal wall, the membrane tension should be less than half;⁹⁴

• Experimental studies by DePrest et al resulted in a membrane tension of 2 to 5 N/cm as strain to be expected in the pelvic floor, 1 N/cm in non-prolapsed tissues;

• The tensile strain in the pelvic floor is expected to lead to an elongation of the textile. An elongation of up to 20% is considered to form the comfort zone, and elongation of 40% defines the safety zone;⁹⁵

• The tensile force during implantation procedure of a pelvic mesh is considered to be up to 30 N,⁹⁶ and correspondingly, the in vitro simulation should have less tensile strength;

• The intra-abdominal pressure to the pelvis is estimated by Janda to be 8.3 kPa, whereas an intra-abdominal pressure of 20 kPa is estimated to stress the abdominal wall to 16 N/cm - a lower intra-abdominal pressure leads to a lower tensile load. Considering the lower diameter of the pelvis, a mechanical load of less than 10 N/cm would be reasonable;⁹⁷

• Pullout force is considered by Ethicon to be 1.6 N/cm (20% elongation; 164g = "physiological" load);⁹⁸

As a consequence, although the burst strength of Prolene is 91 N/cm⁹⁹, we applied forces of 1 to 10 N to the slings, which should cover an elongation of less than 50%; altogether, a range that is used in internal studies of Ethicon as well.¹⁰⁰

⁹³ ETH.MESH.04048515 at 8518: KOL Interview of Carl G. Nilsson

⁹⁴ ETH.MESH.02010834 "Biomechanical consideration for Pelvic floor mesh design" by Juergen Trzewik and Christoph Vailhe; ETH.MESH.04048515 Nilsson KOL interview; Trzewik deposition 09/18/2013 226:20-22, ETH.MESH.02227224 Thunder PowerPoint 05/09/2008

⁹⁵ ETH.MESH.02010834 "Biomechanical consideration for Pelvic floor mesh design" by Juergen Trzewik and Christoph Vailhe

⁹⁶ ETH.MESH.02588182

⁹⁷ ETH.MESH.04006021; ETH.MESH.02185596

⁹⁸ ETH.MESH.03658927

⁹⁹ Klosterhalfen B, Klinge U, Schumpelick V.; Functional and morphological evaluation of different polypropylene-mesh modifications for abdominal wall repair. *Biomaterials* (Dec 1998) 19(24):2235-46

¹⁰⁰ Moalli P, Papas N, Menefee S, Albo M, Meyn L, Abramowitch D; Tensile properties of five commonly used mid-urethral slings relative to TVT. *Int Urogynecol J* (2008) 19:655-663

Ethicon's biomechanical engineer, Juergen Trzewik's "Invention Disclosure" helped to further define our porosity testing parameters and protocols.¹⁰¹ In his Invention Disclosure, Dr. Trzewik wrote:

The physiological, mechanical boundary conditions can be separated into two main conditions. The comfort zone is defined by the load situation within the implant under normal physiological conditions.

Here, 'the main load of 2,5 kPa is delivered by the weight of internal organs 2,5 kPa

[1] S.Janda, "Biomechanics of the pelvic floor musculature." TU Delft, 2006. [2] K.K.O'Dell, A.N.Morse, S.L.Crawford, and A.Howard, "Vaginal pressure during lifting, floor exercises, jogging, and use of hydraulic exercise machines," *Int. Urogynecol. J. Pelvic. Floor. Dysfunct.*, vol. 18, no. 12, pp. 1481-1489, Dec.2007.

The material of the implant basic structure is designed to be characterized by a comfort zone of high elasticity at a low physiological load and a safety zone characterized by low elasticity at high loads. Both zones are separated by the construction of the yield point by tangential approximation of the stress strain curve for the zone of initial elongation and the slope of region of high stress. The yield point for vaginal tissue is considered to be between 10%-200% of area strain.

[1] C.Rubod, M.Boukerrou, M.Brieu, P.Dubois, and M.Cosson, "Biomechanical properties of vaginal tissue. Part 1: new experimental protocol," *J. Urol.*, vol. 178, no. 1, pp. 320-325, July 2007. [2] H.Yamada, *Strength of Biological Materials*. Baltimore: The Williams & Williams Company, 1970.

The stretch of vaginal tissue may exceed 300 % under certain conditions.

[3] J.M.Miller, D.Perucchini, L.T.Carchidi, J.O.DeLancey, and J.Ashton-Miller, "Pelvic floor muscle contraction during a cough and decreased vesical neck mobility," *Obstet. Gynecol.*, vol. 97, no. 2, pp. 255-260, Feb.2001.

The yield point is individually defined for the different structures of the implant (e.g., the arms of the implant are characterized with a lower yield point than the implant body). The material behaviour simulates the behaviour of tendon structures is described by a significantly reduced elasticity compared to the implant body .[H. Yamada, *Strength of Biological Materials*. Baltimore: The Williams & Williams Company, 1970] The yield point for the arms should not exceed 10 %.

The implant material is anisotropic and stretches differently in

¹⁰¹ ETH.MESH.09651393 Invention Disclosure

longitudinal and transversal direction. The yield point in the transversal direction exceeds the longitudinal direction between 100%-500%.

[1] C. Rubod, M. Boukerrou, M. Brieu, P. Dubois, and M. Cosson, "Biomechanical properties of vaginal tissue. Part 1: new experimental protocol," J. Urol., vol. 178, no. 1, pp. 320-325, July 2007. [2] H. Yamada, Strength of Biological Materials. Baltimore: The Williams & Williams Company, 1970.

Biomechanical features like increased flexibility are undesired during the surgical procedure of implant placement, to avoid any uncontrolled or undefined stretching of the implant during implantation. Pre-straining of the implant would change the mechanical properties of the implant. A temporary stress-shielding of the long-term implant is necessary during implantation and wound contraction.

[Y. Abramov, A. R. Webb, J. J. Miller, A. Alshahrour, S. M. Botros, R. P. Goldberg, G. A. Ameer, and P. K. Sand, "Biomechanical characterization of vaginal versus abdominal surgical wound healing in the rabbit," Am. J. Obstet. Gynecol., vol. 194, no. 5, pp. 1472-1477, May 2006]

The yield point of the implant is lower than <10% before absorption of the supporting stress shielding structure.

As a consequence of all this information, we performed measurements to 11 mm TVT and TVT-O slings at a strain of

- 102 g (0.9 N/cm)
- 164 g (1.5 N/cm)
- 250 g (2.2 N/cm)
- 500 g (4.5 N/cm)
- 1000 g (8.9 N/cm)

The significance of the Muehl method of testing these mesh products is that it provides useful data in terms of how a mesh will perform in use, particularly in regard to the risk of fibrotic bridging. The first most important observation from this testing was that the textile porosity, the textile porosity under strain, the effective porosity and the effective porosity under strain in TVT produced results that did not meet the most basic requirements that Ethicon had utilized since the late 1990's, early 2000's. As minimal strain was applied to the test sample, the geometric shape of the pores deformed and ultimately collapsed. This deformation led to even smaller pores that make the Prolene mesh highly susceptible to fibrotic bridging, encapsulation by a rigid scar plate and the array of potential complications that occur as a result of this inflammatory process.

Another significant observation during the porosity testing by Prof. Muehl and me was the "curling", sometimes referred to as "roping", that occurred in the TVT under minimal strain. As

strips of mesh begin to curl, the fibers become situated too close together enhancing the inflammatory response and leading to fibrotic bridging.

Yet another significant observation during the stretch testing in our publications was the “fraying” at the edges of the mesh which could be seen upon removal from the package but became markedly worse in the TVT mesh sample at minimal strain, especially in the mechanical cut slings. These frayed edges create an increased inflammatory process and increase the tendency for curling. As fraying occurs, mesh particles can be released into the tissue, increasing the local load with foreign body surfaces, and creating an even greater inflammatory response in the tissues. This will be discussed in more detail below in this report.

After being subjected to even minimal strain or tension, the TVT slings, frayed and demonstrated deformation of the pores; they also failed to return to their original or near-original geometric shape and design. This phenomenon of permanent elongation “is mostly due to a rearranging of the sling’s architecture and should not be confused with the traditional mechanics definition of plastic deformation of an elastic material.”¹⁰² It is my opinion, to a reasonable degree of medical and scientific certainty, that this permanent elongation of TVT slings leads to permanent pore deformation or collapse and increases the risk of an enhanced inflammatory reaction in the human tissues and thus increases the risk of excessive scarring and the cascade of events related to an enhanced and chronic inflammatory response. It was determined in 2009 by Ethicon that Prolene mesh in its TVT products would distort irreversibly at 164 grams of force.^{103, 104} This irreversible damage would lead to the series of events that are known to occur with permanent distortion or deformation.

Ethicon’s biomechanical engineer, Juergen Trzewik, proposed various ideas to prevent pore collapse in Ethicon’s pelvic floor meshes; however, Ethicon never utilized these or other design changes to reduce the risk of pore collapse and deformation in its TVT meshes. [Figure 8 and 9]

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¹⁰² Moalli P., Papas, N., Menefee S., Albo, M., Meyn, L., Abramowitch, D., *Tensile properties of five commonly used mid- urethral slings relative to TVT*. Int Urogynecol J (2008) 19:665-633

¹⁰³ ETH.MESH.00345806 2009 email re Preclin

¹⁰⁴ ETH.MESH.00072085 Final Report PSE Accession Number 05-0396 Project Number 67379

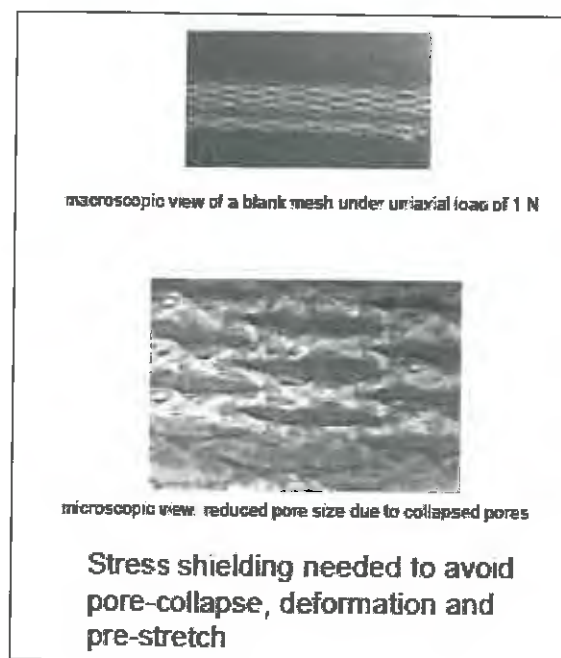


Figure 8¹⁰⁵

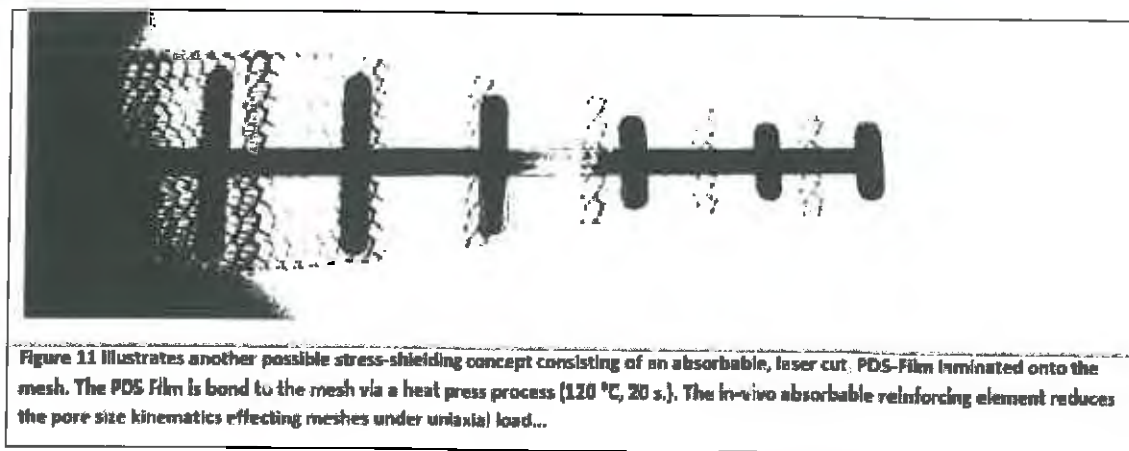


Figure 9¹⁰⁶

In a 2006 email discussing new French AFNOR standards for surgical mesh testing, a Senior Scientist at Ethicon, Gene Kammerer, while referencing the an article by Lin, et al., stated that “the article shows the maximum forces applied to the sling under the urethra is about 1N or 100 grams. So, for in vivo function (while the mesh is in the body) a force to elongate should correspond to about 1N”¹⁰⁷, which is in sharp opposition to the tensile forces withstood by the Prolene hernia mesh.

¹⁰⁵ ETH.MESH.02227224 MGPP Thunder Decision Meeting PowerPoint presentation

¹⁰⁶ ETH.MESH.02010849

¹⁰⁷ ETH.MESH.00584491 2006 email re AFNOR standards

In testing by Moalli et al. of the Ethicon TVT slings, they found in uniaxial testing that “the permanent elongation after C1 (ten cycles between 0.5 and 5 N or roughly 0.1 and 1.1 lbs.) of the Gynecare mesh was different from that of all the other samples tested. Gynecare samples permanently elongated by 17.5 +/- 4.2%, indicating that although very little force is applied, there is irreversible deformation of the TVT.” The study authors went on to state:

The most important finding of the paper is that Gynecare TVT mesh has a unique tensile behavior which is characterized by an initial region of very low stiffness in which the mesh easily elongates in response to small changes in force...As a result of this behavior, after cyclical loading at low loads...Gynecare mesh permanently elongated by more than 10% of its initial length, **confirming the easy permanent deformability of this mesh that is observed clinically during placement.**” (emphasis added)

The published testing by Moali, et al. of the TVT mesh is virtually identical in set up and results as our published testing of the TVT mesh. [Fig. 10 and 11)

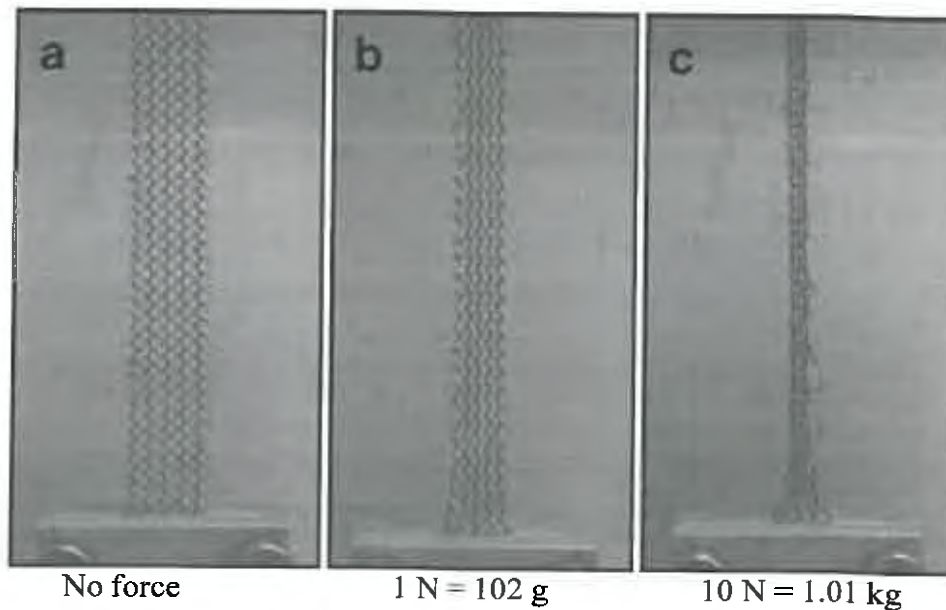


Figure 10¹⁰⁸

¹⁰⁸ Moalli P, Papas N, Menefee S, Albo M, Meyn L, Abramowitch D; Tensile properties of five commonly used mid-urethral slings relative to TVT. Int Urogynecol J (2008) 19:655-663

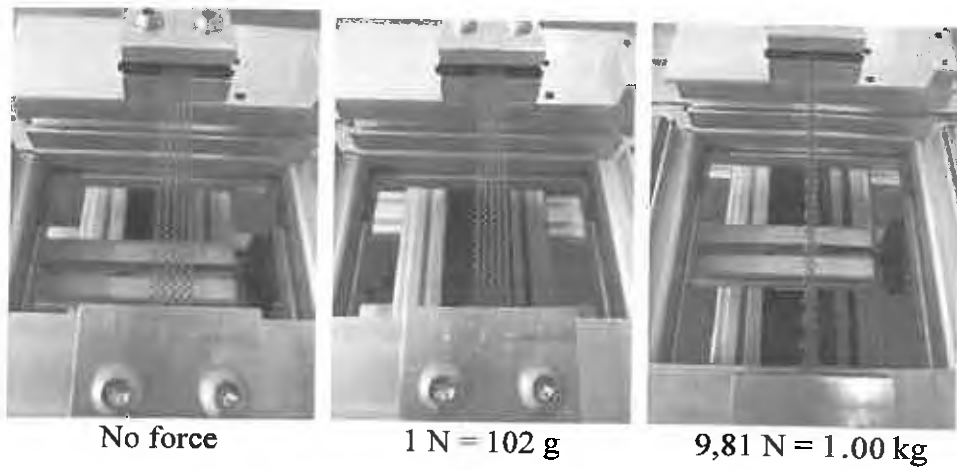


Figure 11¹⁰⁹



Figure 12¹¹⁰

¹⁰⁹ Images from the Expert report of Prof. Dr.-Ing Thomas Muehl

¹¹⁰ Moalli P, Papas N, Menefee S, Albo M, Meyn L, Abramowitch D; Tensile properties of five commonly used mid-urethral slings relative to TVT. Int Urogynecol J (2008) 19:655-663



1000 g → 8.92 N/cm

Figure 13¹¹¹

In his recent deposition, the Medical Director of Ethicon France, Axel Arnaud, states: “My understanding of this is there are two – normally two types of pores [in the TVT Prolene mesh], and when you pull on them, their size might change.” He also agrees that when tension is placed on the mesh that the pore sizes change.¹¹² Both Dr. Arnaud and another Ethicon Medical Director, Piet Hinoul have testified in this litigation that they respect my work and the work of my colleagues, including Dr. Klosterhalfen, and testified that we are highly qualified in this very specific field of biomaterials research on surgical meshes. In fact, Dr. Hinoul testified that he would defer to me as to whether the pores in Ethicon’s meshes collapse and deform under load and further stated that if Ethicon’s pelvic floor meshes do collapse and deform making them, in essence, microporous meshes, “Ethicon would not have wanted to sell that mesh.”^{113,114,115}

My opinion, to a reasonable degree of medical and scientific certainty is that a knitted surgical mesh device like the TVT that is permanently implanted in human tissue must be designed in such a manner that the pores of the mesh do not collapse and deform upon the expected forces of implantation as well as the expected in vivo forces. Under minimal strain, the TVT mesh pores deform and collapse thereby increasing the risk of injury to patients in which it is implanted and is a less safe design than products that better withstand these conditions and do not display these poor outcomes. Permanent deformation and pore collapse of the TVT mesh leads to fibrotic bridging, scar plate formation, excessive scarring through and around the mesh and a host of tissue complications that can lead to chronic pain, recurrence, erosions, dyspareunia

¹¹¹ Images from Expert Report of Prof. Dr.-Ing. Thomas Muehl

¹¹² Arnaud deposition 07/19/2013 108:17 to 109:11

¹¹³ Hinoul trial 01/16/16 1112:17 to 1114:4

¹¹⁴ Hinoul deposition 09/19/12 1054:9 to 1055:5; 1063:5 to 1065:11

¹¹⁵ Arnaud deposition 11/16/12 370:9 to 371:13; 373:20 to 375:2

and need for reoperation, to name a few, making it unsafe for its intended purpose of being permanently implanted in a woman's pelvic tissue.

E. Mesh Contraction

Mesh contraction, also known as mesh shrinkage, retraction, bunching or wrinkling, is a common phenomenon after mesh implantation that is closely related to scarring and fibrotic bridging. Mesh contraction can be defined by a reduction of the surface area of the original implanted mesh. The surface reduction is due not to shrinkage of the mesh fibers themselves but rather to a retraction of the fibrotic scar tissues around the mesh. Retraction of the mesh implant is a physiologic reaction of maturing scar that is characterized by a constant water loss and, consequently, a subsequent surface area decrease to an average of 60% of the former wound region. It is known to take place in the first few weeks after implantation but can last as long as 12 months or more after surgery. The medical literature and Ethicon's own internal documents report that there is considerable mesh contraction of surgical meshes made of polypropylene.^{116, 117, 118, 119, 120, 121, 122}

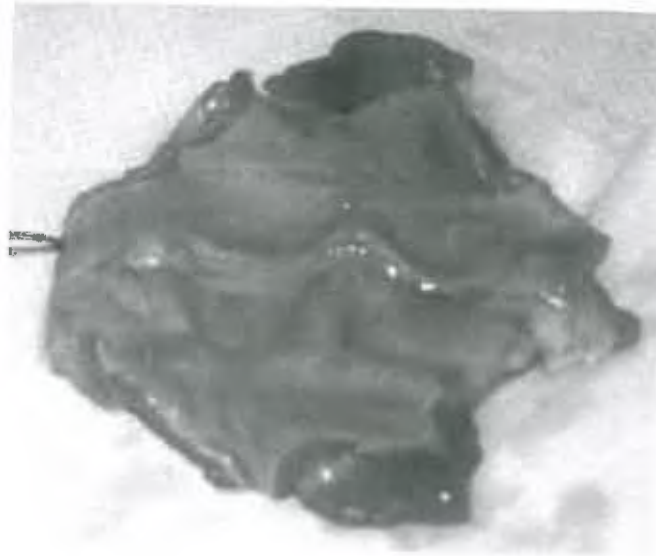
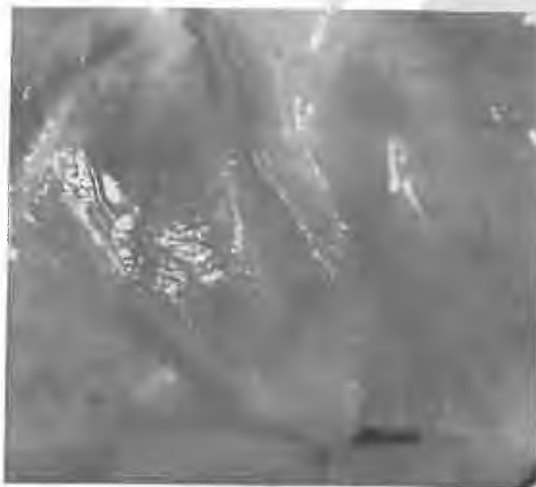


Figure 14¹²³

- ¹¹⁶ ETH-47802 Cobb WS, Burns JM, Peindl RD, Carbonell AM, Matthews BD, Kercher KW, Heniford BT Textile analysis of heavy weight, mid-weight, and lightweight polypropylene mesh in a porcine ventral hernia model. *J Surg Res.* 2006 Nov;136(1):1-7. Epub 2006 Sep 22.
- ¹¹⁷ Cobb W, Kercher K, Heniford T. The Argument for Lightweight Polypropylene Mesh in Hernia Repair. *Surgical Innovation.* 2005; 12(1):T1-T7
- ¹¹⁸ Tunn R, Picot A, Marschke J, Gauruder-Burmester A, Sonomorphological evaluation of polypropylene mesh implants after vaginal mesh repair in women with cystocele or rectocele. *Ultrasound Obstet Gynecol.* 2007 Apr;29(4):449-52.
- ¹¹⁹ ETH.MESH.01192895 Velemir L, Amblard J, Fatton B, Savary D, Jacquetin B, Transvaginal mesh repair of anterior and posterior vaginal wall prolapse: a clinical and ultrasonographic study. *Ultrasound Obstet Gynecol* (2010)
- ¹²⁰ Letouzey V, Fritel X, Pierre F, Courtieu C, Marès P, de Tayrac R. Informing a patient about surgical treatment for pelvic organ prolapse. *Gynecol Obstet Fertil.* 2010 Apr;38(4):255-60.
- ¹²¹ Vollebregt A, Troelstra A, van der Vaart C. Bacterial Colonisation of collagen-coated polypropylene vaginal mesh: Are additional intraoperative sterility procedures useful? *Int Urogynecol J.* 2009; 20:1345-1351
- ¹²² Klinge U, Klosterhalfen B, Muller M, Ottinger A, Schumpelick V. Shrinking of Polypropylene Mesh in vivo: An Experimental Study in Dogs. *Eur J Surg.* 1998; 164; 965-969
- ¹²³ Klinge U, Klosterhalfen B, Muller M, Ottinger A, Schumpelick V. Shrinking of Polypropylene Mesh in vivo: An Experimental Study in Dogs. *Eur J Surg.* 1998; 164; 965-969



Figure 15¹²⁴



Traditional polypropylene mesh. 90 days post-implantation. Fold development (in-vivo study)



Lightweight VYPRO II mesh. 90 days post-implantation. Fold-free incorporation (in-vivo study)

Figure 16¹²⁵

While developing its prolapse meshes, the TVM group in 2006 advised Ethicon of the common occurrence of retraction or shrinkage which then creates a “cord-like” mesh.¹²⁶ This issue not only leads to poor coverage leading to recurrence, but will also increase locally the amount of foreign body reaction due to pore collapse. This phenomenon then leads to additional complications depending from the location of the mesh including: pain, dyspareunia, nerve

¹²⁴ Costello CR, Bachman SL, Ramshaw BJ, Grant SA., Materials characterization of explanted polypropylene hernia meshes. J Biomed Mater Res B Appl Biomater. 2010 Aug;94(2):455-62

¹²⁵ Ethicon Products Worldwide – Tissue Reinforcement Solutions 2004

¹²⁶ ETH.MESH.01774758 December 2006 email regarding TVM Group mesh design input

entrapment, increased inflammation, urinary and fecal incontinence, urinary retention, blood vessel injury and others.

In referencing his internal Ethicon paper “Shrinking Meshes?”, Ethicon scientist Joerg Holste stated in an email on March 13, 2006 “this was our scientific statement on mesh shrinkage: Basically, small pores, heavy weight meshes induce more fibrotic bridging tissue reaction causing more mesh shrinkage during maturing of the collagenous tissue. See my presentation about biocompatibility.”¹²⁷ That email was in response to a string of internal Ethicon emails in which Ethicon employees were discussing their concerns over a study by Ramshaw in which polypropylene meshes actually shrank more than polyester.¹²⁸

In February of 2007, Dr. Kerstin Spychaj, Ethicon R&D prepared a presentation entitled, “State of the knowledge in ‘mesh shrinkage’ – What do we know?” which she presented at an Ethicon Expert Meeting on February 23, 2007 at Ethicon’s Norderstedt facility. Dr. Spychaj did a literature review and concluded that the “ideal mesh” in order to avoid shrinkage would be a lightweight material (partially absorbable) with a pore size > 1mm and mild but not excessive FBR and wound contraction with swift and adequate tissue growth.¹²⁹ Not only had Ethicon determined that shrinkage was obviously critical to the quality of its mesh products, they also stated that it could cause “vaginal anatomic distortion which may eventually have a negative impact on sexual function.” Furthermore, they stated that “its treatment is difficult.”¹³⁰ Several other Ethicon employees and/or consultants provided testimony or presentations regarding the issue of mesh shrinkage.^{131, 132, 133, 134, 135} The Prolene mesh in TVT is both heavyweight and has pore sizes <1mm in all directions, making it highly susceptible to harmful, painful contraction.

Johnson & Johnson hired an outside consulting firm named PA Consulting in 2010 to do a comprehensive and confidential analysis of its surgical meshes in order to look at the increased risk of erosions in its meshes. The final report was issued in June 2011.¹³⁶ As part of their investigation and study, PA Consulting interviewed both outside and in-house Ethicon experts. One such expert was Dr. Bernd Klosterhalfen, a KOL for Ethicon and consultant for 20 years. In his interview on January 18, 2011, Dr. Klosterhalfen informed PA Consulting and an Ethicon representative of many variables inherent in Ethicon’s meshes that lead to patient complications and failures of the devices.¹³⁷ Regarding the shrinkage of Ethicon’s meshes, Dr. Klosterhalfen restated what was known or should have been known for greater than a decade:

At the high level, there are two classes of “shrinkage” observed with mesh implant (Note: the term ‘shrinkage’ is a misnomer. Tissue reaction over time encapsulates the mesh with connective tissue and effectively ‘crushes’ the mesh into a ball (like crushing a sheet of paper); the mesh does not truly shrink):

¹²⁷ ETH.MESH.05446127 Email from Holste to Engel et al. re: Mesh and tissue contraction in animals

¹²⁸ ETH.MESH.05446127 Email from Holste to Engel et al. re: Mesh and tissue contraction in animals

¹²⁹ ETH.MESH.01218361-01218367: Dr. Kerstin Spychaj, State of the knowledge in “mesh shrinkage” – What do we know? 04/05/2007

¹³⁰ ETH.MESH.02992139 Lightning Clinical Strategy dtd 11/22/06

¹³¹ Robinson deposition 03/13/12, 260:5-22

¹³² Ciarrocca deposition 3/29/12, 340:9 to 340:12

¹³³ Kirkemo deposition 04/18/12, 105:14 to 108:16

¹³⁴ ETH.MESH.03924887 Meshes in Pelvic Floor Repair

¹³⁵ ETH.MESH.00870466 06/2/2006 Expert Meeting

¹³⁶ ETH.MESH.07192929 6/22/2011 PA Consulting “Investigating Mesh Erosion in Pelvic Floor Repair”

¹³⁷ ETH.MESH.07192412 PA Consulting meeting notes with Dr. Klosterhalfen

- The first is in the immediate short term following implant; the implant is observed to lift and may 'roll up' from its position. This occurs as a result of poor positioning, placement and/or suturing of the implant by the clinician

- The second class of shrinkage is the formation of scar tissue; observed in the longer term (months) following implantation. This scar tissue can reduce and compact, causing the mesh to crumple up.

That last quote is important because it documents what was known widely in mesh science and manufacturing industry since the 1990's; older, heavy weight, small pore meshes like the Prolene in Ethicon's TVT slings, increase the risk of mesh shrinkage or contraction – up to 50% of the area of the mesh. By this time in 2011, Dr. Klosterhalfen had received approximately 1,000 mesh explant samples over 10 years, and he and I had published a widely-circulated and discussed publication regarding our analysis of these 1,000 explants. He and I had also published a significant amount of peer-reviewed literature regarding explants, animal models and newer designs for more “ideal” meshes and had explained this phenomenon to Ethicon for many years as their consultants. Thus, in this interview, Dr. Klosterhalfen was simply restating what we had both studied in conjunction with Ethicon while researching safer mesh design with them since the early 1990's – all of their polypropylene meshes shrink from 30-50%, and the heavier the weight and smaller the distance between the fibers, the more this shrinkage phenomenon will occur.

It is my opinion, to a reasonable degree of medical and scientific certainty, based upon my background training and experience as a general and abdominal surgeon who used Prolene mesh for hernia repair in dozens of patients and treated Prolene-mesh-related complications in dozens of patients, and based on over 20 years of studying Prolene meshes, 10 years of which were as a consultant to Ethicon in developing safer mesh design and designing and carrying out their preclinical studies of Prolene and other surgical meshes, authoring or co-authoring numerous peer-reviewed publications regarding Prolene mesh, reviewing hundreds of internal Ethicon documents and hundreds of pages of deposition testimony that the mesh used in all of Ethicon's TVT sling products unnecessarily increases the risk of mesh shrinkage or contraction that in turn leads to an increased risk of intense and chronic FBR, severe and chronic inflammatory response, excessive scar formation, fibrotic bridging, increased risk of mesh encapsulation, scar plate formation, mesh shrinkage, nerve entrapment, chronic pelvic pain, erosions, chronic sexual dysfunction and dyspareunia, recurrence, inability to remove the device and need for painful and, at times, dangerous revision surgery and multiple, life-long, debilitating injuries in some women.

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F. Fraying/Particle Loss/Curling/Roping/MCM/LCM

As discussed above, it is known that the TVT tape frays under minimal tension. In fact, one of Ethicon's Medical Directors noted in a memo and testified that fraying is inherent in the design of the mesh.¹³⁸ In that memo to file, he stated “Fraying is inherent in the design and construction of the product. The mesh elongates in places; the mesh narrows in places; and small particles of Prolene might break off.” He also stated that the “stretching of the mesh increases the probability of fraying.”¹³⁹ In 2000, surgeons in the field advised Brigitte Hellhammer, an

¹³⁸ ETH.MESH.00541379 Memo to File dtd 11/18/03 from Martin Weisberg Re: Mesh Fraying for TVT Devices

¹³⁹ Id.

Ethicon employee, that Ethicon's surgical mesh "released particles that migrate through the vaginal wall causing pain during intercourse".¹⁴⁰

Then, in 2001, Dr. Alex Wang, who was described as "one of the most experienced TVT users in the world", informed Ethicon that he was having problems with frayed mesh and the uneven width of the sling.¹⁴¹

In November of 2003, Marty Weisberg, who at the time was the Senior Medical Director of Gynecare, made a note to the TVT file indicating that there had been 58 complaints of mesh fraying since 2000.¹⁴² Also in 2003, Pariente published a study in which he evaluated the amount of material shed by different suburethral slings under certain test conditions.¹⁴³ Dr. Pariente's conclusion was that "the very high particle shedding for both SPARC (AMS) and TVT (Ethicon) may be of significant long term clinical concern in some quarters." TVT had the highest percentage loss of initial weight at 8.5%. Other authors have commented on the fraying phenomenon of Ethicon's TVT slings as well.¹⁴⁴

The Pariente article then prompted the French regulatory agency, AFNOR to seek additional information from Ethicon regarding the high amount of particle loss. Ethicon Senior Scientist, Gene Kammerer believed that the method that AFNOR was requesting that they use in order to determine particle loss was unrealistic and too rigorous.¹⁴⁵ Kammerer, who is not a medical doctor, also stated that particle loss "is most likely an aesthetic issue".¹⁴⁶ However, information regarding the impact of particle loss on foreign body reaction and its clinical outcomes is concerning and required further study by Ethicon. These particles cause a greater risk for bacterial adherence¹⁴⁷ and increase the area of inflammatory response surrounding the implant in the tissues. There was insufficient medical and scientific data for this Ethicon scientist to simply state that there was no impact on clinical outcomes of this loss of particles without any scientific or clinical testing to support such a statement. Ethicon's Medical Director, Dr. Martin Weisberg, confirmed in his deposition that he was not sure whether or not particle loss and fraying would lead to clinical implications and did not know if Ethicon ever tested particulates for clinical implications.¹⁴⁸ One such implication was a report to Ethicon by a TVT surgeon whose patient had erosion into her vaginal wall following implantation with a TVT sling.¹⁴⁹ The patient's husband reported that during sexual intercourse the "tape appeared frayed and tiny fibers were protruding through the vaginal wall".

In 2004, Ethicon received clinical reports from other surgeons who were using their TVT products of this "crumbling" mesh problem. One of their surgical consultants informed the company that "it is embarrassing to see how the tape is crumbling" and it "gets worse if there is a

¹⁴⁰ ETH.MESH.03924557 Meshes in Pelvic Floor Repair

¹⁴¹ ETH.MESH.03905472

¹⁴² ETH.MESH.01126906

¹⁴³ ETH.MESH.01221055 Pariente J-L; An independent biomechanical evaluation of commercially available suburethral slings. Issues in Women's Health

¹⁴⁴ Moalli P, Papas N, Menefee S, Albo M, Meyn L, Abramowitch D; Tensile properties of five commonly used mid-urethral slings relative to TVT. Int Urogynecol J (2008) 19:655-663

¹⁴⁵ ETH.MESH.00583446 5/4/06 email from Gene Kammerer re French Regulatory and Particle Loss

¹⁴⁶ ETH.MESH.0058448 email re Urethral Sling particle loss standards and AFNOR

¹⁴⁷ Jongebloed WL. Doc Ophth 1986; 64:143, Sternschuss G J Urol 2012; May 12 epub, Clave A. Int Urogyn J 2010; 21:261

¹⁴⁸ Weisberg deposition 5/31/13, 469:23 to 470:16

¹⁴⁹ ETH.MESH.02622276 TVT Complaint

stretch on the tape". This Ethicon consultant, Dr. Eberhard stated "the quality of the tape is terrible" and "I can't understand that no one will solve the problem for such a long time".^{150, 151}

Austrian Ethicon surgical consultants had also reported problems with fraying and particle loss. An email in 2004 detailed the problem that a preceptor for TVT training in Austria was having when he "noticed that small blue particles kept falling off the mesh, as if the mesh was as he put it 'brittle'".¹⁵² The email states that "[s]ince our mesh is now blue, would it be possible that this was always the case but now it is simply visible as opposed to before the introduction of TVT Blue?" In a later email in that string, Dan Smith stated "I believe the board has to set a directive that can be filtered down to the reps, saying it's OK and it's not an issue, same as TVT clear except you can see it. By the way you can also see it in the package as the pieces fall out of the sheath splits!" He then sates what appears to be a pattern in Ethicon's reaction to reports from surgeons regarding problems with the TVT mesh: "This is not going away anytime soon and competition will have a field day, major damage control offensive needs to start to educate the reps and surgeons UPFRONT that they will see BLUE shit and it is OK."

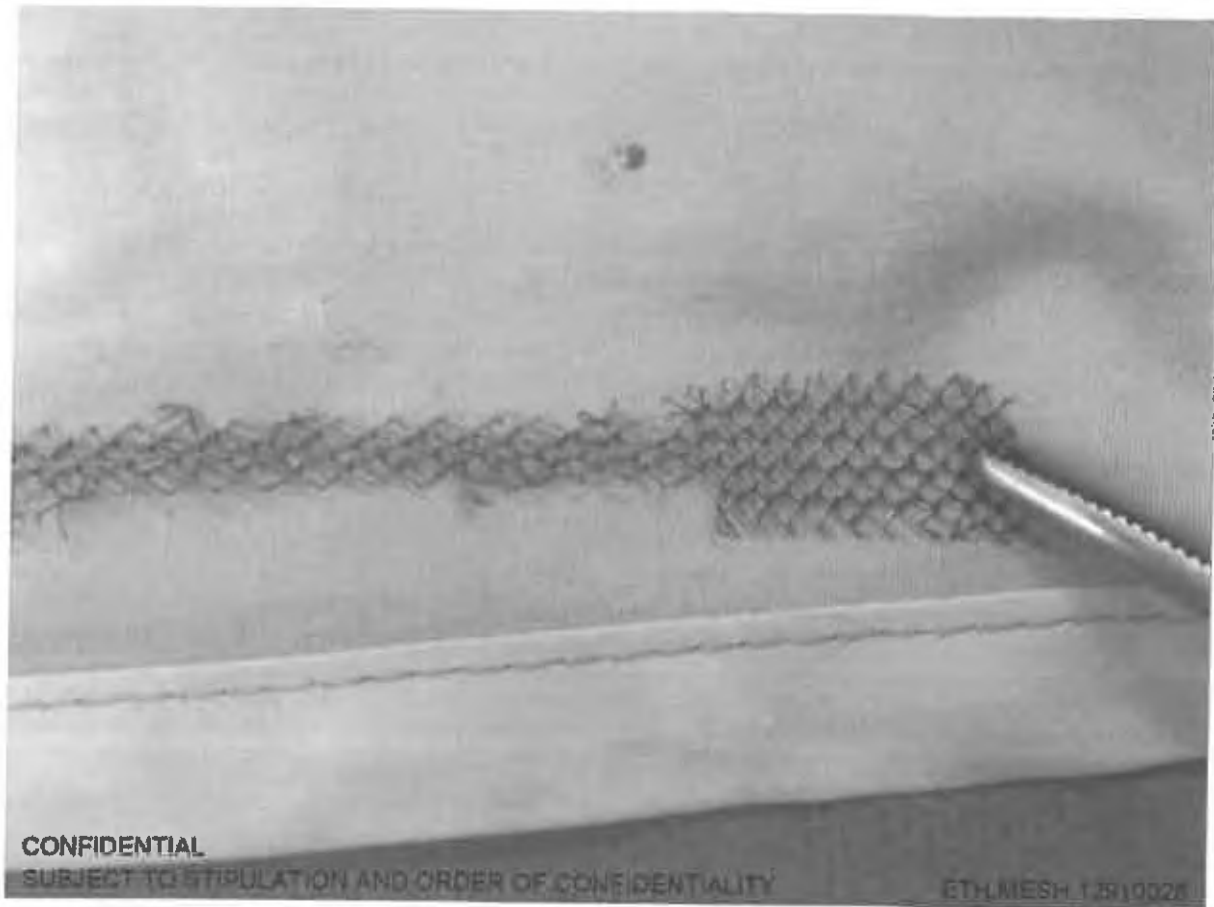
A Canadian KOL, in fact, the highest volume user of TVT in that country, Dr. Kenny Maslow complained to Ethicon about the fraying of their mesh down to a thin fiber even with "very little tension applied to the sling".¹⁵³

¹⁵⁰ ETH.MESH.02180833 Translation of Eberhard Letter

¹⁵¹ ETH.MESH.02180828 Eberhard complaint

¹⁵² ETH.MESH.06881079 Email from Dan Smith re Important: 2 TVT Complaints concerning allegedly brittle mesh

¹⁵³ ETH.MESH.12910023



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Figure 17¹⁵⁴

Correspondence indicates that Ethicon was attempting to move Dr. Maslow to the TVT-Abbrevio sling, which is only offered in laser cut mesh, and Dr. Maslow informed Ethicon that he was interested in laser cut edges for the TVT-O product as he was still having many of them “fry” down to a thin fiber sling with very little tension applied. This is consistent with feedback from surgeons in 2006, who told Ethicon that the TVT Laser cut mesh is smoother and has less rough edges than the mechanically cut TVT mesh.¹⁵⁵ One surgeon told Ethicon that the mechanically cut strips had fraying “hairs” on the edges that scratched with abrasive texture scraping like Scotch-brite pads. Multiple surgeons in 2006 told Ethicon that a rope-string effect could occur if force was applied to the mechanically cut mesh, just as Dr. Maslow experienced and documented with photographic evidence in 2013. Ethicon also received feedback from customers and regulators that the edges of the TVT mesh appear to be sharp and likely to cut tissue.¹⁵⁶

¹⁵⁴ ETH.MESH.12910023

¹⁵⁵ ETH.MESH.06696589

¹⁵⁶ ETH.MESH.00330760

While Ethicon employees such as Gene Kammerer believed this fraying and particle loss to be “an aesthetic issue”, actual TVT surgeons, including Ethicon consultants, obviously believed differently. However, Ethicon chose to continue to sell their TVT mesh as it was with no design changes to address the problem. Instead, members of the sales and marketing team at Ethicon were instructed to tell doctors that “Prolene is proven to be inert”; that “the particles will not cause any problem”; and that the sales representatives should be “proactive” because “the competition will try to target this!”¹⁵⁷ Ethicon’s position during this time was that the particles were not reactive and created no risk to patient safety.¹⁵⁸

MCM/LCM

In 2005, Ethicon attempted to address the problem of the fraying of TVT mechanical cut mesh (“MCM”) by instituting a new method of cutting its TVT mesh called laser cutting (“LCM”).¹⁵⁹ At first, Ethicon’s design engineers evidently felt that testing for critical design considerations like particle loss, flexural rigidity and elongation at various forces was not “critical to quality” and stated this in internal documents as “!!!!GREAT NEWS FOR TVT LASER CUT MESH!!!!” and “less work for all of us.”¹⁶⁰ Ethicon had evidently determined that although there was greater particle loss with MCM, their test results showed that the difference was not significant enough to be concerned.¹⁶¹

The 2006 Clinical Expert Report for TVT LCM indicated that LCM had decreased particle loss from MCM and that this “decrease would lead to less non-functioning material left in the tissues”.¹⁶² There simply is no patient benefit to excess, “non-functioning” polypropylene in a woman’s pelvic tissues. More fibers migrating in the tissues create an additional foreign body reaction and inflammatory response at the site of each piece of TVT mesh fiber in the body causing an increased risk of harm to patients, including chronic pain.

Ethicon considered the hazards and resulting harms in a woman’s pelvic tissue due to roping, rough/frayed edges, pore deformation and other possible design failures of the TVT device in its dFMEA for LCM in 2006.¹⁶³ Ethicon admits that one of the primary functions of performing a harms/hazards design risk assessment is patient safety.¹⁶⁴ The Medical Affairs Director for the dFMEA, David Robinson, testified that these were in fact the considerations by the Ethicon team charges with completing the dFMEA.¹⁶⁵

In elongation studies conducted by Ethicon in 2004 comparing its MCM and LCM TVT meshes to competitor meshes, Ethicon used an Instron machine (using uniaxial forces) to stretch the meshes to 20% elongation.¹⁶⁶ Ethicon scientists concluded that “[c]utting the TVT mesh with

¹⁵⁷ ETH.MESH.00865322 email from Charlotte Owens re Reminder on Blue Mesh!

¹⁵⁸ ETH.MESH.03535750 Letter to Herve Fournier re TVT Device, Blue Mesh; ETH.MESH.00541379 Memo re Mesh Fraying to TVT Devices; ETH.MESH.00858252: Memo re Mechanical Cut vs. Laser Cut Mesh Rationale

¹⁵⁹ ETH.MESH.00301741 email from Daniel Lamont re !!!!Great News for TVT Laser Cut Mesh!!!!; ETH.MESH.00394544: Global Regulatory Strategy – GYNECARE TVT – Laser Cutting Project memo; Weisberg deposition 05/31/2013, 487:13 to 488:7

¹⁶⁰ ETH.MESH.00301741; Weisberg deposition 05/31/2013, 490:15 to 491:17

¹⁶¹ ETH.MESH.01219984 Completion Report for the Design Verification of TVT Laser Cut Mesh; ETH.MESH.00585842 Email from Gene Kammerer re TVT LCM – Particle loss

¹⁶² ETH.MESH.00167109 Martin Weisberg Clinical Expert Report: Laser Cut Mesh for TVT

¹⁶³ ETH.MESH.012180109 DFMEA

¹⁶⁴ Smith deposition 06/04/2013 654:1 to 655:20

¹⁶⁵ Robinson deposition 09/11/2013 1070:23 to 1072:25

¹⁶⁶ ETH.MESH.01809080 Comparison of Laser-Cut and Machine-Cut TVT Mesh to Meshes from Competitive Devices (BE-2004-1641)

a laser rather than a machine does not impact the established relationship between TVT and its competitors with regard to tensile behavior at low (20%) elongation.”

In 2006, Gene Kammerer performed comparisons of LCM to MCM.¹⁶⁷ He placed samples of LCM and MCM TVT mesh under strain to 50% elongation and found that the MCM samples showed “degradation of the structure of the mesh in certain areas where, because of particle loss, the knit has opened and a portion of the construction has been lost. The area may also be stretched and narrowed resulting in roping due to this occurrence.” The LCM sample also showed stretching and narrowing, “but is generally less than the MCM”. [Fig. 18]

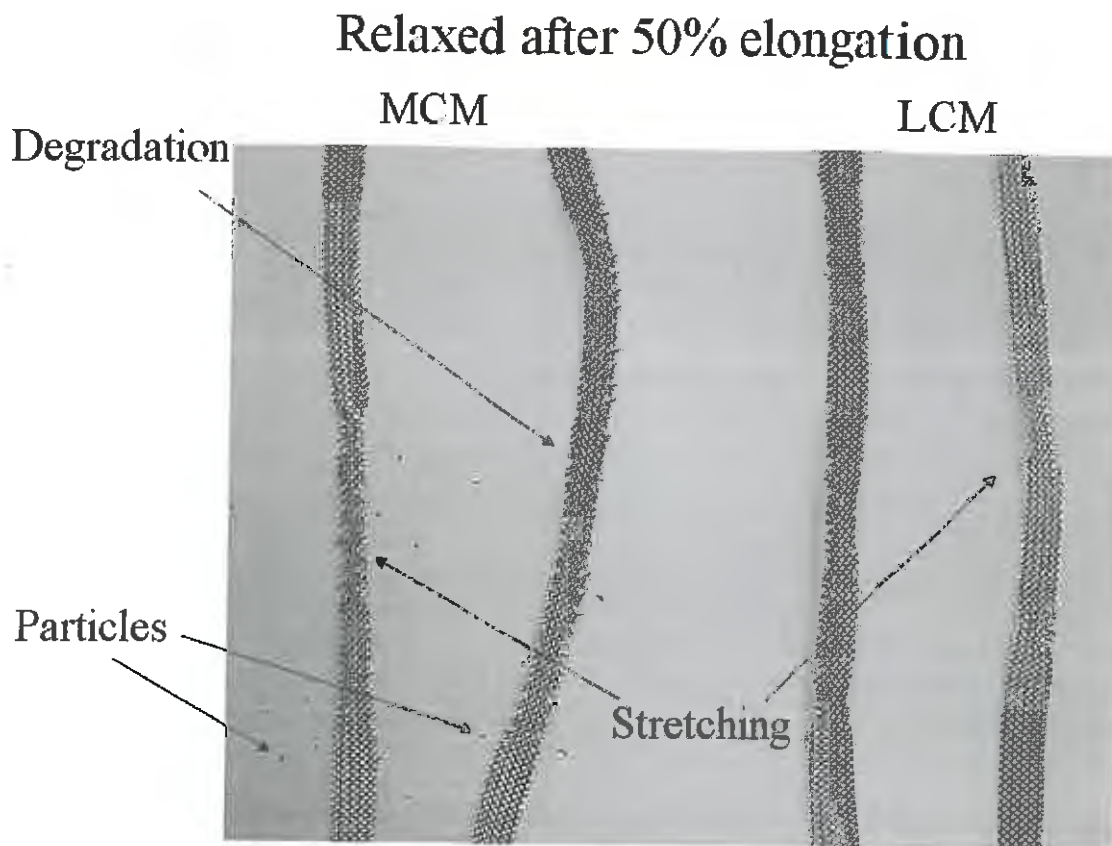


Figure 18

Mr. Kammerer stated in internal documents that according to his experience “viewing many surgical procedures and performing numerous procedures on cadavers myself, that the mesh stretches approximately 50% at the maximum”.¹⁶⁸

¹⁶⁷ ETH.MESH.08334244 email from Gene Kammerer re Photographs of LCM vs. MCM

¹⁶⁸ ETH.MESH.00584811

Ethicon Medical Affairs director, David Robinson, admitted at his deposition that the stiffer LCM TVT was intended to address the problems noted by Mr. Kammerer in his internal studies. He testified that “customers were expressing they wanted a change with the particle loss, roping, change in tension during sheath removal” and admitted that one of the goals of LCM was to prevent roping and that roping was due to the elasticity problem with MCM TVT.¹⁶⁹ Ethicon’s internal failure modes and analysis demonstrated that the potential for roping, curling and frayed edges could cause erosions, pain and recurrence.¹⁷⁰

Despite these internal test results and recognition of the problems associated with the Prolene MCM mesh utilized in the TVT devices, upon developing the LCM Prolene mesh, Ethicon continued to sell BOTH products simultaneously. In an internal Ethicon email dated May 6, 2005, Ethicon Product Director, Allison London Brown, stated “[t]he basic story here is that the current mesh (MCM) is perceived by some physicians as inferior and we do get a high number of complaints on linting [fraying]¹⁷¹ and roping (mesh particles falling off and the material stretching to the point of being a string). The new material will dramatically reduce the incident of linting [fraying] and should all but eliminate the roping as it stays nice and flat”.¹⁷² Ms. Brown asked for her Ethicon colleagues to help her “craft” a story for its TVT customers (surgeons) to “reduce confusion and complexity” and to “tell a nice story without overly admitting that the current procedure may some have perceived aesthetic problems (not clinically relevant problems).”

Other Ethicon employees had similar marketing strategies/concerns in mind. Ethicon U.S. Group Product Director, Kevin Mahar, in an email dated May 24, 2005 had this to say regarding positioning both TVT products in the market at the same time: “Positioning? While we would work with our agency to get this right, my thoughts are we KEEP selling regular TVT (the Colonel’s “Original Recipe”) to those customers that want/love it...and KEEP going forward with 8 years of data, etc. with the original recipe...we simply ADD these 2 LCM codes and if we have customers demanding LCM, we say, here you go! We do not mislead them that this is the same product, we simply say ‘...from the makers of TVT...the company ‘built’ on a tradition of trust, blah, blah, blah’”.¹⁷³ Earlier in that email string, Ms. Brown stated that the marketing strategists inside Ethicon had “some discussions on the Laser-cut mesh and the impact to base. Most definitely we need to understand how we globally utilize the material and take advantage of the new product, without detriment to the Base business.”

In other internal Ethicon emails, Dan Smith from R&D explains that the TVT and TVT-O meshes cause more urinary retention than its TVT-Secur product because the TVT and TVT-O products “curl and rope which reduces the surface area of the mesh under the urethra and therefore, increases the pressure in a localized point”.¹⁷⁴ At the deposition of yet another Ethicon employee, Dan Lamont, he confirmed Mr. Smith’s statements saying “[t]here is a potential for roping to occur on the TVT mechanically cut mesh” but “Ethicon chose to continue to sell mechanically cut mesh”.¹⁷⁵ The top complaint of TVT surgeons from 2003-2006 was

¹⁶⁹ Robinson deposition 07/25/2013 492:10 to 493:19

¹⁷⁰ ETH.MESH.01218019

¹⁷¹ Robinson deposition 07/25/2013 502:21-503:1

¹⁷² ETH.MESH.00526473 Email from Allison London Brown re Laser-Cut mesh

¹⁷³ ETH.MESH.00687819 Email from Kevin Mahar re Laser cut mesh

¹⁷⁴ ETH.MESH.01822361 Email from Dan Smith re TVT Secur

¹⁷⁵ Lamont deposition 09/11/2013 25:8 to 25:20; 35:19-36:4

“Mesh Fraying/Roping”.¹⁷⁶ (I have viewed an Ethicon TVT implantation DVD which confirms Mr. Lamont’s observations that even during the implant procedure, one can see the deformed pores and narrowing of the sling above the scissors and below the urethra while tensioning the sling intra-operatively).¹⁷⁷

It is my opinion, to a reasonable degree of medical and scientific certainty that the TVT mesh is a knitted textile design without a sealed border and therefore, it has frayed edges that tend to shed particles of polypropylene before, during and after the surgery. As tension is placed on the mesh, it curls, ropes and sheds these particles, all of which makes the TVT Mechanical-cut mesh (MCM) unreasonably and unnecessarily unsafe for its intended purpose of being permanently implanted in a woman’s pelvic tissues as an anti-incontinence device. The curled, frayed, sharp edges and the dislodged, migrating particles of the TVT MCM products increase the risk of increased inflammatory response, chronic foreign body reaction, erosions, chronic pelvic pain, failure of the implant, dyspareunia, organ damage, urinary dysfunction and the need for surgical intervention.

VI. SAFER ALTERNATIVE DESIGN

There are alternative design characteristics that would be safer in a woman’s pelvic tissues as a treatment for incontinence than some of the design characteristics of the Prolene mesh in TVT. One such safer alternative design would be a mesh product with less material and larger distance between the mesh fibers (Ethicon’s Ultrapro mesh has 3-5mm between the fibers and has a weight of 25 g/m²).

Another safer design would be a polymer that elicits a more favorable inflammatory response. PVDF, as a synthetic, non-absorbable suture or mesh material has improved textile and biological properties over polypropylene. It is thermally stable and more abrasion resistant than other fluoroplastics and induces a minimal cellular response, shows exceptional chemical stability and has excellent resistance to aging. PVDF sutures are routinely used in cardiovascular and orthopaedic surgery.¹⁷⁸

In 1998, with the support of Aachen University, I started a research project to develop a monofilament mesh made of pure PVDF, as it was suspected to be the best polymer available at that time. Ethicon supported our study by providing us with one of their PVDF meshes for testing in an animal experiment. Our study showed that the PVDF material had a better performance in the tissue than Prolene. The results were presented to Ethicon in 2001 and were published in 2002.¹⁷⁹ However, upon presenting the results to Ethicon, they rejected any further collaboration with our research group to develop meshes of PVDF with the comment that there was no interest by Ethicon to replace their polypropylene meshes with PVDF.

Despite telling me and our group that Ethicon had no interest in working with us to develop a PVDF surgical mesh, in 2000, Ethicon had received 510(k) clearance in the United States for a

¹⁷⁶ ETH.MESH.00302390 TVT-Base & TVT-O Review for Laser Cut Mesh (LCM) Risk Analysis

¹⁷⁷ ETH.MESH.PM.000004 TVT Retropubic Implantation Video

¹⁷⁸ Laroche G, Marois Y, Guidoin R. Polyvinylidene fluoride (PVDF) as a biomaterial: from polymeric raw material to monofilament vascular suture. *J. Biomed. Mater. Res.* 1995; 29:1525-1536

¹⁷⁹ PVDF as a new polymer for the construction of surgical meshes. Klinge U, Klosterhalfen B, Ottinger AP, Junge K, Schumpelick V. *Biomaterials.* 2002 Aug;23(16):3487-93

PVDF suture. The product name was "Pronova".¹⁸⁰ In 2002, Ethicon obtained a German patent No. DE 10043396C1 20.06.2002 for a PVDF surgical implant, including requirement of pore sizes of > 1.5 mm.¹⁸¹ The advantage of a PVDF device was explained by studies listed in the patent.¹⁸² Those studies, as well as some of which that I have published, have shown that this material has improved textile and biological properties.^{183, 184}

In an email from a top Ethicon German scientist in 2007 regarding internal reaction to recently-published literature concerning degradation of polypropylene meshes in human tissue explants, Dr. Dieter Engel stated, "What is the future? We will change the material of our mesh and move to Pronova as the future material platform for mesh...Pronova has a reduced foreign body reaction compared to Prolene, as shown in several animal studies, and will improve the perceived biocompatibility of our mesh. Besides, Pronova is much less susceptible to mechanical damage...it is much easier to process in the knitting machines, less quality issues."¹⁸⁵

Ethicon reveal that they funded internal studies to develop Pronova (PVDF) sutures as a prolapse mesh. They investigated this PVDF pelvic floor repair design concept through a new project dubbed by Ethicon as "Project Thunder". In the August 14, 2007 Project Thunder meeting minutes, Ethicon scientists reported the progress of the project and listed the pros and cons of Pronova to polypropylene as follows: Pro: Softness, Elasticity, better biocompatibility, less "aging"/long time breakage, easier to manufacture and sterilize. Con: "May be more expansive [sic]".¹⁸⁶ Other Ethicon documents also focused on the fact that Ethicon determined that PVDF would cost more than polypropylene.^{187, 188} In a May 9, 2008 Project Thunder presentation, one slide is particularly telling. It shows the PVDF products all out-performing Ethicon's polypropylene meshes in every design attribute except one...cost.¹⁸⁹ Project Thunder was "killed" by Ethicon despite the fact that at multiple meetings, it was described as the "holy grail" of pelvic floor meshes, the first "patient-centric" mesh, the first Ethicon mesh actually "designed for the pelvic floor" and explained that it would address the concern by Ethicon that its surgical meshes at the time that were all "overengineered".¹⁹⁰

It has been found in literature that polypropylene degrades and PVDF does not. This can be found in numerous articles, by numerous authors. Numerous other articles have demonstrated the superior benefits of PVDF in tissue.^{191, 192, 193, 194, 195}

¹⁸⁰ ETH.MESH.01819833 "Pelvic Floor Repair Platform" Slide 35

¹⁸¹ German Patent No. DE10043396C1 20.06.2002; Certified Translation of Patent

¹⁸² German Patent No. DE10043396C1 20.06.2002; Certified Translation of Patent

¹⁸³ Klinge U, Klosterhalfen B, Ottinger A, Junge K, Schumpelick V. PVDF as a new polymer for the construction of surgical meshes. *Biomaterials* 2002; 23:3487-3493

¹⁸⁴ Klink C., Junge, J., Binnebosel., Alizai, H., Otto, J., Neumann, U., Klinge, U. Comparison of Long-Term biocompatibility of PVDF and PP meshes. *Journal of Investigative Surgery* (2011); 24:292-299

¹⁸⁵ ETH.MESH.05447475 Email from Dieter Engel to John Gillespie et al. re How inert is polypropylene?

¹⁸⁶ ETH.MESH.00869908 Thunder Meeting Minutes dated 8/14/07

¹⁸⁷ ETH.MESH.02227224 PowerPoint Presentation dated 05/09/08 titled MGPP Thunder Decision Meeting

¹⁸⁸ ETH.MESH.00869908 Thunder Meeting Minutes dated 8/14/07

¹⁸⁹ ETH.MESH.02227224 PowerPoint Presentation dated 05/09/08 titled MGPP Thunder Decision Meeting

¹⁹⁰ ETH.MESH.00562421 untitled PowerPoint updated from November 2010-October 2011

¹⁹¹ Klink C., Junge, J., Binnebosel., Alizai, H., Otto, J., Neumann, U., Klinge, U. Comparison of Long-Term biocompatibility of PVDF and PP meshes. *Journal of Investigative Surgery* (2011); 24:292-299

¹⁹² Silva, R., Silva, P., Carvalho, M. Degradation Studies of Some Polymeric Biomaterials: Polypropylene (PP) and Polyvinylidene Difluoride (PVDF). *Material Science Forum* (2007); 593-543

¹⁹³ Conze, J., et al., New polymer for intra-abdominal meshes--PVDF copolymer. *J Biomed Mater Res B Appl Biomater*, 2008. 87(2): p. 321-8.

¹⁹⁴ Klinge U, Klosterhalfen B, Ottinger A, Junge K, Schumpelick V. PVDF as a new polymer for the construction of surgical meshes. *Biomaterials* 2002; 23:3487-3493

¹⁹⁵ Laroche G, Marois Y, Guidoin R. Polyvinylidene fluoride (PVDF) as a biomaterial: from polymeric raw material to monofilament vascular suture. *J. Biomed. Mater. Res.* 1995; 29:1525-1536

The characteristics of implanted polyvinylidene fluoride and polypropylene sutures used in vascular surgery were analyzed in 1998 by Celine Mary et al. They found that after periods of 1 and 2 years there was little to no sign of surface cracking of polyvinylidene fluoride whereas explanted polypropylene sutures showed visual evidence of surface stress cracking. The authors concluded that the PVDF likely has superior biostability to polypropylene over the long term.¹⁹⁶

Klink et al. compared the performance of PVDF and polypropylene meshes. The SEM data clearly suggests degradation on the part of polypropylene mesh with virtually none found in the PVDF mesh after implantation in rats. They concluded that PVDF meshes show low inflammation and mature scar formation after six months and that PVDF would be a possible alternative to polypropylene mesh implants.¹⁹⁷

In fact, even in Ethicon's own 7-year dog study, conducted in the late 1990's, it was found that after seven years, Ethicon's Prolene sutures showed progressive degradation, while PVDF sutures showed none.¹⁹⁸

Our published studies regarding the structural stability of meshes under various stresses in 2013 and 2014 have shown superior characteristics of mesh made of PVDF versus Ethicon's surgical meshes.¹⁹⁹ Overall, the alternative textile structure made of PVDF (product name "Dynamesh") showed remarkable effective porosity and high effective porosity persisting even under strain whether the measurements were taken in the center portion of the prosthetic or in the arm. It also showed roughly equivalent performance under strain whether being tensed in the warp or cross direction. In sum, Dynamesh showed excellent structural stability under tension and excellent effective porosity to resist fibrotic bridging. Another significant observation of the Dynamesh product is that unlike Prolift, Dynamesh has a smooth seam around the entirety of the mesh with no fraying at the edges nor curling in the arms under strain as was seen with both of the Ethicon products.

At his deposition, Dr. Holste was asked about Ethicon activities involving comparing their products to Dynamesh. According to Ethicon documents, they were examining Dynamesh's manufacturer, FEG's website and trying to determine if they could disprove any of FEG's claims regarding their meshes, including Dynamesh. Ethicon field representatives in Brazil were so concerned about the competition by Dynamesh sling products in that country that in 2009, they were sending emails regarding how to disparage FEG's product to keep them from using Dynamesh.²⁰⁰

Based on these characteristics, my studies comparing PVDF to polypropylene, Ethicon's internal documents and other scientific literature, as well as my background, training and experience over 30 years, it is my opinion, to a reasonable degree of medical and scientific

¹⁹⁶ Celine Mary, Yves Marois, Martin W. King, Gaetan Laroche, Yvan Douville, Louise Martin, Robert Guidoin, Comparison of the In Vivo Behaviour of Polyvinylidene Fluoride and Polypropylene Sutures Used in Vascular Surgery, *ASAIO Journal*, 44 (1998) 199-206

¹⁹⁷ C. D. Klink, K. Junge, M. Binnebosel, H. P. Alizai, J. Otto, U. P. Neumann, U. Klinge, Comparison of Long-Term Biocompatibility of PVDF and PP Meshes, *Journal of Investigative Surgery*, 24 (2011) 292-299.

¹⁹⁸ ETH.MESH.09557798 7 Year Dog Study

¹⁹⁹ Otto, J., Kaldenhoff, E., Kirschner-Hermanns, R., Muhl, T., Klinge, U. Elongation of textile pelvic floor implants under load is related to complete loss of effective porosity, thereby favoring incorporation in scar plates. Wiley Online

²⁰⁰ ETH.MESH.04066979 Email re Dynamesh in Brazil

certainty, that PVDF, in the appropriate design, is a safer alternative mesh material for treatment of stress urinary incontinence than Ethicon's TVT Prolene mesh.

I reserve the right to modify these opinions as necessary based upon any new or additional information or data that I may obtain or with which I am presented including, without limitation, any materials that I produce in response to Ethicon's requests.

VII. EXHIBITS

My current curriculum vitae is attached as Exhibit "A"

All exhibits that will be used to support my finding and opinions are included above and listed below in Exhibit "B"

VIII. RECENT TESTIMONY

I have testified as an expert at the following trials:

Linda Gross, et al. vs. Gynecare, et al.; Superior Court of New Jersey Law Division – Middlesex County Case No. MID-L-9131-08

Carolyn Lewis v. Ethicon, Inc., et al.; Southern District of West Virginia Charleston Division Case No. 2:12-cv-04301

Dianne M. Bellew v. Ethicon, Inc., et al.; Southern District of West Virginia Charleston Division Case No. 2:13-CV-22473

IX. COMPENSATION

I am compensated for investigation, study and consultation in the case at the rate of \$500.00 per hour.

This 24th day of August, 2015

Prof. Dr. Med. Uwe Klinge



EXHIBIT A

CV Professor Dr. med. Uwe Klinge

Born at 30.4.1959 in Wilhelmshaven, Germany

Primary, secondary, high school 1964-1977 Wilhelmshaven
Medical school 1977-1983 RWTH Aachen

Medical profession

12/1983 – 2/85: military service VKK 321, Düsseldorf

1.3.1985: surgical resident ship at the Surgical Department of the University Hospital at the RWTH Aachen (Head Prof. Reifferscheidt, after 12/85 Prof. Schumpelick, after 3/2010 Prof. Neumann)

1992: Thesis at the Department for biochemistry, Prof. Gersonde at 29.4.1985 „In-vitro investigation of the oxygen binding curve of human erythrocytes in the presence of glucose and insulin “

15.12.1993: Specialist for general surgery

since 15.10.1999: Oberarzt of the surgical Department

1/2000 Venia legendi for Surgery, Habilitation with the title „Use of alloplastic meshes for the repair of abdominal wall hernia: optimisation by adjustment to the physiological requirements “

Since 15.10.2000: Principal investigator of the surgical department

21.3.2002: specialist for surgical intensive care medicine

1.1.2003 – 1.11.2006: Assistant medical director

21.7.2004: Specialist for visceral surgery

13.12.2005: appointment as a.pl. Profess

1.11.2006-28.2.2009: Cooperation with the Institute for applied medical engineering of the Helmholtz institute

1. Scientific work

- Pathophysiology and treatment of abdominal wall hernia
- Biomaterials and tissue response
- Impact of altered ECM for wound healing and cancer development
- Analysis of biological networks
- Identification of prognostic markers
- Optimisation of staplers

Member of the Editorial Board of World Journal of Gastrointestinal Surgery (WJGS)
Member of the scientific committee for the research program START of the university clinic
Member of the German Society of surgeons
Member of the European Hernia Society
Member of the German Hernia Society

Publications

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176. U. Klinge: Experimental investigations with alloplastic materials: Which properties are essential for use at the pelvic floor? International collaboration of the pelvic floor ICOPF
177. U. Klinge: Welche Hernie braucht ein Mesh? 1. Tagung der Schweizer Herniengesellschaft in Bern, 4.4.2008
178. U. Klinge: Welche Probleme können bei der Verwendung von Netzen in der Hernienchirurgie auftreten? 125. Kongress der DGfC, 22.-25.4.2008, Berlin
179. U. Klinge : Low-weight polypropylene mesh: what is the clinical importance of the porosity for hernia repair? 30. congrèß of the EHS, Sevilla, Spain: 7-10.5.2008
180. U. Klinge: Grundlagen der Hernienreparation aus Sicht des wissenschaftlichen Chirurgen. 5. Tagung der Deutschen Hernien-Gesellschaft, Baden-Baden:29.-31.5.2008
181. U. Klinge: Postoperative CRPS in inguinal hernia patients. 5. Suvretta-Workshop, St. Moritz: 1.-7.7.2008
182. U. Klinge: Two controversial concepts: Standard procedure in a standard patient versus tailored surgery with procedures adjusted to individual patients? 5. Suvretta-Workshop, St. Moritz: 1.-7.7.2008
183. U. Klinge: Degradationsprozesse und Netzbrüche in der Hernienchirurgie. 3. Wilhelmsburger Hernientage, Hamburg: 5.-6.9.2008
184. U. Klinge: Update Biomaterialien und Netze in der Hernienchirurgie. 12. chir. Forschungstage, Freiburg: 25.7.-29.9.2008
185. U. Klinge: Classification of incisional hernia - from Aachen's point of view. Consensus meeting on the development of an EHS classification, Gent, Belgium, October 2nd - 4th 2008
186. U. Klinge: What should be considered for selection of mesh material. AHS, Beijing, 1.-2.11.2008
187. U. Klinge: The CRPS after groin hernia repair. AHS, Beijing, 1.-2.11.2008
188. U. Klinge: Hernia repair tailored to the patient instead of using a gold standard?. AHS, Beijing, 1.-2.11.2008
189. U. Klinge: Future perspectives in textile implants. AHS, Beijing, 1.-2.11.2008
190. U. Klinge: Update mesh. Shanghai. 28.11.2008
191. U. Klinge: Hernia and Collagen. 4. Rotterdam interactive congress for hernia, 21.11.2008, Rotterdam, NL
192. U. Klinge: Was ist bei der Auswahl von Meshes zu beachten? Zürser Hernienforum 14.12.-16.12.2008, Zürs, Austria
193. nicht mehr aktualisiert
194. U. Klinge, N. Farthmann, A. Fiebler: Aldosterone network. San Diego, 17.6.2010
195. U. Klinge et al: ISIR, Rostock, chirurgische Forschungstage
... not longer actualised

Oral presentation, on invitation:

1. U.Klinge Review of literature and experimental results of mesh surgery Expert-Meeting Suffretta-House St. Moritz Feb. 1994
2. U.Klinge Pathophysiologie der Narbenhernie Chirurtag Nürnberg 24.10.1996
3. Conze, J., U.Klinge (1998) Biocompatibility of biomaterials – clinical and mechanical aspects. II Suvretta meeting: abdominal wall: function, defects and repair. 8.-14.3.1998 St. Moritz Swiss
4. U. Klinge, B. Klosterhalfen (1998) Biocompatibility of biomaterials – experimental aspects. II Suvretta meeting: abdominal wall: function, defects and repair. 8.-14.3.1998 St. Moritz Swiss
5. B. Klosterhalfen, U. Klinge (1998) Biocompatibility of biomaterials – histological aspects. II Suvretta meeting: abdominal wall: function, defects and repair. 8.-14.3.1998 St. Moritz Swiss
6. U. Klinge (1998) Meshes zur Hernienreparation. 7. Interdisziplinäres Forum der Förderung operativer medizinisch-wissenschaftlicher Fachgesellschaften 17.10.1998 Wiesbaden
7. U. Klinge (1999) Chirurgie der Narbenhernie. 5. Kölner Tagung ambulantes Operieren. Köln, 7.5.1999
8. U. Klinge (1999) Pathophysiologie der Bauchdecke. Weissensee Operationskurs 24.9.99
9. U. Klinge (1999) Rezidive und Patientenkomfort im Langzeitverlauf. Weissensee Operationskurs 24.9.99
10. U. Klinge (7.12.1999) Meshes in der Hernienchirurgie. 5. Zürser Hernienforum, Zürs, Austria
11. U. Klinge (9.3.2000) Narbenhernienchirurgie: Primärverschluß oder Netzimplantat? Interdisziplinäre Viszeralchirurgie am Inselspital, Bern, Schweiz
12. U. Klinge (3.5.2000) Biomaterialien in der Hernienchirurgie. FomwF, 117. Kongreß der Deutschen Gesellschaft für Chirurgie 2.-6.5.2000, Berlin
13. U. Klinge (4.5.2000) Epidemiologie und Pathophysiologie der Bauchwanddefekte. Narbenhernie, 117. Kongreß der Deutschen Gesellschaft für Chirurgie 2.-6.5.2000, Berlin
14. U. Klinge (26.5.2000) Anatomy and physiology of the abdominal wall. Laparoscopic incisional hernia repair a standard therapy? Rastatt, 25.5-27.5.2000
15. U. Klinge (2.6.2000) Technical aspects, abdominal wall physiology, integration and inflammatory reaction. 35. ESSR-Kongreß, Malmö, 1.-3.6.2000
16. U. Klinge (2.6.2000) News and future outlooks. 35. ESSR-Kongreß, Malmö, 1.-3.6.2000
17. U. Klinge (2000) Pathophysiologie der Bauchdecke. Weissensee Operationskurs 2000, 8.9.2000, Berlin
18. U. Klinge (2000) Rezidive und Patientenkomfort im Langzeitverlauf. Weissensee Operationskurs 2000, 8.9.2000, Berlin
19. U. Klinge (2000) Netzimplantate in der Hernienchirurgie – Charakteristika und Anforderungen. Netzimplantate 22.-23.9.2000, Würzburg
20. U. Klinge (2000) Minimale Polypolypropylen-Netze zur präperitonealen Netzplastik – prospektive Studie. 22.-23.9.2000, Würzburg
21. U. Klinge (2000) Implantierbare Netze in der Chirurgie – Nutzen oder Risiko? Fortbildungsveranstaltung der Kreisstelle Mülheim/Ruhr 10.10.2000. Evang. Krankenhaus Mülheim a. d. Ruhr
22. U. Klinge, B. Klosterhalfen, V. Schumpelick (2000) Kollagenstoffwechselstörungen und Konsequenzen für die chirurgische Therapie. Gründungskongress der Arbeitsgemeinschaft Wundheilung der DGfC, 13-14.10.2000 Tübingen
23. U. Klinge (2000) Offene Mesh-augmentierte Reparatursverfahren der Leistenhernie. 12. Wuppertaler Workshop für laparoskopische Operationen, 16.-17.11.2000, Wuppertal

24. U. Klinge (2001) Netzimplantate in der Hernienchirurgie: Charakteristika und Anforderungen. Implantate in der Hernienchirurgie – Quo vadis? 2.-4.4.2001, European Surgical Institute, Norderstedt
25. Klinge, U (2001) Rezidivoperationen und Biomaterial. 1668. Jahrestagung der Vereinigung Niederrheinisch-Westfälischer Chirurgen, 27.-29.9.2001 Bielefeld
26. Klinge, U (2001) Rezidive und Patientenkomfort im Langzeitverlauf. 3. Weißenseer Operationskurs 28.-29.9.2001, Berlin
27. Klinge U (2001) Welcher Patient bekommt ein Rezidiv? Aktueller Stand der Forschung. Workshop Viszeralchirurgie 24.-26.10.2001
28. Klinge U (2002) Epidemiologie, Pathologie und sozioökonomische Bedeutung der Narbenhernie. Baden-Baden 21-23.2.2002: Symposium Laparoskopische und konventionelle Narbenhernienreparation. Konkurrierende oder ergänzende Verfahren?
29. Klinge U (2002) Shouldice Methode der Wahl? Symposium 20.4.2002, European Surgical Institute, Norderstedt
30. Klinge U (2002) Pathophysiological concept for hernia repair. ESSR Congress Szeged, 23.-25.5.2002
31. Klinge, U (2002) Der Shouldice. 18. Krefelder Chirurgen-Symposium, 12.6.2002, Krefeld
32. Klinge U (2002) Die parastomale Hernie – seine Ursachen und Möglichkeiten der Therapie. ILCO Aachen, 26.8.2002, Aachen
33. Klinge, U (2002) Impact of mesh material on clinical results. III Spotkanie Polskiego Klubu Przepuklinowego 20.-21.9.2002, Bydgoszcz, Poland
34. Klinge U (2002) Epidemiologie und Pathogenese der Narbenhernie sowie Ansätze zu deren RepARATION. 2. Österreichischer Chirurgenstag, Baden, 22.-23.11.02
35. Klinge U (2003) How to construct a mesh? III. Suvretta meeting 14.-18.1.2003-01-22
36. Klinge U (2003) Mesh materials: tissue response and tissue engineering. ESAO 3.9-6.9.2003, Aachen
37. Klinge U (2004) Laparoskopische Narbenhernienreparation – Contra. Mic-Club West, 2. 4. 2004, Aachen
38. Klinge U (2004) Spätfolgen und –ergebnisse nach Netzimplantation in der Bauchdecke. 10. 10. Kölner Tagung des BDC „Ambulante Chirurgie in Klinik und Praxis“, 14.-15.5.2004, Köln, Crowne Plaza Hotel
39. Klinge, Uwe (2004) Incisional hernia: Laparoscopic versus open – open. 12th international Congress of the European Association for endoscopic surgery, 9-12.6.2004, Barcelona
40. Klinge, Uwe (2004) Vorteile der konventionellen Hernienchirurgie. Marburg, 30.6.2004
41. Klinge, Uwe (2004) Das Netz als Gewebeersatz. 2. Mitteldeutscher Chirurgenkongress, Leipzig 23.-25.9.2004-09-27
42. Klinge U (2004) Pathophysiology and therapeutic impact of meshes. Utrecht 13.9.2004
43. Klinge U (2004) Biomaterials for Hernia repair. Utrecht 13.9.2004
44. Klinge U (2004) Standardoperationen – unterer GI-Trakt. Workshop Praktische Onkologie, Bonn 23.-24.10.2004
45. Klinge U (2004) Standardoperationen – oberer GI-Trakt. Workshop Praktische Onkologie, Bonn 23.-24.10.2004
46. Klinge U (2004) Novel textile structures in medicine. 31th Aachen Textile conference, 24.-25.11.2004, Aachen, Eurogress
47. Klinge U (2.1.2005) Complications in open incisional hernia, European hernia symposium, London
48. Klinge (2.1.2005) Evidence based open IH, European hernia symposium, London
49. Klinge, U (2005) Nabel-, Narbenhernie. BDC-Seminar, Kassel. 14.-18.2.2005
50. Klinge, U (2005) Open-Non-Mesh: Shouldice – the good old way. 16.2.2005 Leistenhernienchirurgie 2005, Bethlehem-Krankenhaus, Stolberg

51. Klinge U (2005) Alloplastische Implantate und Gewebereaktion. Luzern 22.9.2005 1. gemeinsame Fortbildung der Vereinigung der Gynäkologen Luzern/Zentralschweiz
52. Klinge U (2005) Standardoperationen – unterer GI-Trakt. Workshop Praktische Onkologie, Bonn 14.-16.10.2005
53. Klinge U (2005) Standardoperationen – oberer GI-Trakt. Workshop Praktische Onkologie, Bonn 14.-16.10.2005
54. Klinge U (2005) Narbenhernien – nur bei den anderen? State of the art lecture. 16. Berner Symposium, Bern 4.11.2005
55. Klinge (2006) Rezidivhernien – ein biologisches Problem? 123. Kongress der DGfC, Berlin 2.-5.5.2006
56. Klinge (2006) Modern hernia repair. Workshop Prof. Berger, Baden-Baden 28.4.2006
57. Klinge (2006) Komplikationen der minimal-invasiven Hernientherapie. Mic-Club West, Dinslaken, 19.5.2006
58. Klinge (2006) Auswahlkriterien für Netze. Hernienchirurgie 2006. Deutsche Herniengesellschaft Hannover 26.-27.5.2006
59. Klinge (2006) Modern hernia surgery. Hong Kong 28.6.2006
60. Klinge U (2006) Pathohistological data of meshes. 10th world congress of endoscopic surgery, Berlin 13.-16.9.2006
61. Klinge U (2006) Technical and biological aspects of meshes. 10th world congress of endoscopic surgery, Berlin 13.-16.9.2006
62. Klinge U (2006) Narbenhernie: chirurgische Fehler oder Schicksal? Gastroenterologie 2006, 13.-16. September 2006, Hannover
63. Klinge U. Anatomical limitation for mesh positioning. 2nd Congress of the Asia pacific hernia society 2006, 6-8th October
64. Klinge U Recurrence as a problem of biology & collagens. 2nd Congress of the Asia pacific hernia society 2006, 6-8th October
65. U. Klinge Standardoperationen bei Tumoren des unteren GI-Traktes. Interdisziplinärer Workshop GI Tumore. 20-22.10.2006, Bonn
66. U. Klinge Standardoperationen bei Tumoren des oberen GI-Traktes. Interdisziplinärer Workshop GI Tumore 20-22.10.2006, Bonn
67. Klinge U. Meshes in der Chirurgie. Berlin 4.11.2006 Uro-gynäkologische Tage
68. Klinge U: Biomaterialien für die Hernienchirurgie: für wen, wie und wieviel? Berliner Hernien-Tage 18-20.1.2007
69. U. Klinge Der chronische Leistenschmerz. 4.5.2007. Jahreskongreß der DGfC
70. U. Klinge The concept of flat meshes. 8.8.2007, Shanghai
71. U. Klinge How to prevent recurrences. 8.8.2007, Shanghai
72. U. Klinge Standardverfahren oder maßgeschneiderte Therapie – wo soll die Reise hingehen? Herbstkongreß der DGVC vom 12. bis 15.09.2007, Bochum
73. U. Klinge Evidence-basierte Datenlage zur chirurgischen Narbenhernien-Versorgung. Herbstkongreß der DGVC vom 12. bis 15.09.2007, Bochum
74. U. Klinge Was sind die Probleme mit schwergewichtigen Netzen? Herbstkongreß der DGVC vom 12. bis 15.09.2007, Bochum
75. U. Klinge Meshes in der Chirurgie, Hamburg ESI Mesh-Forum 17.9.2007
76. U. Klinge Update Hernienchirurgie, Freiburg, 8.10.2007
77. U. Klinge: Does material and porosity of meshes matter? 8th congress of the panhellenic surgical society of northern Greece, 18-21.10.2007, Thessaloniki
78. U. Klinge: Concept of CRPS in the groin. and strategies for treatment. Pain & Hernia surgery symposium, ESI, Hamburg, 30th October 2007
79. U. Klinge: The CRPS – concept for chronic pain in the groin? Rotterdam Interactive Congress on Hernia RICH 2007, 16.11.2007, Rotterdam

80. U. Klinge: The CRPS as concept for chronic pain? Belgium surgical society 2007, 29.11.2007, Brüssel
81. U. Klinge: Was können Goldstandards leisten? 14.12.2007 Berlin, <http://www.gcp-workshop.de/1331.html>
82. U. Klinge: Concept of complex regional pain syndrome in the groin and strategies for treatment. 3rd annual meeting of IEHS 17.-19.1.2008 Stuttgart
83. U. Klinge Polyester, PVDF oder PTFE – kein, zwei oder vier Fluoratome? 2. Berliner Hernientage 25.-26.1.2008 Berlin
84. U. Klinge Schluß mit der Suche nach dem Gold-Standard! 2. Berliner Hernientage 25.-26.1.2008 Berlin
85. U. Klinge: Experimentelle Untersuchungen zu alloplastischen Materialien: Welche Eigenschaften sollten sie für die Verwendung am Beckenboden haben? 17. Urolog. Winterworkshop Leogang 28.01. - 01.02.2008
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92. U. Klinge: Postoperative CRPS in inguinal hernia patients. 5. Suvretta-Workshop, St. Moritz: 1.-7.7.2008
93. U. Klinge: Two controversial concepts: Standard procedure in a standard patient versus tailored surgery with procedures adjusted to individual patients? 5. Suvretta-Workshop, St. Moritz: 1.-7.7.2008
94. U. Klinge: Degradationsprozesse und Netzbrüche in der Hernienchirurgie. 3. Wilhelmsburger Hernientage, Hamburg: 5.-6.9.2008
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96. U. Klinge: Classification of incisional hernia - from Aachen's point of view. Consensus meeting on the development of an EHS classification, Gent, Belgium, October 2nd - 4th 2008
97. U. Klinge: What should be considered for selection of mesh material. AHS, Beijing, 1.-2.11.2008
98. U. Klinge: The CRPS after groin hernia repair. 4th International Congress of the Asia-Pacific Hernia Society, 5th Annual Conference of China hernia Society, 30.10.-2.11.2008, Beijing
99. U. Klinge: Hernia repair tailored to the patient instead of using a gold standard?. 4th International Congress of the Asia-Pacific Hernia Society, 5th Annual Conference of China hernia Society, 30.10.-2.11.2008, Beijing
100. U. Klinge: Future perspectives in textile implants. 4th International Congress of the Asia-Pacific Hernia Society, 5th Annual Conference of China hernia Society, 30.10.-2.11.2008, Beijing
101. U. Klinge: Update mesh. Master class Shanghai 28.11.2008
102. U. Klinge: Hernia and Collagen. 4. Rotterdam interactive congress for hernia, 21.11.2008, Rotterdam, NL

103. U. Klinge: Was ist bei der Auswahl von Meshes zu beachten? Zürser Hernienforum 14.12.-16.12.2008, Zürs, Austria
104. U. Klinge: Die „männliche Schlinge“ zur Therapie der Harninkontinenz. AGKAMED „Neue Behandlungswege der männlichen Inkontinenz“, Berlin, 12.5.2009
105. U. Klinge: Was bedeutet Biokompatibilität in der Chirurgie. 1.5.2009 München, Jahreskongreß der DGFC
106. U. Klinge: Lightweight mesh Konzept. 28.4.2009 München, Jahreskongreß der DGFC
107. U. Klinge: Welche Netze für die offene/laparoskopische Narbenhernienreparation? 30.4.2009 München, Jahreskongreß der DGFC
108. U. Klinge: Biomechanische Anforderungen: Was sollen und können Netze leisten? 30.1.2009, Berlin 3-Chirurgen
109. U. Klinge: What has to be considered for selection of alloplastic nets and slings at the pelvic floor? 28.3.2009, Dijon
110. U. Klinge: Leuven Aachen Rotterdam Herniosis Studygroup LARHS 10.4.2009, Leuven
111. U. Klinge: Biologicals für die Hernienchirurgie? Jahreskongreß der Deutschen Herniengesellschaft in Neuss, 19-20.6.2009
112. U. Klinge: Mesh – structure or confusion? 4. Internationaler Welthernienkongreß in Berlin 9.-12.9.2009
113. U. Klinge: Das ideale Mesh? Euregio Bodensee, 3.7.2009 St. Gallen
114. U. Klinge: Limitation and perspective of Biologicals. Leeds, 23.10.2009
115. U. Klinge: Update Narbenhernienchirurgie unter Einbeziehung von Grundlagen der Netzstabilität Chirurgische Abteilung, Uniklinik Essen, 26.10.2009
116. U. Klinge: Principles of hernia repair. Masterclass Baden-Baden, 20.11.2009
117. U. Klinge: Biologicals. Masterclass Baden-Baden, 21.11.2009
118. U. Klinge: Update Literature for hernia. Masterclass Baden-Baden, 20.11.2009
119. U. Klinge: Textile structures for the pelvic floor. Kopenhagen, 27.11.2009
120. U. Klinge: Biologicals as standard for hernia repair. 4. Berliner Hernien-Tage, 28.1.2010
121. U. Klinge: Das ideale Mesh: 4. Berliner Hernien-Tage, 30.1.2010
122. U. Klinge: Große Datenmengen für die Medizin? Arbeitstreffen E-Health, RWTH-Aachen, 25.1.2010
123. U. Klinge: Was unterscheidet die Netze? DGfC Berlin 2010
124. U. Klinge: the ideal mesh. Oslo 4/2010
125. U. Klinge: What is the ideal mesh? Dubai 4/2010
126. U. Klinge: biologicals for every hernia? Dubai 2010
127. U. Klinge: mesh classification? Dubai 2010
128. U. Klinge: Meshes für die Chirurgie. Fulda, EKK 17.5.2010
129. U. Klinge: Hernie - Gibt es eine einfache „Pathophysiologie“ München 11.6.2010 Deutsche Herniengesellschaft
130. U. Klinge: Wie kann man Meshes klassifizieren? BvMed 2.7.2010
131. U. Klinge: Gibt es eine einfache Pathophysiologie, DHG München, 10-12.6.2010
132. U. Klinge: Mesh in der Leistenhernienchirurgie. Schwarzenberg, Scheyer, Austria 1.-3.7.2010
133. U. Klinge: Basic principles of mesh implants and actual status of knowledge. Liedl, München Bogenhausen, 13-14.10.2010
134. U. Klinge: Alloplastische Materialien in der Hernienchirurgie – was gibt es Neues? Wilhelmsburger Hernientage 23-24.10.2010
135. U. Klinge: Biomechanics, immunology and tissue response to the mesh. Brazilian hernia Congress November 25th to 27th, 2010 InterContinental Hotel Rio de Janeiro

136. U. Klinge: Biologicaals. Brazilian hernia Congress November 25th to 27th, 2010 InterContinental Hotel Rio de Janeiro
137. U. Klinge: Sublay, Why and How ? Brazilian hernia Congress November 25th to 27th, 2010 InterContinental Hotel Rio de Janeiro
138. U. Klinge: Paracolostomic hernia. Brazilian hernia Congress November 25th to 27th, 2010 InterContinental Hotel Rio de Janeiro
139. U. Klinge: PVDF. Brazilian hernia Congress November 25th to 27th, 2010 InterContinental Hotel Rio de Janeiro
140. U. Klinge: Prophylaxe der Hernienentstehung? Berliner Hernientage 24-29.1.2011
141. U. Klinge: Grundlagen und Materialien. Berliner Hernientage 24-29.1.2011
142. U. Klinge: Classification of surgical meshes for hernia repair. EHS, Gent, 11-13.5.2011
143. U. Klinge: Risk factors for incisional hernia development. EHS, Gent, 11-13.5.2011
144. U. Klinge: Statistics and analysis for biological material in hernia treatments – the current status quo. Cook Symposium. Berlin, 19-20.5.2011
145. U. Klinge: Biologische Netze heute. 1. Düsseldorfer Herniensymposium. 2.4.2011
146. U. Klinge: Chaos bei den Kunststoffnetzen: Vorschlag zur standardisierten Einteilung. DHG Oldenburg, 26-28.5.2011
147. U. Klinge: Das ideale Mesh. Fürth, 30.6.2011
148. U. Klinge: Surface modification: do we really need it ? EHS Winter conference, Madonna di Castillo, 10-12.3.2011
149. U. Klinge: Abdominal wall hernia. current update. 10. – 12.11.2012 Masterclass Baden-Baden
150. U. Klinge: Prophylaxe der Hernienentstehung. Symposium Rotkreuzklinikum München. 25.11.2012
151. U. Klinge: "Surface modification to direct tissue response" RICH, Rotterdam, 13.1.2012
152. U. Klinge: Grundlagen und Materialien. Hernia Kompakt, Hamburg, 19.1.2012
153. U. Klinge: Klassifikation von Netzimplantaten in der Hernienchirurgie. 4. Wilhelmsburger Hamburg, 20.1.2012
154. U. Klinge: Evidence based medicine - Was sollen wir glauben? 25.4.2012, DGfC, Berlin
155. U. Klinge: Uni Essen Chirurgie-Fortbildung: Hernienchirurgie – wann welches Netz. 21.5.2012
156. U. Klinge: Classification of meshes for risk assessment. EuraHS, Brüssel, 7.6.2012
157. U. Klinge: Change in pore size and weight of abdominal wall meshes: What did it bring us so far? Brüssel, 25.10.2012
158. U. Klinge: Materialien in der Hernienchirurgie. Hernia Kompakt München, 24-26.10.2012
159. U. Klinge: EBM – was sollen wir glauben. Hernie interaktiv, München, 27.10.2012
160. U. Klinge: From view of experimental surgeon – meshes for pelvic floor. Munc, 17.11.2012
161. U. Klinge: Biomechanic aspects of meshes for pelvic floor surgery. Expert class Cologne Prof. Jäger, 7.-8.12.2012
162. U. Klinge Klassifikation der Netze. 25.-26.1.2013, 6. Berliner Hernientage
163. U. Klinge Sichtbare Netze, erste Ergebnisse, 25.-26.1.2013, 6. Berliner Hernientage.
164. U. Klinge Netz- und Materialentwicklung: Biomaterialien in der Chirurgie: Fluch oder Segen ? 59. Kongress der Nordrhein-Westfälischen Gesellschaft für Urologie. 11. – 12. April 2013 [Rheinterrasse Düsseldorf.
165. U. Klinge: Individual patient centred outcome research as alternative to randomized controlled trials (RCT). Gdansk EHS 14.5.2013, EHS

166. U. Klinge: Ist Randomisierung der Schlüssel zur evidenzbasierten Hernienchirurgie ?
Cottbus 7.-8.6.2013, DHG
167. U. Klinge Das richtige Netz TAPP / TEP / offen. Saale-Unstrut, 29.6.2013
168. U. Klinge. Textile meshes in Surgery:
FDA Warnings – New Standards – Registries - What can we learn from Hernia Surgery?
Barcelona ICS. 29.8.2013
169. U. Klinge Moderne Netz-Technologie. 2. Düsseldorfer Hernien-Symposium Zarras,
26.9.2013

Grants

	Principal investigator, co-workers	topic	Supporter, duration	period	Amount of resources
	Klinge, Hörer	Panacryl-Fadenstudie	Ethicon / 3 Jahre	1999-2002	260.000
	Klinge, Welty	Internationale Vypro-Studie	Ethicon / 3 Jahre	1999-2002	54.000
	Klinge, Welty	SHM-Studie	Ethicon / 2 Jahre	1997-1999	262.000
	Klinge	Kollagen-Studie	Ethicon / ½ Jahr	1999	30.000
TV 9	Klinge	Verwendung von Biomaterialien beim Bauchdeckenverschluß	BIOMAT 4 Jahre	1995-1998	208.107
TV 41/42	Klinge/Stein	PVDF-Mesh	BIOMAT 2 Jahre Nachfolgeprojekt 2 Jahre	1999-2000 2001-2002	347.940
	Klinge	Mesh-Entwicklung	Ethicon	2000-2003	375.000 Kostenstelle: 9876170 Anforderungsnummer: 98761770
TV 66	Mertens, Klinge	Mesh-Fibroblasten	BIOMAT	2001-2002	330.000
TV 61	Bertram, Tietze, Klinge	Kokulturen	BIOMAT	2001-2002	210.000
FEG/BMBF	Klinge, Klosterhalfen	Entwicklung von neuartigen bioverträglichen Netzmaterialien zur anatomisch angepassten chirurgischen Hernientherapie - Beschichtete Meshes	03N4024 FEG-065/1-2001	1.3-2001-2004	358.824,-
DFG	Klinge, Klosterhalfen, Mertens	Kollagen und Hernie	KL 1320/2-1	21.6.2001-21.6.2003	350.000,-
Ethicon	Schumpelick,	Optimierung von Mesh-Strukturen	370253	1.4.2003-	360.000 €

	Principal investigator, co-workers	topic	Supporter, duration	period	Amount of resources
	Klinge, Stumpf, Junge, Schachtrupp, Steinau, Schwab			31.3.2006	
DFG	Lynen-Jansen Mertens Klinge Jansen	Einfluß von Biomaterialien auf die MMP-2 Genexpression in vivo	DFG JA1123/1-1	2004-2005	120.000 Euro
DFG-Projekt	Lynen-Jansen Mertens Klinge Jansen	Untersuchungen zur Gewebe-Integration von Biomaterialien bei selektiver Blockade der TNF α -abhängigen MMP-2 Expression	DFG JA 1123/1-2,	Laufzeit 2 Jahre, Umfang Start 2008	ca. 120.000 Euro,
INNONENT	HIA und Frauenhofer	Die sichere Naht	VDI/VDE	2/2008-2011	Gesamtvolume n 1,1 Mill €
Mesh insight	FEG und UK-Aachen Klinge U, Otto J, Krämer N, Obolenski B:	Sichtbarmachung von textilen Implantaten im MRT durch Einlagerung von superparamagnetischen Eisenoxid-Nanopartikeln Innovationswettbewerb 2007 des BmbF zur Förderung der Medizintechnik, 18.10.2007	BMBF 01EZ0849	1.4.2008-31.1.2011 3.2008-1.2.2011	Gesamtvolume n ca. 900.000€
	Kämmer, Otto, Klinge	PVDF-Mesh Beschichtung mit NN-Hormonen	ESAC	2008	12 000€
Bioinside	FEG/Fiebeler/Berlin	Beschichtung mit DHEA	BMBF BioInside 13N9827-13N9833 PN 372552	2008-2010	70 000€
	Klinge	InnoMeT.NRW: Patientenadaptierte Medizintechnische Lösungen für die Kardiovaskuläre Therapie	005-1003-0067 IAN 700584	1.8.2010-31.7.2013	270 000
	Klinge	Elastisches Netz-Implantat für die Chirurgie am Zwerchfell (Hiatus-Mesh)	ZIM-Projekt KF2621701AJ0	14.4.2010-31.10.2011	110 000€
	Klinge/Tolba	Covidien Stapler Pase I	372708	1.2.2010-31.1.2011	120 000 Eur
	Klinge/Tolba	Covidien Stapler Pase II	372708	1.4.2011-31.3.2012	180 000 Eur
	Klinge et al, ZIM 3D	3D Implantat	ZIM / AiF 13EZ1201C	1.10.11-30.9.2013	174 893 €
	Klinge et al, ZIM Hiatus-Mesh	Zwerchfell-Netzimplantat	ZIM / AiF KF2621701AJ0	1.4.10-31.11.2011	110 365 €
	Klinge et al E-	Elastisches Mesh	01EZ1201C	1.6.2012-	240 000€

	Principal investigator, co-workers	topic	Supporter, duration	period	Amount of resources
	Mesh BMBF (DLR)			31.5.2015	

Patents:

02754251.3-2107-DE0202287 FEG Textiltechnik vom 25.6.02: Textiles Implantat mit monofilen Polyvinylidenfluorid-Fäden

„Einstückiges Stomaunterstützungsimplantat“ WO 2008/031411 A1

„Medizinisches Implantat mit Oberflächenbeschichtung“ AZ 10 2009 005 792.7

„Meshförmiges Implantat“ (Mesh mit Ferrofluiden) PCT/DE 2008/000805

„Textiles Intraperitoneal-Mesh“ DE 10353930.1

„Textiles Erzeugnis mit Oberflächenmodifikation und entsprechendes Verfahren zur Oberflächenmodifikation“ PCT/DE02/04291

„Textiles Implantat“ WO PCT/DE02/02287

EXHIBIT B

Date	Bates Number	Title
November 2010- October 2011	ETH.MESH.00562421	Untitled PPT update
3/26/2008	ETH.MESH.02170708	Email from David Robinson to Dr. Vincent Lucente re: UP
	ETH.MESH.01760854	David Robinson, Gynemesh PS Clinical Expert Report
8/14/2007	ETH.MESH.00869908	Thunder Meeting Minutes
7/31/2007	ETH.MESH.01819505	Thunder Meeting Minutes
	ETH.MESH.01405166	"Exploratory Program 'Thunder' A Material designed for Pelvic Floor" Powerpoint presentation By: Clifford Volpe and Peter Meier
4/12/2007	ETH.MESH.00832555	Thunder Meeting Minutes
	ETH.MESH.00742724	"Ethicon Women's Health & Urology: Project Lightning Update"
2/13/2006	ETH.MESH.00585937	Email from Gene Kammerer to Quentin Manley et al re: TVM Discussions
2/26/2004	ETH.MESH.02270823	Email from Joshua Samon to Scott Ciarrocca et al. re: mesh implants - user needs
1/18/2005	ETH-18761	Email from Kelly Brown to Gene Kammerer re: Proposal for work with CBAT
3/25/2004	ETH.MESH.01988643	Email from Vincenza Zaddem to Scott Ciarrocca re: disclosure questions
	ETH.MESH.01424246	Holste, J; Test report No.: B0086/02, Histopathological report/Immunohistochemical report
2001	ETH.MESH.02017169	Hellhammer, B., <i>Meshes in Pelvic Floor Repair – Findings from literature review and interviews with surgeons.</i>
	ETH.MESH.03719177	Chris Vailhe report "Polypropylene Mesh for Pelvic Floor Repair (PFR) – Focus on Mesh Exposure – Road to Improvement
06/2009	ETH.MESH.02157879	Klosterhalfen B., <i>Interim Report Mesh Explants Pelvic Floor Repair</i>
	ETH.MESH.01819528	WW Customer Complaints – received from Carey Brennan
1/13/2005	ETH.MESH.02286052	Email from Sean O'Bryan to Scott Ciarrocca re: IFU Prolift
03/2009	ETH.MESH.00017369	Elmer C, Blomgren B, Falconer C, Zhang A, and Altman D; <i>Histological Inflammatory Response to Transvaginal Polypropylene Mesh for Pelvic Reconstructive Surgery.</i> The Journal of Urology Vol. 181, 1189-1195, March 2009
01/2009	ETH.MESH.00017239	Elmer C., Altman D., Ellstrom Engh M., Axelsen S., Vayryen T., and Falconer C.; <i>Trocar-Guided Transvaginal Mesh Repair of Pelvic Organ Prolapse.</i> ACOG Vol. 113, No. 1, January 2009

2/1/2006	ETH.MESH.0394544	Memo to Sunny Rha re: Global Regulatory Strategy - Gynecare TVT - Laser Cutting Project
11/21/2005	ETH.MESH.00301741	Email From Dan Lamont to Jacqueline Flatow re: !!!!!GREAT NEWS FOR TVT LASER CUT MESH!!!!
10/12/2005	ETH.MESH.0353750	Letter from Carol Holloway to Herve Fournier re: TVT Device, Blue Mesh
	ETH.MESH.02059212	Prolift Surgical Guide
	ETH.MESH.01221055	Pariente J-L; <i>An independent biomechanical evaluation of commercially available suburethral slings.</i> Issues in Women's Health
6/6/2000	ETH.MESH.03904451	Meshes in Pelvic Floor Repair
11/22/2006	ETH.MESH.02992137	Lightning Clinical Strategy
4/5/2007	ETH.MESH.01218361	"State of the knowledge in 'mesh shrinkage' - What do know" by Kerstin Spychaj
3/4/2008	ETH.MESH.00832562	Thunder Meeting Minutes
12/18/2007	ETH.MESH.00832562	Thunder Meeting Minutes
2010	ETH.MESH.01192895	Velemir L, Amblard J, Fatton B, Savary D, Jacquetin B, <i>Transvaginal mesh repair of anterior and posterior vaginal wall prolapse: a clinical and ultrasonographic study.</i> Ultrasound Obstet Gynecol (2010)
6/22/2011	ETH.MESH.07192929	PA Consulting report "Investigating Mesh Erosion in Pelvic Floor Repair"
2/27/2008	ETH.MESH.03731339	Email from Dan Smith to Matter Henderson, et al. re: tape position at rest
2/28/2005	ETH-03558	DDSA
2/17/2011	ETH.MESH.01264497	Email from Vincenza Zaddem to Vernon Ghee et al. re: Mesh pore size - tissue compliance and contraction
1/17/2010	ETH.MESH.01785259	Email from Dr. Piet Hinoul to Dr. David Robinson, et al. Re: +M relaxation
4/22/2009	ETH.MESH.02148431	Email from Dr. Joerg Holste to Jonathan Meet, et al. re: Question on Monocryl absorption
11/18/2008	ETH.MESH.00008072	Ethicon PFR online training course
8/23/2007	ETH.MESH.00000272	Email from Vincenza Zaddem to David Robinson re: macroporous - lower limit of pore size
3/28/2007	ETH.MESH.00593165	Vailhe Technical report
	ETH.MESH.00237968	"R&D Perspective - The Journey from Prolift to Prolift +M" Powerpoint by Cliff Volpe
2007	ETH.MESH.01782867	"Factors Related to Mesh Shrinkage" by Kerstin Spychaj
2/23/2007	ETH.MESH.02017152	Expert Meeting Minutes
6/2/2006	ETH.MESH.00870466	Expert Meeting Minutes
6/14/2006	ETH-83454	Email from Scott Ciarrocca to Rebecca Leibowitz, et al. re: Mesh Microns
2/5/2008	ETH.MESH.01259495	David Robinson, Gynecare Prolift +M Pelvic Floor Repair System Clinical Expert Report

	ETH-83788	Ethicon Corporate Product Characterization analysis by Dan Burkley
	ETH-00291	GPS for Pelvic Floor Repair
2005	ETH.MESH.02232937	Klosterhalfen, B., K. Junge, and U. Klinge, <i>The lightweight and large porous mesh concept for hernia repair</i> .
2004	ETH.MESH.00280338	Berrocal J., Clave H., Cosson M., Debodinance Ph., Garbin O., Jacquetin B., Rosenthal C., Salet-Lizee D., Villet R., <i>Conceptual advances in the surgical management of genital prolapse The TVM Technique;</i>
10/14/2003	ETH.MESH.01220710	Email from Gene Kammerer to Georgina NG re: Technical data on competitive meshes from Europe
4/22/2003	ETH.MESH.02183533	Email from Dan Burkley to Elizabeth Vailhe re Pore Size Request
2/8/2002	ETH.MESH.00199408	Gynemesh PS Design Validation Strategy
2002	ETH.MESH.02232930	Klinge U., Klosterhalfen B., Birkenhauer V., Junge K., Conze J., and Schumpelick V., <i>Impact of Polymer Pore Size on the Interface Scar Formation in a Rat Model</i> .
2/28/2008	ETH.MESH.02590865	"Thunder: Technical Review" powerpoint presentation
1/16/2001	ETH.MESH.01160507	Email from Edward Dormier including the December 2000 Corporate Product Characterization
	ETH.MESH.01992236	"Form for Test Method Applicability/Suitability"
1/18/2008	ETH.MESH.00906445	Email from Vincenza Zaddem to Bryan Lisa re: 510(k) mesh data with strength
	ETH-01754	FDA letter stating necessary force for arm pull-out
12/15/2008	ETH.MESH.00067363	Email attaching Vincent Lucente Webinar Transcript
	ETH.MESH.02227368	Meshes/Devices Chart
	ETH.MESH.02212840	
	ETH.MESH.00081180	Prolift Characteristics
9/10/2007	ETH.MESH.021989933	Email From Christoph Walther to Vincenza Zaddem re: "Info needed for FDA"
8/29/2007	ETH.MESH.00080842	Letter from Dr. Jiyoung Dang to Bryan Lisa regarding Prolift & Prolift +M changes
9/12/2007	ETH.MESH.00922443	Email from Vincenza Zaddem to Price St. Hilaire et al. regarding bidirectional elasticity statement
6/18/2007	ETH.MESH.01405170	"Exploratory Program 'Thunder'" Powerpoint presentation By: Clifford Volpe and Peter Meier
5/9/2008	ETH.MESH.02227224	"MGPP Thunder Decision Meeting" powerpoint presentation
12/1/2006	ETH.MESH.02195798	Email from Axel Arnud re Strength
6/26/2008	ETH.MESH.02195788	Prolift +M DRM

3/7/2007	ETH.MESH.00078537	Email from Joerg Holste re: Lightning 510(k) requirements
10/26/2008	ETH.MESH.02207388	Email from Jonathan Meek to Julie Bird et al. re: Prolift +M Pre-Reading
2012	ETH.MESH.03753245	"Biomechanics (Pelvic Forces) PowerPoint
	ETH.MESH.00396836	"Review of Surgical Techniques using Mesh" by David Robinson
5/8/2008	ETH.MESH.00318775	Email from Mark Yale to Jennifer Paine, Jonathan Meek et al. re: Prolift mesh was "not specifically design".
2/16/2011	ETH.MESH.02010834	"Biomechanical consideration for Pelvic floor mesh design" by Juergen Trzewik and Christoph Vailhe
2006	ETH-00255	Ethicon Marketing Brochure
	ETH.MESH.00033325	Professional Education PowerPoint presentation titled "The Science of Augmented Extracorporeal Reconstructive Pelvic Surgery"
2006	ETH-47802	Cobb WS, Burns JM, Peindl RD, Carbonell AM, Matthews BD, Kercher KW, Heniford BT <i>Textile analysis of heavyweight, mid-weight, and lightweight polypropylene mesh in a porcine ventral hernia model ...J Surg Res.</i> 2006 Nov;136(1):1-7. Epub 2006 Sep 22.
7/13/2009	ETH.MESH.02011199	Email from Peter Meier to Jonathan Meek, Piet Hinoul et al. re TPO_TPP and the comparison of PVDF to PP
2009	ETH.MESH.01264260	Piet Hinoul Presentation
2004	ETH-65881	Gynecare Prolift IFU
2003	ETH.MESH.02053630	Gynemesh PS "White Paper"
1/23/2003	ETH-03883	"Prolene Resin Manufacturing Specifications" by John Karl
2/28/2005	ETH-03534	DDSA Appendix II Prolift "Summary Report"
2/28/2002	ETH-03558	DDSA Appendix VI "Form" describing hazards
7/20/2007	ETH.MESH.05920616	Email from Martin Chomiak to Boris Batke, et al. re Defining light weight mesh
	ETH.MESH.01816990	Kammerer Product development chart
	ETH.MESH.05479535	Microporous, Medium & Macroporous grid
3/13/2006	ETH.MESH.05446127	Email from Holste to Engel et al. re: Mesh and tissue contact in animals
03/2011	ETH.MESH.05479718	"Ethicon Polypropylene Mesh Technology" Powerpoint by Boris Batke
4/17/2003	ETH.MESH.05920530	Email from Boris Batke to Jill Schiaparelli et al. re Literature list of Lightweight Meshes
2/2/2008	ETH.MESH.05920618	Email from Petra Koehler to Boris Batke, et al. re Dr. Schumpelick
3/1/2012	ETH.MESH.04015102	Email from Boris Batke to Casey Mayes re AWES Pelvic Floor Conference - Gala Dinner invitation

6/3/2012	ETH.MESH.05585066	"Ultrapro" PowerPoint presentation by Boris Batke
	ETH.MESH.05916450	"Chronic Pain Prevention/future - Bioengineer's point of view"
	ETH.MESH.04037600	"Innovations in Mesh Development" By Boris Batke
	ETH.MESH.05479410	"The (clinical) argument of lightweight mesh in abdominal surgery" presentation by Boris Batke
5/4/2004	ETH.MESH.05918776	Email from Jill Schiaparelli to Karen Zaderej, Boris Batke et al. re Marlex experience
1/13/2005	ETH.MESH.04036976	Dynamesh, Dynamesh Light, Dynamesh IPOM: Analysis of Competitor meshes: Report
	ETH.MESH.02219202	Material Specification for TVT Prolene Polypropylene Mesh Roll Stock
4/3/2009	ETH.MESH.02184435	Email from Osman Rathore to Meng Deng et al. re Analytical characterization - Optimization of Structure
3/1/2012	ETH.MESH.07226377	Email from Laura Vellucci to Dennis Jamiolkowski re Polypropylene mesh
2/29/2012	ETH.MESH.04038180	Email from Dennis Jamiolkowski to Laura Vellucci et al. re Your Professional Opinion
3/5/2012	ETH.MESH.04937874	Email from Piet Hinoul to Laura Vellecci et al. re Polypropylene mesh
3/6/2012	ETH.MESH.07212397	Response to email from Clare Huntington 26 January 2012 (15:38) with attached publication: " <i>Polypropylene as a reinforcement in pelvic surgery is not inert: comparative analysis of 100 explants</i> ", <i>Int Urogynecol J</i> (2010) 21:261-270
3/12/2012	ETH.MESH.07205370	Response to email from Clare Huntington 26 January 2012 (15:38) with attached publication: " <i>Polypropylene as a reinforcement in pelvic surgery is not inert: comparative analysis of 100 explants</i> ", <i>Int Urogynecol J</i> (2010) 21:261-270
3/7/2012	ETH.MESH.07226404	Email from Dennis Jamiolkowski to Laura Vellucci et al. re Information on PROLENE Suture and PROLENE Mesh
04/2008	ETH.MESH.00006636	Klosterhalfen B., Interim Report Mesh Explants Pelvic Floor Repair
	ETH.MESH.07726805	Burkley notes on Dr. Klinge Prolift expert report
10/15/1992	ETH.MESH.05453719	Seven Year Data for Ten Year Prolene Study: ERF 85-219
12/14/2010	ETH.MESH.02588977	ERM team Meeting Minutes
	ETH.MESH.03699547	PA Consulting Cost
5/18/2011	ETH.MESH.02589032	PA Consulting "Investigating Mesh Erosion in Pelvic Floor Repair" Draft
3/31/2011	ETH.MESH.07198250	Email Christophe Vailhe to Joe Robinson re: Thanks & pictures

7/3/2002	ETH.MESH.02183537	Porosity Measurements of Various Meshes by D.F. Burkley
2/17/2010	ETH.MESH.05443495	Porosity Measurements of Various Meshes by D.F. Burkley
	ETH.MESH.05443059	Operating Procedure for Optical Evaluation to Determine Porosity of Mesh Samples Using the Nikon Stereomicroscope and Image-Pro Image Analysis System
	ETH.MESH.05443077	AST-2010-0587 "Pore Size Measurement of Surgical Mesh Products"
1/2/2006	ETH.MESH.00585906	Email from Gene Kammerer to Sunny Rha re TVT - TVT-O Specifications
11/14/2007	ETH.MESH.02212596	"Mesh Testing" Powerpoint presentation By Elizabeth Vailhe
2005	ETH.MESH.01424029	Cobb W, Kercher K, Heniford T. <i>The Argument for Lightweight Polypropylene Mesh in Hernia Repair</i> . Surgical Innovation. 2005; 12(1):T1-T7
	ETH.MESH.00528626	Product Quality Plan for Gynecare Gynemesh XL
4/25/2002	ETH.MESH.01808729	Corporate Product Characterization: Product Performance Evaluation Group; "Transfer of Finishing Operations for 6-mil Old Constructions Clea and 50% Blue PROLENE Mesh from ETHICON-Cornelia to PRODESCO, Inc"
	ETH.MESH.05918082	"Solving the Device Design Puzzle" Powerpoint
3/19/2003	ETH.MESH.01218446	Corporate Product Characterization: Product Performance Evaluation Group; "Validation for Knitting, Scouring and Heat Setting 6-mil Old Construction Blue PROLENE Mesh at Secant Medical"
4/7/2004	ETH.MESH.07190442	Memo to Josh Samon from Michael Pelekis re Risk Assessment for Laser Cutting of D'art Gynemesh PS Implants
8/26/2011	ETH.MESH.06261965	Email from John Karl to Bob Washington et al. re: Braskem.....A Little History
2/3/2003	ETH.MESH.02268613	Email from Daniel Burkley to Dorothy Dion et al. re Athos: Analytical Testing
2/21/2003	ETH.MESH.02268618	Email from Dorothy Dion to Scott Ciarrocca re ATHOS: PROLENE Additive and Exposure
4/27/2005	ETH.MESH.03908707	Email from Paula Evans to Gynecare Marketing & Gynecare Umbrella re PROLENE vs. polypropylene
3/9/2006	ETH.MESH.00750766	Interim Report, PSE Accession NO: 05-0070 "Test and Control Article Material Characterization Program" with TVT-Secur Implant and EO Sterilization
4/27/2010	ETH.MESH.02185004	Email from James Flint to Elizabeth Vailhe re surface area

	ETH.MESH.09479067	TVT PROLENE Polypropylene Mesh Rool Stock Appendix II Digital Photograph of 050166
2/16/2011	ETH.MESH.03146492	Email from Joerg Holste to Judi Gauld et al. re Prosima +M clin stra
3/13/2006	ETH.MESH.05446127	Email from Joerg Holste to Dieter Engel re Mesh and Tissue Contraction in Animal
	ETH.MESH.00838428	"Characteristics of Synthetic Materials Used in Prolapse and Incontinence Surgery" powerpoint presentation By A. Arnaud & D. Robinson
10/2/2003	ETH.MESH.05483362	"ULTRAPRO Mesh Pricing Committee Presentation"
9/25/2012	ETH.MESH.08315779	Piet Hinoul Clinical Expert Report Gynecare Prolift +M Pelvic Floor Repair System
11/2004	ETH.MESH.00659678	The TVM Group, "Conceptual advances in the surgical management of genital prolapse" article
	ETH.MESH.05718952	Project Edelweiss Characteristics grid
3/11/2005	ETH.MESH.05549189	Email from Joerg Holste to Sandy Savidge re Infection Risk implantation TVT-U
	ETH.MESH.05505944	Clinical Infection Risk Assessment for Gynecare TVT Universal (TVT U)
12/21/2004	ETH.MESH.05245392	Email from Joerg Holste to Steve Bell et al. re TVT - Next Generation Questionstion
6/2/2005	ETH.MESH.06403725	Final Report: Ethicon Study No. SOD4/2-2-1: A 3 month pre-clinical trial to assess the fixation force of a new TVT (TVTx) in the sheep model
1/3/2006	ETH.MESH.05246116	Email from Dan Smith to Allison London Brown et al. re Results of TVTx preclinical trial
	ETH.MESH.00840056	TVT - Secur PPT
2/28/2006	ETH.MESH.04939027	Corporate Prodcut Characterization Plan for Gynecare TVT S (Secur)
11/28/2005	ETH.MESH.00019925	Letter to Patrica Hojnoski from FDA re Gynecare TVT Secure System
7/16/2010	ETH.MESH.04940233	Preclinical Efficacy Assessment for ETHICON GYNECARE GYNEMESH M
1/20/2010	ETH.MESH.05127423	Email from Joerg Holste to Petra Koehler and Axel Arnaud re Tissue reaction ULTRAPRO
1/9/2012	ETH.MESH.08579092	Email From Christophe Vailhe to Clifford Volpe et al. Re Mesh Exposure - Ethicon Position - Short List
2/1/2012	ETH.MESH.07200381	Email from Christophe Vailhe to Clifford Volpe Re Exposure Position Norderstedt 2012.pptx
2/2/2012	ETH.MESH.07200382	"Mesh Exposure Ethicon Position" Powerpoint presentation
3/5/2012	ETH.MESH.04548236	CDMA Meeting Minutes -2012
11/1/2010	ETH.MESH.07192033	Letter to Michael Richter from PA Consulting re "Investigation into mesh erosion in pelvic floor repair"

2/17/2011	ETH.MESH.07192242	Email from Peter Meier to Julie Bird et al., Re Sales reps in UK
7/21/2011	ETH.MESH.07198825	Email from Christophe Vailhe to Ian Rhodes at PA Consulting re Mesh erosion report attached
1/20/2011	ETH.MESH.07192012	PA Consulting Group - Mesh Erosion Interview - Surgeon (Rhona Kearney)
1/18/2011	ETH.MESH.07192412	PA Consulting Group - Mesh Erosion Interview - Pathology (Klosterhalfen)
1/14/2005	ETH-07152	Clinical Expert Report: GYNECARE PROLIFT Pelvic Floor Repair System by Charlotte Owens
2/9/2011	ETH.MESH.07197998	Email from Christophe Vailhe to Michael Richter et al. Re: You have been selected - Forces on the pelvic floor - challenge to determine
5/18/2011	ETH.MESH.07192872	Email from Piet Hinoul to Pann Hermansson and Christophe Vailhe Re Forces in the pelvic floor
2/16/2011	ETH.MESH.02185584	Biomechanical consideration for Pelvic floor mesh design
1/16/2012	ETH.MESH.07200224	Email from Christophe Vailhe to Juergon Trzewik re Biomechanics of the pelvic floor
	ETH.MESH.07876572	TVT Secure 510(k)
	ETH.MESH.01217925	An exploratory 91-Day Tissue Reaction Study of Polypropylene Based Surgical Mesh in Parts (PSE ACC. NO. 00-0035)
8/8/2006	ETH.MESH.02091873	Holste & Barbolt signed ISO 10993 testing documents
2/27/2004	ETH.MESH.00863391	Email from Dan Smith to Janice Burns re Important: 2 TVT complaints concerning allegedly brittle mesh
11/10/2004	ETH.MESH.02180828	Letter from Dr. Eberhard
10/18/2004	ETH.MESH.02180833	Translation of Dr. Eberhard letter
10/12/2005	ETH.MESH.03535750	Letter to Herve Fournier RE 810041B TVT Device, Blue Mesh - complaint
2/15/2006	ETH.MESH.00584291	Email from Jacqueline Flatow to Sungyoon Rha et al. Re Dver protocol for particle loss
5/1/2006	ETH.MESH.03358217	Email from Gene Kammerer to Herve Fourier re French Standard on TVT & Meshes
5/4/2006	ETH.MESH.01221024	Email from Gene Kammerer to Herve Fournier et al. Re: New Standards for Urethral Slings
5/9/2006	ETH.MESH.01219629	Email from Jacqueline Flatow to Gene Kammerer re Particle loss on TVT
6/6/2006	ETH.MESH.00584488	Email from Herve Fournier to Gene Kammerer et al., Re: New Standards for Urethral Slings
8/31/2007	ETH.MESH.00844331	Email from David Robinson to Yukie Yamano et al. Re: Asking TVT Complication? - Fraying
8/31/2007	ETH.MESH.00844341	Email from David Robinson to Thomas Barbolt Re: Asking TVT Complications? - Fraying

6/18/1999	ETH.MESH.05315240	A 28-Day Intramuscular Tissue Reaction Study in Rats of Polypropylene Mesh from the TVT (Ulmsten) Device (PSE ACCESSION NO. 97-0197)
7/19/1996	ETH.MESH.04447134	Corporate Product Characterization - Product Safety Profile (Prolene)
10/1/1997	ETH.MESH.08218336	Biocompatibility Risk Assessment for PROLENE Polypropylene Mesh
10/1/1997	ETH.MESH.08218337	Literature Review on Biocompatibility of Prolene Sutures and Implants
	ETH.MESH.02134271	Mechanisms of Cytotoxicity for TVT Polypropylene Mesh (DRAFT)
3/5/2003	ETH.MESH.05316755	Histological Evaluation and Comparison of Mechanical Pull Out Strength of Prolene Mesh and Prolene Soft Mesh in A Rabbit Model
8/8/2005	ETH.MESH.07876890	Examination of an Extract of TVT-Secur Implant ETO Steril, Implantat for Cytotoxix Properties in a Cell Culture Test
8/8/2005	ETH.MESH.07876905	Intracutaneous Test of an Extract of TVT Secur Implant ETO Steril Implantat in Rabbits
8/8/2005	ETH.MESH.07876870	Examination of an Eluate of TVT-Secur Implant ETO Steil, Implanat of Pyrogenic Properties in Rabbits
	ETH.MESH.07876820	K052401: Response to FDA's Request for Additional Information: Gynecare TVT Secur System
1/28/1998	ETH.MESH.00371496	Letter to Gregory Jones from FDA re Tension Free Vaginal Tape (TVT) System
11/2/2001	ETH.MESH.07469275	Biocompatibility Risk Assessment for TVT-AA - Revised
12/8/2003	ETH.MESH.00019863	TVT-O 510(k)
2/8/2006	ETH.MESH.00874032	Email from Mark Yale to Cindy Crosby et al. Re: MHRA Request - TVT (change to dying process)
6/6/2001	ETH.MESH.01159961	Biocompatibility Risk Assessment for the TVT-L Device
8/27/2008	ETH.MESH.06851860	Gynecare TVT AA - CE Mark Technical File
	ETH.MESH.02026591	Sunoco MSDS
7/9/1992	ETH.MESH.09557798	7 Year Dog Study with explant images
3/30/2012	ETH.MESH.03949361	Dyed Prolene Batch Review
10/1/1992	ETH.MESH.09557819	Handwritten notes from 7 year dog study
	ETH.MESH.00339437	5 years Sales Piece - TVT
	ETH.MESH.09671620	Weights, elasticity etc chart
	ETH.MESH.09651393	Invention disclosure
	ETH.MESH.09654601	Uniaxial Test- theoretical considerations
	ETH.MESH.03032928	FDA Review - R&D
	ETH.MESH.02995494	"Evidence to Support Innovation" PowerPoint presentation by Judi Gauld
12/21/2007	ETH.MESH.02588170	Slide from Trzewik presentation

6/6/2000	ETH.MESH.03924557	"Meshes in Pelvic Floor Repair" By Brigitte Hellhammer
	ETH.MESH.03658980	TVT-PA 510 (k)
7/9/2007	ETH.MESH.05588123	Email from Stephen Wolhert to Brigitte Hellhammer et al. re Costello Article
2008-2010	ETH.MESH.02340504	Gynecare TVT IFU
2006	ETH.MESH.00584491	Email re AFNOR standards
2010-Present	ETH.MESH.03427878	TVT IFU
2006-2008	ETH.MESH.05222673	TVT IFU
2005-2006	ETH.MESH.02340471	TVT IFU
2003-2005	ETH.MESH.02340306	TVT IFU
2001-	ETH.MESH.05225354	TVT IFU
	ETH.MESH.02340568	TVT-S IFU
	ETH.MESH.02340902	TVT-O IFU
	ETH-10187	Prolift Patient Brochure
	ETH.MESH.00748451	Prolif & Prolift +M 510
	ETH.MESH.02341954	Prolift & Prolift +M Patient Brochure
	ETH.MESH.00006796	Stand and Deliver PowerPoint Presentation
	ETH.MESH.04941016	Lightweight Mesh Development PowerPoint by Juergen Trzewik
7/6/2007	ETH.MESH.05447475	Email from Dieter Engel to John Gillespie et al. re How inert is polypropylene?
	ETH.MESH.05237872	"Mesh Properties - How Important are they?" by Peter Meier
1999	ETH.MESH.05644163	Pelvic Floor Repair – Surgeon's Feedback on Mesh Concept
8/4/2009	ETH.MESH.04066979	Email re Dynamesh in Brazil
6/23/1998	ETH.MESH.09266657	Email from Larry Ellington re Prolene Mesh for TVT
	ETH.MESH.05225380	TVT IFU
	ETH.MESH.02340331	TVT IFU
	ETH.MESH.03427878	TVT IFU
2007	ETH.MESH.06861473	Gynecare TVT Secure Competitive Product Update PowerPoint presentation
7/12/2000	ETH.MESH.01317515	Preventia document
8/21/2000	ETH.MESH.03909708	Email from Axel Arnaud re Pelvic Floor Repair Procedural Strategy
10/2000	ETH.MESH.04044797	TVT Update: Success & Complications (Causes and recommendations)
6/22/2001	ETH.MESH.02089392	Scientific Advisory Panel on Pelvic Floor Repair - Preliminary Minutes
4/25/2002	ETH.MESH.01317510	Device Design Safety Assessment (DDSA) Re-Evaluation for TVT
12/2/2005	ETH.MESH.04385229	Clinical Expert Report - Gynecare TVT Secur System
1/29/2009	ETH.MESH.04093125	Email from Meng Chen re TVT IFUs on tape extrusion, exposure and erosion
	ETH.MESH.04081189	Meeting agenda

12/17/2008	ETH.MESH.00772231	Email from Robin Osman re Updated Fair Balance for TVT Brochure
12/17/2008	ETH.MESH.00772228	Email from Robin Osman re 2008 Budget Spend
12/18/2008	ETH.MESH.00339083	Email from Bryan Lisa re TVT Patient Brochure Fair Balance/EPI changes
3/2/2004	ETH.MESH.00865322	Email from Charlotte Owens re Reminder on BLUE mesh!
3/9/2004	ETH.MESH.00863405	Email from Brian Luscombe re Complaint TVTO
	ETH.MESH.01805985	"The Mesh Story" PowerPoint presentation by Dan Smith
11/10/2009	ETH.MESH.06921060	Email from Joseph Lanza re Preread for Web Conference
	ETH.MESH.06696593	Design FMEA TVT LCM Project
	ETH.MESH.06856958	"Gynecare TVT Obturator System" PowerPoint Presentation
10/13/2002	ETH.MESH.03910183	Email from Axel Arnaud re Soft Prolene
6/6/2001	ETH.MESH.03905472	Email from Martin Weisberg re TVT recommendation from Dr. Alex Wang
2/27/2004	ETH.MESH.00863391	Email from Dan Smith re Important: 2 TVT Complaints concerning allegedly brittle mesh
11/10/2004	ETH.MESH.02180828	Dr. Eberhard Compliant
10/18/2004	ETH.MESH.02180833	Translation of Dr. Eberhard letter
5/9/2006	ETH.MESH.00585802	Email from Gene Kammerer re Particle Loss on TVT
6/12/2006	ETH.MESH.00585842	Email from Gene Kammerer re TVT LCM - particle loss (reimbursement submission)
	ETH.MESH.03932912	The History of TVT
	ETH.MESH.06859904	"TVT: Insights into the Making of a Revolution" by Sheri Dodd
11/7/2005	ETH.MESH.05220458	Email from Wanda Petire-Singer re TVT Records
	ETH.MESH.03714599	Unsigned Clinical Expert Report Gynecare TVT Secur System
9/15/2005	ETH.MESH.03905619	Email from Martin Weisberg re clinical expert report
11/18/2003	ETH.MESH.00541379	"Mesh fraying for TVT Devices" memo
10/21/2008	ETH.MESH.02310653	Email from Sandy Pompilio re Information about FDA notification on use of mesh in pelvic surgery
12/10/2004	ETH.MESH.01811770	Email from Steve Bell re VOC on Laser Cut Mesh
	ETH.MESH.06857406	"TVT-Bridge) Retaining Leadership" PPT
	ETH.MESH.01265223	Risk Managent Report (legacy) for TVT and TVT-O
	ETH.MESH.00070187	Company Procedure for Medical Device Risk Management Plan
11/29/2004	ETH.MESH.01811758	Email from Paul Parisi re TVT Laser Cut mesh business case (for meeting this afternoon)
1/18/2011	ETH.MESH.08474562	2010 Performance and Development Plan Summary for Daniel Smith
	ETH.MESH.01816988	Mesh Timeline

	ETH.MESH.00838428	"Characteristics of Synthetic Materials Used in Prolapse and Incontinence Surgery" powerpoint presentation By A. Arnaud & D. Robinson
		Section of Ethicon Powerpoint showing Weights
04/2008	ETH.MESH.06867612	"Matrix Material" PowerPoint Presentation
2002	ETH.MESH.06894461	Klinge, U., Klosterhalfen, B., Birkenhauser, V., Junge, K., Conze, J., Schumpelick, V. <i>Impact of Polymer Pore Size on the Interface Scar Formation in a Rat Model</i> . Journal of Surgiccal Research. 103, 208-214 (2002)
	ETH.MESH.06893952	"Evaluation of UltraPro Meshes" PowerPoint Presentation
11/26/2002	ETH.MESH.03910418	Email from Axel Arnaud re Mini TVT - mesh adjustment
1/16/2007	ETH.MESH.06868377	Email from Reinhard Juraschek re shrinkage review
3/4/2008	ETH.MESH.08474542	2007 Performance and Development Plan Summary for Daniel Smith
2/28/2003	ETH.MESH.01222617	Histological Evaluation and Comparison of Mechanical Pull Out Strength of Prolene Mesh and Prolene Soft Mesh in A Rabbit Model
	ETH.MESH.06923868	TVTO-PA Clinical Strategy
1/20/2012	ETH.MESH.08474570	2011 Performance and Development Plan Summary for Daniel Smith
3/8/2009	ETH.MESH.08474547	2008 Performance and Development Plan Summary for Daniel Smith
1/25/2010	ETH.MESH.08474555	2009 Performance and Development Plan Summary for Daniel Smith
9/13/2010	ETH.MESH.06917699	Form for Customer Requirements Specification (CRS) For Project TVT-O PA
08/2010	ETH.MESH.02218268	"TOPA & SCION PA Alignment" PowerPoint Presentation
11/1/2004	ETH.MESH.05548122	Email from Dan Smith re Update from the Oct 27 cadaver
12/14/2004	ETH.MESH.01809080	Comparison of Laser-Cut and Machine-Cut TVT Mesh to Meshes from Competitive Devices (BE-2004-1641)
6/18/2008	ETH.MESH.04048515	Meeting minutes re Project Scion
	ETH.MESH.01228079	Nilsson Podcast Transcript
	ETH.MESH.02227368	Meshes/Devices Chart
	ETH.MESH.02219202	Material Specification for TVT Prolene Polypropylene Mesh Roll Stock
9/25/2012	ETH.MESH.08315779	Piet Hinoul Clinical Expert Report Gynecare Prolift +M Pelvic Floor Repair System
1996	ETH.MESH.05795664	Ulmsten, U., et. Al. <i>An Ambulatory Surgical Procedure Under Local Anesthesia for Treatment of Female Urinary Incontinence</i>

	ETH.MESH.05972834	Asset Purchase Agreement
	ETH.MESH.08477464	Company Procedure for the Ethicon Product Development Process (PDP)
	ETH.MESH.03742864	Operating Procedure for Failure Modes and Effects Analysis Application (AFMEA) or Design (dFMEA)
	ETH.MESH.03742571	Company Procedure for Medical Device Risk Management Plan
	ETH.MESH.01268264	Risk Management Report (legacy) for TVT and TVT-O
	ETH.MESH.03652924	Form for Internal Audit Corrective Action Plan
2/24/2006	ETH.MESH.00302105	Memo re TVT Laser Cut Mesh (LCM) Risk Analysis Summary
	ETH.MESH.01310061	Risk Management report TVT Laser Cut Mesh (LCM)
	ETH.MESH.01310476	Risk Management report TVT Laser Cut Mesh (LCM)
1/29/2009	ETH.MESH.06858146	Email from Dan Smith re TVT-O resin Minute Jan 31th
	ETH.MESH.06858314	Test Method for the Thickness of Mesh
	ETH.MESH.08438961	Work instructions for Device Design Risk Management
2/14/2003	ETH.MESH.06873447	Due Diligence Growth Opportunity Outline
3/4/2003	ETH.MESH.00858094	Gynecare R&D Monthly Update - March
	ETH.MESH.00858092	Gynecare R&D Monthly Update - June
6/24/2003	ETH.MESH.02180737	Email from Ronnie Toddywala re Project Mulberry
	ETH.MESH.03932909	History of TVT-O
	ETH.MESH.00857891	"Top Ten Reason To Pursue....Gynecare TVT Obturator System" PowerPoint Presentation by Brian Luscombe
	ETH.MESH.00858891	TVT projects charting document
1/22/2004	ETH.MESH.00857821	Gynecare TVT Obturator System Sales Training Launch Meeting
8/8/2003	ETH.MESH.03803462	Email from Laura Angelini re Transient Leg Pain with Mulberry
12/19/2003	ETH.MESH.00259473	TVT-O DDSA
3/29/2004	ETH.MESH.02180759	Letter from Jean de Leval
7/24/2003	ETH.MESH.00864101	Email from Dan Smith re TOVT development
8/8/2007	ETH.MESH.06861426	Email from Julie Hocknell re Adventures with TVT Secur
8/15/2003	ETH.MESH.00864131	Email from Brian Luscombe re Aug 11 program
	ETH.MESH.03926030	Meeting minutes re Project Scion
	ETH.MESH.00858096	Gynecare R&D Monthly Update - May
5/29/2003	ETH.MESH.00260020	Study Grid
6/17/2003	ETH.MESH.01815611	Email from Dan Smith re Discussion 11th June 2003
6/3/2003	ETH.MESH.00858175	Mulberry Weekly Meeting Minutes
1/16/2004	ETH.MESH.06164409	Email from Dan Smith re Dedication
2010	ETH.MESH.06260647	R&D CO-OP Welcome Guide Spring 2010

	ETH.MESH.01316727	Design History 1 book 1999 - TVT 5mm version
	ETH.MESH.01317508	Design History 1 book 1998 - TVT factbook
11/19/2010	ETH.MESH.00748213	TVT Classic IFU Revision Project Design Requirements Waiver Rationale Memo
	ETH.MESH.00858636	TVT Secur lessons learned review
7/18/2005	ETH.MESH.04939148	Corporate Product Characterization plan for Gynecare TVT S (Secur)
	ETH.MESH.01150009	Gynecare TVT Secur Presentation by Dan Smith
2007	ETH.MESH.06861473	Gynecare TVT Secur Competitive Product Update
	ETH.MESH.06860553	TVT & TVT Secur Documents
	ETH.MESH.04316544	Company Procedure for the Ethicon Product (PDP) - Design Controls
	ETH.MESH.00363605	Company Procedure for Design Changes to Existing Products
	ETH.MESH.05432198	Operating Procedure for Failure Modes and Effects Analysis Application (AFMEA) or Design (dFMEA)
10/7/2004	ETH.MESH.05456924	Email from Dan Smith to TVTx - Next Generation TVT "Project Initiation"
11/22/2004	ETH.MESH.00259042	2004 Strategy Tree Project Definition
	ETH.MESH.01217673	TVT-NEXT (TVTx) Development contract
4/25/2005	ETH.MESH.06274935	Email from Raimo Sump re TVT Secur Minutes - Team Meeting April 12 2005
	ETH.MESH.01410044	Gynecare TVT Secur Product Specs and changes
	ETH.MESH.05554367	Finger Pad Detail Drawings
	ETH.MESH.04385192	Gynecare TVT Secur Product Specs and changes
	ETH.MESH.05502894	Design Requirements Matrix - TVT S
	ETH.MESH.01592178	Design Validation Report - TVT S
	ETH.MESH.07876572	TVT Secure 510(k)
	ETH.MESH.02135955	Design Validation Report - TVT S
10/29/2007	ETH.MESH.00642325	Email from Kevin Mahar re TVT O versus TVT Secur efficacy and safety rate
7/28/2004	ETH.MESH.06869750	Human Cadaver Wetlab
2/8/2005	ETH.MESH.01037530	A 3 month pre-clinical trial to assess the fixation force of a new TVT (TVTx) in the sheep model - Ethicon's Final Report
2005	ETH.MESH.00034720	A 3 month pre-clinical trial to assess the fixation force of a new TVT (TVTx) in the sheep model - Published article
10/27/2004	ETH.MESH.05537701	Email from Walter Artibani re Results of TVTx preclinical trial
8/23/2005	ETH.MESH.00749504	Final Report, PSE Accession Number 05-0395, Project Number 67379: Evaluation of fixation force for the Gynecare TVT Secur Device in a sheep cadaver pelvic floor model

8/23/2005	ETH.MESH.00749518	Final Report, PSE Accession Number 05-0396, Project Number 67379: Evaluation of the Pullout Force of Gynecare TVT Secur implanted into the urogenital diaphragm and obturator membrane of a human cadaver
12/2/2005	ETH.MESH.03714002	Clinical Expert Report - Gynecare TVT Secur System
	ETH.MESH.00853802	Medical device risk management/company procedure for Medical Device Risk Management Plan: PR602-003
	ETH.MESH.00538202	A Pilot Study of the Gynecare TVT Secur System for Treatment of Stress Urinary Incontinence
11/21/2005	ETH.MESH.00752863	Gynecare TVT Secur - Manufacture and subsequent operations of the Inserter Body
11/22/2005	ETH.MESH.03648795	Gynecare TVT Secur - Inserter Assembly Welded
6/6/2006	ETH.MESH.0109412	Process at Ethicon Sarl and Ethicon BmbH for the TVT Secur System
5/18/2006	ETH.MESH.0554680	Email from Risa Cantimbuhan re Design Transfer checklist discussion
	ETH.MESH.05534022	aFMEA for TVT Secur - CO-0011927 change
	ETH.MESH.00823549	aFMEA for TVT Secur - Additional Change
	ETH.MESH.05534...	Design GMEA for TVT Secur, Version 1, FMEA-00002680
	ETH.MESH.01407837	PFMEA-100152
	ETH.MESH.00752921	Risk Management Report TVT Secur Revision A
	ETH.MESH.00752928	Risk Management Report TVT Secur Revision B
	ETH.MESH.00752933	TVT Secur Harms/Hazards table Version A
	ETH.MESH.05534013	Risk Management Report: TVT Secur
6/20/2003	ETH.MESH.01814371	Email from Katrin Elbert re Design Control
	ETH.MESH.01814384	Work Instruction for New Product Design Control
3/16/2004	ETH.MESH.03364540	Email from Dan Smith re TVTO training Carmel Ramage
8/18/2004	ETH.MESH.06884516	Email from Kevin Mahar re Dr. Jensen Follow up
6/2/2003	ETH.MESH.00862727	Email from Dan Smith re My notes from the Thursday evening presentation 5/22/03 and Friday's surgery
6/22/2004	ETH.MESH.06881589	Email from Janice Burns re Gynecare TVT Oburator Global Launch Update - Issue 4
8/17/2004	ETH.MESH.01815505	Email from Janice Burns re TVTO Dr. Feagins case follow up
9/8/2004	ETH.MESH.06884726	Email from Shannon Campbell re Ongoing TVT-O Action Items
9/14/2004	ETH.MESH.00864493	Email from Dan Smith re Ongoing TVT-O Action Items
8/17/2004	ETH.MESH.06881576	Email from Janice Burns re TVTO
5/5/2004	ETH.MESH.00864407	Email from Dan Smith re TVT-O

2/19/2004	ETH.MESH.06892171	Email from Dan Smith re TVT-O recognition Submission JANICE FOR YOUR COMMENTS!!!!!!!
9/8/2004	ETH.MESH.00864490	Email from Dan Smith re Ongoing TVT-O Action Items
2/20/2003	ETH.MESH.03911107	Email from Axel Arnaud re TVT complications (an Prof. Hausler)
7/21/2004	ETH.MESH.03910799	Email from Axel Arnaud re TVT Erosions?
11/28/1999	ETH.MESH.03917309	Email from Rodrigo Bianchi re TVT event
1/31/2006	ETH.MESH.03911712	Email from Axel Arnaud re TVT - TVT-O Specifications
6/6/2003	ETH.MESH.03907853	Email from Laure Le Treguilly re TVT - Serious Complication
	ETH.MESH.03907468	Second Generation TVT
	ETH.MESH.03907327	Trans-obturator TVT - Procedure In-Out Pr J. de Leval (University of Liege, Belgium)
5/25/2003	ETH.MESH.03910890	Email from Axel Arnaud re Follow up Mulberry
6/9/2003	ETH.MESH.00261584	Email from Sean O'Bryan re Mulberry stage gate action item closed
8/14/2003	ETH.MESH.03911390	Email from Axel Arnaud re Transient leg pain with Mulberry
1/7/2009	ETH.MESH.01202101	Email from Aaron Kirkemo re My revised writeup of the DeLeval and Waltregny visit
2/20/2006	ETH.MESH.03938897	Email from Xavier Buchon re Pr Cosson
3/26/2003	ETH.MESH.03919404	Email from Axel Arnaud re Mulberry
6/1/2009	ETH.MESH.00860142	Email from Dan Smith re Sample Medio TVTO
	ETH.MESH.02340568	TVT-S IFU
1999	ETH.MESH.04193990	Major Executive Committee Actions
	ETH.MESH.00826057	"Gynecare TVT Secur Project Overview"
11/30/2006	ETH.MESH.03921612	Email from Ralf Felix Gotter re The more procedures the more problems
12/5/2006	ETH.MESH.03921580	Email from Dan Smith re TVT-Secur follow up conference call last week
12/15/2006	ETH.MESH.01770534	Email from Axel Arnaud re TVT-S Cookbooks
	ETH.MESH.01770535	"TVT-Secur: 'Hammock' Position"
	ETH.MESH.01770541	"TVT-Secur: 'U' Position"
12/19/2006	ETH.MESH.01000731	Email from David Robinson re TVT-S Cookbooks
12/19/2006	ETH.MESH.00519476	Email from Dan Smith re TVT-S Cookbooks
12/19/2006	ETH.MESH.03921499	Email from David Robinson re TVT Secur
12/20/2006	ETH.MESH.01784428	Email from David Robinson re TVT-S Cookbooks
1/8/2007	ETH.MESH.03912639	Email from Axel Arnaud re TVT Cookbooks
	ETH.MESH.03912647	Document re TVT procedure
1/9/2007	ETH.MESH.04204341	Email from Harel Gadot re report from Austria
	ETH.MESH.04204343	Women's Health - Monthly Report December 06
1/10/2007	ETH.MESH.03922966	Email from David Robinson re Report from Austria
1/16/2007	ETH.MESH.03922950	Email from David Robinson re TVT Secur procedural steps

3/9/2007	ETH.MESH.01000323	Email from Dan Smith re DRAFT of the latest "cookbook" after my trip to Germany
	ETH.MESH.01000449	Gynecare TVT Secur System Key Technical Points (Procedural Pearls)
5/4/2007	ETH.MESH.00163952	Gynecare TVT Secur System Key Technical Points
5/22/2007	ETH.MESH.00527832	Email from Dan Smith re TVT SECUR EU Experts Meeting - feedback & future actions
	ETH.MESH.00158289	TVT Secur Patient Brochure
1/16/2007	ETH.MESH.03922953	Email from Xavier Buchon re French data on TVT Secur
6/6/2007	ETH.MESH.03922405	Email from Andrew Beveridge re TVT Secur & NICE
10/3/2007	ETH.MESH.03922261	Email from Andrew Beveridge re AMS mini arc
11/15/1999	ETH.MESH.06692673	Ulmsten & Ethicon Consulting Agreement
10/17/1997	ETH.MESH.08476335	Scandinavian Multicenter Study of the tension free vaginal tape procedure
1998	ETH.MESH.00145084	International Urogynecology Journal and Pelvic Floor Dysfunction: Ulmsten "A Multicenter Study of Tension-Free Vaginal Tape (TVT) for Surgical Treatment of Stress Urinary Incontinence"
2001	ETH.MESH.00658806	Nilsson: Long-term Results of the Tension-Free Vaginal Tape (TVT) Procedure for Surgical Treatment of Female Stress Urinary Incontinence
2004	ETH.MESH.03930120	Nilsson study: Seven-Year Follow-Up of the Tension-Free Vaginal tape Procedure for Treatment of Urinary Incontinence
2008	ETH.MESH.00355003	Nilsson Study: Eleven Years prospective follow-up of the tension-free vaginal tape procedure for treatment of stress urinary incontinence
	ETH.MESH.00339437	TVT brochure
	ETH.MESH.01186068	Sales Aid
	ETH.MESH.08148403	Goretzlehner, U., Mollen, A. <i>PVDF as an implant material in urogynaecology.</i>
	ETH.MESH.PM.000004	TVT Retropubic Implantation video
4/23/2001	ETH.MESH.05642489	Email from Mark Sumeray to Greg Jones et al re Vypro Pelvic Floor Repair PD 00/3
2006	ETH.MESH.05457602	2006 Johnson Medal Nomination: Ultrapro Lightweight mesh product line
2002	ETH.MESH.02232930	Klinge, U., Klosterhalfen, B., Birkenhauser, V., Junge, K., Conze, J., Schumpelick, V. Impact of Polymer Pore Size on the Interface Scar Formation in a Rat Model. <i>Journal of Surgical Research</i> . 103, 208-214 (2002)
4/18/2005	ETH.MESH.04945496	Email from Klosterhalfen to Holste re Ultrapro vs. Prolene Soft Mesh
	ETH.MESH.05495419	Shrinking Meshes?
10/6/2006	ETH.MESH.09651966	Lightning PowerPoint presentation by Peter Meier

8/25/2008	ETH.MESH.03021946	T-Pro (Thunder) Pipeline Leadership Team (PLT) PowerPoint Presentation
12/12/2006	ETH.MESH.08168728	State of the knowledge of "mesh shrinkage" - What do we know?
	ETH.MESH.05489861	Sponsored Research Contract the Curators of the University of Missouri
10/1/1997	ETH.MESH.08218336	Biocompatibility Risk Assessment for Prolene Polypropylene Mesh
1/13/2010	ETH.MESH.09653077	Ethicon R&D Seminar Series meeting minutes
7/1/2006	ETH.MESH.09671612	Email from Juergen Trzewik to Peter Meier re Netzdiskussion
5/1/2008	ETH.MESH.08385338	Technical Memo Project Nuvance
	ETH-00295	Gynecare Prolift IFU
	ETH.MESH.02342194	Gynecare Gynemesh PS IFU
8/5/2009	ETH.MESH.09655947	Email from Juergen Trzewik re def. Stress Shielding
	ETH.MESH.09645766	When the Implant Worries the Body presentation
	ETH.MESH.02588182	Exploratory Program "Thunder" presentation by Trzewik and Meier
1/8/2009	ETH.MESH.09656632	Biomechanical consideration presentation
	ETH.MESH.09652185	Today's vaginal implants do not consider the patients' biomechanical needs
8/1/2006	ETH.MESH.05454207	Email from Juergen Trzewik to Peter Meier re fotos cadevar lab
6/21/2011	ETH.MESH.05718101	Email from Konrad Schmitt to Boris Batke et al. re Classification of Meshes - UPDATE
4/13/2011	ETH.MESH.09656790	Email from Juergen Trzewik to Stale Kvitle et al re laser cutting
1998	ETH.MESH.09264884	Long term goals
1998	ETH.MESH.10183005	Gynecare European marketing plan
6/20/2001	ETH.MESH.00159473	Gynecare TVT Tension-free Support for Incontinence Mesh Sales Aid
	ETH.MESH.09279097	Prolene Mesh Improvement Project
11/14/2008	ETH.MESH.01203957	The Future of Surgical Meshes PowerPoint
5/6/2005	ETH.MESH.00526473	Email from Allison London Brown re laser-cut mesh
4/19/2004	ETH.MESH.0058411	Email from Gene Kammerer to Fabrice Jendly et al re Ultrasonic Slitting of Prolene Mesh for TVT
12/19/2005	ETH.MESH.00687819	Email from Kevin Mahar re Lazer cut mesh
10/18/2006	ETH.MESH.01822361	Email from Dan Smith re TVT Secur
2/27/2004	ETH.MESH.06881079	Email from Dan Smith re Important: 2 TVT Complaints concerning allegedly brittle mesh
4/18/2006	ETH.MESH.00167104	Martin Weisberg Clinical Expert Report Laser Cut Mesh
3/22/2006	ETH.MESH.01219984	Completion Report for the Design Verification of TVT Laser Cut Mesh

	ETH.MESH.00858252	Memo from Allison London Brown re Mechanical Cut vs. Laser Cut Mesh Rationale
	ETH.MESH.00156909	TVT Professional Education Program
2006	ETH.MESH.03131261	Barbolt, T., Biology of polypropylene/polyglactin 910 grafts
	ETH.MESH.00081133	Prolift +M IFU
6/18/2008	ETH.MESH.02126222	KOL Interview - Carl G. Nilsson
	ETH.MESH.02310501	Matrix - A powerful new tool in "Advanced Tissue Reconstruction"
	ETH.MESH.02310498	Matrix Avator Thunder Product Requirements
11/11/1998	ETH.MESH.09264884	Meeting minutes of Project Planning Meeting
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	Klinge, U	Powerpoint Titled "Textile for the pelvic floor (flat meshes or slings)"	
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8/21/2004		Ethicon Products Tissue Reinforcement Solutions	

Date	Deponent
02/28/2012	Cliff Volpe
02/29/2012	
04/05/2012	Piet Hinoul
04/06/2012	
09/18/2012	
06/29/2013	
06/27/2013	
01/13/2013	
01/15/2013	
03/13/2012	David Robinson
03/14/2012	
08/23/2012	
09/11/2013	
3/9/2012	Sunny Rha
4/18/2012	Aaron Kirkemo
5/18/2012	Sean O'Bryan
03/29/2012	Scott Ciarrocca
03/30/2012	
12/03/2012	
03/27/2012	
03/28/2012	Vincenza Zaddem
2/24/2012	Elizabeth Vailhe
06/20/2013	Christophe Vailhe
06/21/2013	
12/14/2012	Joerg Holste
12/15/2012	
07/29/2013	
07/30/2013	
08/01/2013	Boris Batke
08/02/2013	

EXPERT REPORTS:

Expert Report of Prof. Dr.- Ing Thomas Muehl
Expert Report of Vladimir Iakovlev, MD, FRCPC, FCAP
Expert Report of Howard Jordi, Ph.D.
Expert Report of Paul Ducheyne, Ph. D.
Expert Report of Dr. Daniel Elliott, MD
Expert Report of Shelby Thames, Ph.D
Expert Report of Thomas Barbolt, Ph.D
Expert Report of Michael Greenberg, MD
Expert Report of Dr. Bernard Klosterhalfen
Expert Report of Daniel Sexton, MD